

S1. PHASE CORRECTION:

For both the temperature-controlled experiments and the multi-center datasets, a phase correction for multi-echo complex acquisitions was performed. For bipolar and/or interleaved echo train acquisitions, phase correction is needed to produce complex-based PDFF maps. A phase correction method previously implemented by Hernando et al¹ was applied to all complex acquisition images. A linear phase offset was applied in the readout and phase-encoding directions before constructing PDFF maps by minimizing the difference in water and fat amplitudes between magnitude and complex fitting. This would subsequently minimize the PDFF map inaccuracies by reducing the phase irregularities across echoes.

As mentioned earlier however, magnitude-based fitting is more susceptible to temperature-related errors than complex-based fitting². Because of this, and since we are minimizing the difference in water and fat amplitudes between magnitude and complex fitting, the effect of temperature on this phase correction method is unknown, potentially leading to residual phase errors. Also, in this work, we compare the effect of temperature on purely magnitude, purely complex, and hybrid fitting, as these three fitting methods are expected to have different sensitivity to temperature-related errors in the signal model. Because magnitude-based fitting was not applied after complex-based fitting as in Hernando et al¹, these phase errors may remain.

S2. TABLES:

MR System	Site	Vendor	Model	Software Version	Field Strength (T)
1	1	General Electric	Signa HDxt	HD23.0_V02	1.5
2	1	General Electric	Optima MR450w	DV26.0_R02/3	1.5
3	1	General Electric	Signa Premier	RX27.0_R01/2	3
4	1	General Electric	Signa PET/MR	MP26.0_R01	3
5	1	General Electric	Signa Artist	DV26.0_R02/3	1.5
6	1	General Electric	Discovery MR750	DV26.0_R01/3	3
7	1	General Electric	Signa Architect	DV26.0_R03	3
8	1	General Electric	Signa HDxt	HD23.0_V02	1.5
9	2	Philips	Ingenia	5.3.1.1	3
10	2	Philips	Ingenia	5.4.1.0	3
11	2	Philips	Ingenia	5.4.1.0	1.5
12	3	Siemens	Prisma	Syngo MR E11	3
13	3	Siemens	Skyra	Syngo MR E11	3
14	4	Siemens	Avanto	Syngo MR E11	1.5
15	4	Siemens	Skyra	Syngo MR E11	3
16	5	General Electric	Discovery MR750	DV26.0_R01	3
17	5	General Electric	Discovery MR750	DV26.0_R01	3
18	6	Siemens	Aera	Syngo MR E11	1.5
19	6	Siemens	Skyra	Syngo MR E11	3
20	7	Philips	Ingenia	5.3.1.1	1.5
21	7	Philips	Ingenia	5.3.1.1	3
22	8	Siemens	Aera	Syngo MR E11	1.5
23	8	General Electric	Discovery MR750	DV26.0_R01	3
24	8	General Electric	Discovery MR750	DV26.0_R01	3
25	9	Philips	Ingenia	5.3.0.3	1.5
26	9	Philips	Ingenia	5.3.0.3	3

Table S1: List of unique MR systems used in the multi-center study.

MR System	Field Strength (T)	TE _{mit} (ms)	ΔTE (ms)	ETL	Readout	Number of Echo Trains	Flip Angle (°)	TR (ms)	Slice Thickness (mm)	FOV (cm ²)	Matrix
1	1.5	1.66	2.30	6	bipolar	1	10	120	6	26x26	256x256
2	1.5	1.55	2.70	6	bipolar	1	10	120	6	26x26	256x256
2	1.5	1.55	2.61	6	bipolar	1	10	120	6	26x26	256x256
3	3	1.30	1.16	6	bipolar	2	10	120	6	26x26	256x256
4	3	1.14	0.83	8	bipolar	2	10	120	6	26x26	256x256
5	1.5	1.74	2.46	6	bipolar	1	10	120	6	26x26	256x256
5	1.5	1.76	2.48	6	bipolar	1	10	120	6	26x26	256x256
6	3	1.32	1.13	6	bipolar	2	10	120	6	26x26	256x256
7	3	1.34	1.21	6	bipolar	2	10	120	6	26x26	256x256
9	3	1.15	1.19	6	monopolar	1	10	121	10	50x50	384x384
9	3	1.15	1.15	6	bipolar	1	10	121	10	50x50	288x288
10	3	1.15	1.19	6	monopolar	1	10	121	10	50x50	384x384
10	3	1.15	1.15	6	bipolar	1	10	121	10	50x50	288x288
11	1.5	2.30	2.30	6	monopolar	1	10	121	10	42x42	288x288
11	1.5	2.30	2.30	6	bipolar	1	10	121	10	42x42	288x288
12	3	1.15	1.15	6	bipolar	1	10	150	10	42x42	160x160
12	3	1.15	1.15	6	bipolar	1	10	150	7	42x42	160x160
13	3	1.12	0.99	6	bipolar	1	10	150	10	42x42	128x128
13	3	1.15	1.15	6	bipolar	1	10	262	5	42x42	128x128
14	1.5	1.15	1.15	6	bipolar	1	10	160	10	42x42	160x160
14	1.5	1.12	0.99	6	bipolar	1	10	150	10	42x42	256x256
14	1.5	2.30	2.30	6	bipolar	1	10	150	10	42x42	256x256
14	1.5	2.30	2.30	6	bipolar	1	10	216	10	42x42	160x160
15	3	1.15	1.15	6	bipolar	1	10	199	10	42x42	160x160
15	3	1.12	0.99	6	bipolar	1	10	150	10	40x45	224x256
15	3	1.12	1.18	6	bipolar	1	10	150	10	40x45	224x256
15	3	1.15	0.96	6	bipolar	1	10	150	10	40x45	140x160
15	3	1.15	1.15	6	bipolar	1	10	150	10	40x45	224x256
16	3	1.32	1.13	6	bipolar	2	10	120	6	26x26	256x256
17	3	1.32	1.13	6	bipolar	2	10	120	6	26x26	256x256
18	1.5	2.30	2.30	6	bipolar	1	10	271	10	26x26	160x160
19	3	1.14	1.16	6	bipolar	1	10	150	5	26x26	160x160
20	1.5	2.30	2.30	6	bipolar	1	10	120	5	34x34	192x192
21	3	1.15	1.15	6	bipolar	1	10	120	5	34x34	192x192
22	1.5	2.30	2.30	6	bipolar	1	10	128	10	30x30	160x160
23	3	1.30	1.11	6	bipolar	2	10	120	6	26x26	256x256
24	3	0.93	1.21	6	bipolar	1	10	120	10	50x50	256x256
24	3	1.30	1.11	6	bipolar	2	10	120	6	26x26	256x256
25	1.5	2.30	2.30	6	bipolar	1	10	120	5	34x34	192x192
26	3	1.15	1.15	6	bipolar	1	10	120	5	34x34	192x192

Table S2: All unique magnitude-based CSE-MRI protocols used in the multi-center study. Some protocols were performed multiple times to produce the total 68 magnitude-based CSE-MRI acquisitions. For all acquisitions, vials were oriented along B₀ and a multi-echo spoiled gradient echo was used. Details of the MR systems are listed in Table S1. Abbreviations: ETL = echo train length, TE = echo time, TR = repetition time, FOV = field of view.

MR System	Field Strength (T)	TE _{mit} (ms)	ΔTE (ms)	ETL	Readout	Number of Echo Trains	Flip Angle (°)	TR (ms)	Slice Thickness (mm)	FOV (cm ²)	Matrix
2	1.5	0.91	1.46	6	monopolar	1	5	12.67	10	40x40	130x130
2	1.5	1.02	1.72	6	monopolar	1	5	14.11	10	40x40	104x104
2	1.5	1.12	1.94	6	monopolar	1	5	25.57	3	26x26	148x148
3	3	0.87	0.69	6	monopolar	2	3	5.84	10	44x44	144x144
3	3	1.09	0.88	6	monopolar	2	3	7.35	3	26x26	160x160
4	3	0.99	0.83	6	monopolar	2	3	7.32	8	40x40	104x104
4	3	1.08	0.94	6	monopolar	2	3	11.37	4	26x26	140x140
5	1.5	0.94	1.98	6	monopolar	1	5	14.08	8	40x40	130x130
5	1.5	0.94	1.98	6	monopolar	1	5	14.13	8	40x40	130x130
5	1.5	1.12	1.95	6	monopolar	1	3	23.71	3	26x26	148x148
6	3	0.88	0.70	6	monopolar	2	3	5.82	10	44x44	144x144
6	3	1.13	0.90	6	monopolar	2	3	7.38	3	26x26	150x150
7	3	0.94	0.78	6	monopolar	2	3	6.85	10	44x44	144x144
7	3	0.94	0.78	6	monopolar	2	3	6.71	10	44x44	144x144
7	3	1.09	0.94	6	monopolar	2	4	11.79	3	26x26	140x140
8	1.5	0.87	1.64	6	monopolar	1	5	11.79	10	40x40	256x256
8	1.5	1.11	1.79	6	monopolar	1	4	18.27	3	26x26	256x256
9	3	0.91	1.30	6	monopolar	1	3	10.00	5	34x34	256x256
9	3	0.97	0.71	6	bipolar	1	3	5.65	6	40x40	224x224
9	3	1.30	1.18	6	bipolar	1	3	10.00	5	40x40	224x224
11	1.5	0.92	0.66	6	bipolar	1	5	5.32	6	40x40	192x192
11	1.5	1.49	1.30	6	bipolar	1	5	10.00	5	22x22	160x160
12	3	1.21	1.25	6	bipolar	1	4	9.02	5	28x28	320x320
12	3	1.25	1.23	6	bipolar	1	3	10.00	5	28x28	160x160
16	3	0.88	0.70	6	monopolar	2	3	5.82	10	44x44	144x144
16	3	1.13	0.90	6	monopolar	2	3	7.38	3	26x26	150x150
17	3	0.88	0.70	6	monopolar	2	3	5.82	10	44x44	144x144
17	3	1.13	0.90	6	monopolar	2	3	7.38	3	26x26	150x150
19	3	1.25	1.24	6	bipolar	1	3	10.00	5	30x30	160x160
20	1.5	0.66	0.66	6	bipolar	1	5	5.32	6	40x40	192x192
20	1.5	0.98	0.98	6	bipolar	1	5	7.43	5	26x26	176x176
20	1.5	2.00	2.00	6	bipolar	1	3	13.30	5	34x34	224x224
20	1.5	2.00	2.00	6	monopolar	2	3	13.30	5	34x34	224x224
21	3	0.69	0.95	6	monopolar	2	3	5.55	10	40x40	192x192
21	3	0.71	0.97	6	bipolar	1	3	5.65	6	40x40	224x224
21	3	1.03	1.30	6	monopolar	2	3	10.00	5	34x34	224x224
21	3	1.18	1.30	6	bipolar	1	3	10.00	5	34x34	224x224
25	1.5	0.98	0.71	6	bipolar	1	5	5.69	6	34x34	176x176
25	1.5	2.00	2.00	6	bipolar	1	3	14.00	6	34x34	224x224
26	3	0.98	0.71	6	bipolar	1	3	5.69	6	34x34	192x192
26	3	1.30	1.19	6	bipolar	1	3	10.00	5	34x34	224x224

Table S3: All complex-based CSE-MRI protocols used in the multi-center study. Some protocols were performed multiple times to produce the total 60 complex-based CSE-MRI acquisitions. For all acquisitions, vials were oriented along B_0 and a multi-echo spoiled gradient echo was used. Details of the MR systems are listed in Table S1. Abbreviations: ETL = echo train length, TE = echo time, TR = repetition time, FOV = field of view.

S3. FIGURES:

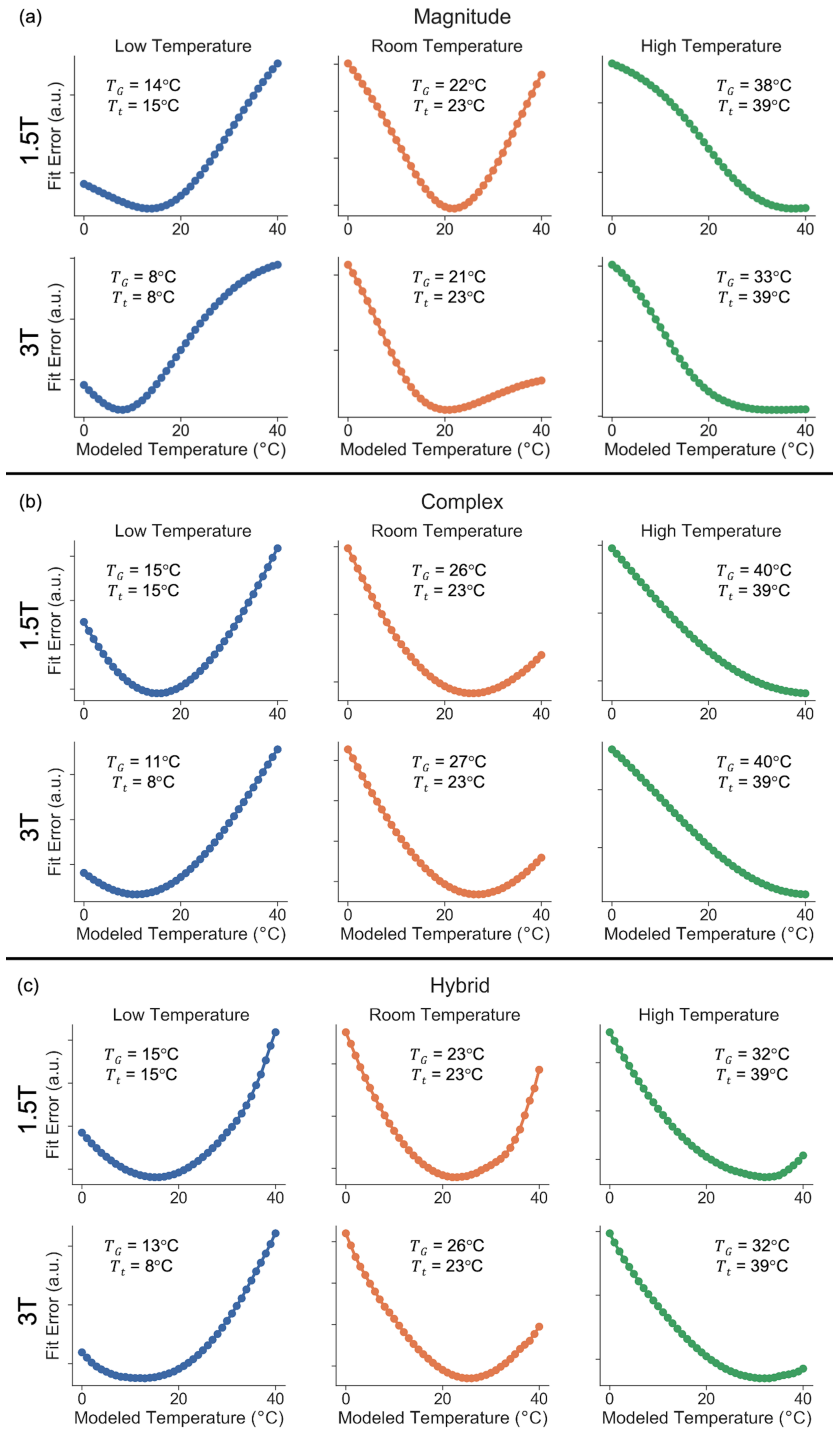


Figure S1. Global fit error can be used to estimate the true temperature of the phantom in order to correct for temperature-dependent errors in PDFF quantification. Fit error as a function of modeled temperature is shown in temperature-controlled experiments using two different field strengths (1.5T and 3T) at three different phantom temperatures (approximately 10°C, 20°C, 40°C) using a) magnitude-based b) complex-based c) hybrid-based methods. Global temperature at minimum fit error, T_G , and thermometer-measured phantom temperature, T_t are shown.

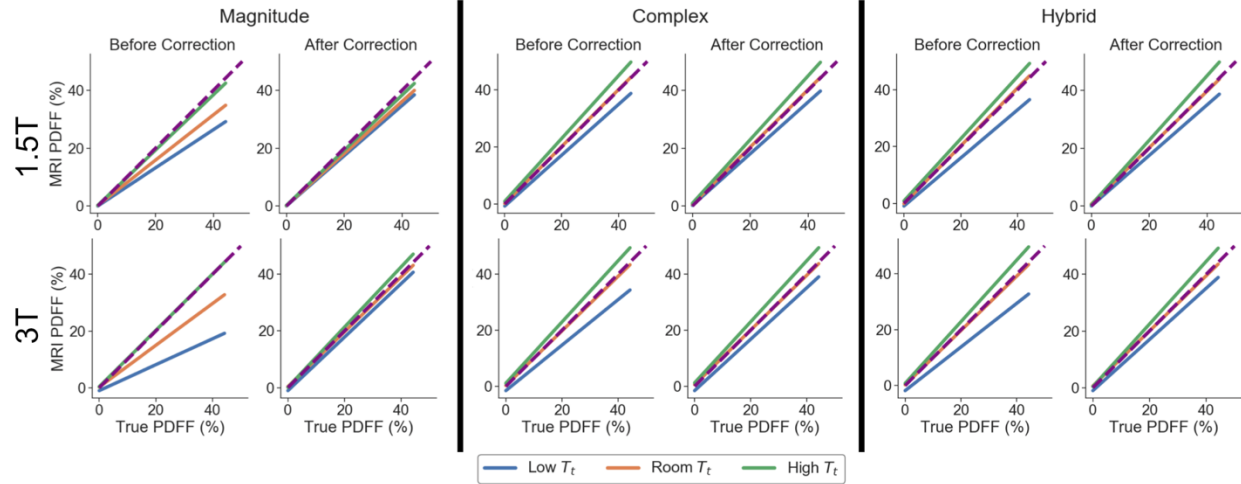


Figure S2. PDFF bias is reduced for all given true phantom temperatures (T_t) using the proposed temperature-correction method with T_G found in Figure S1. Linear regression plots of MRI PDFF as a function of the true PDFF are shown for the temperature-controlled experiments at 1.5T and 3T, before and after temperature correction, using magnitude-based, complex-based, and hybrid-based methods. The identity line is also plotted as a dashed line.

S4. REFERENCES:

1. Hernando D, Sharma SD, Ghasabeh MA, et al. Multisite, multivendor validation of the accuracy and reproducibility of proton-density fat-fraction quantification at 1.5T and 3T using a fat–water phantom. *Magn Reson Med*. 2017;77(4):1516-1524. doi:10.1002/mrm.26228
2. Hernando D, Sharma SD, Kramer H, Reeder SB. On the confounding effect of temperature on chemical shift-encoded fat quantification. *Magn Reson Med*. 2014;72(2):464-470. doi:10.1002/mrm.24951