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BASEBALL IMPACTS TO DUMMY HEADS

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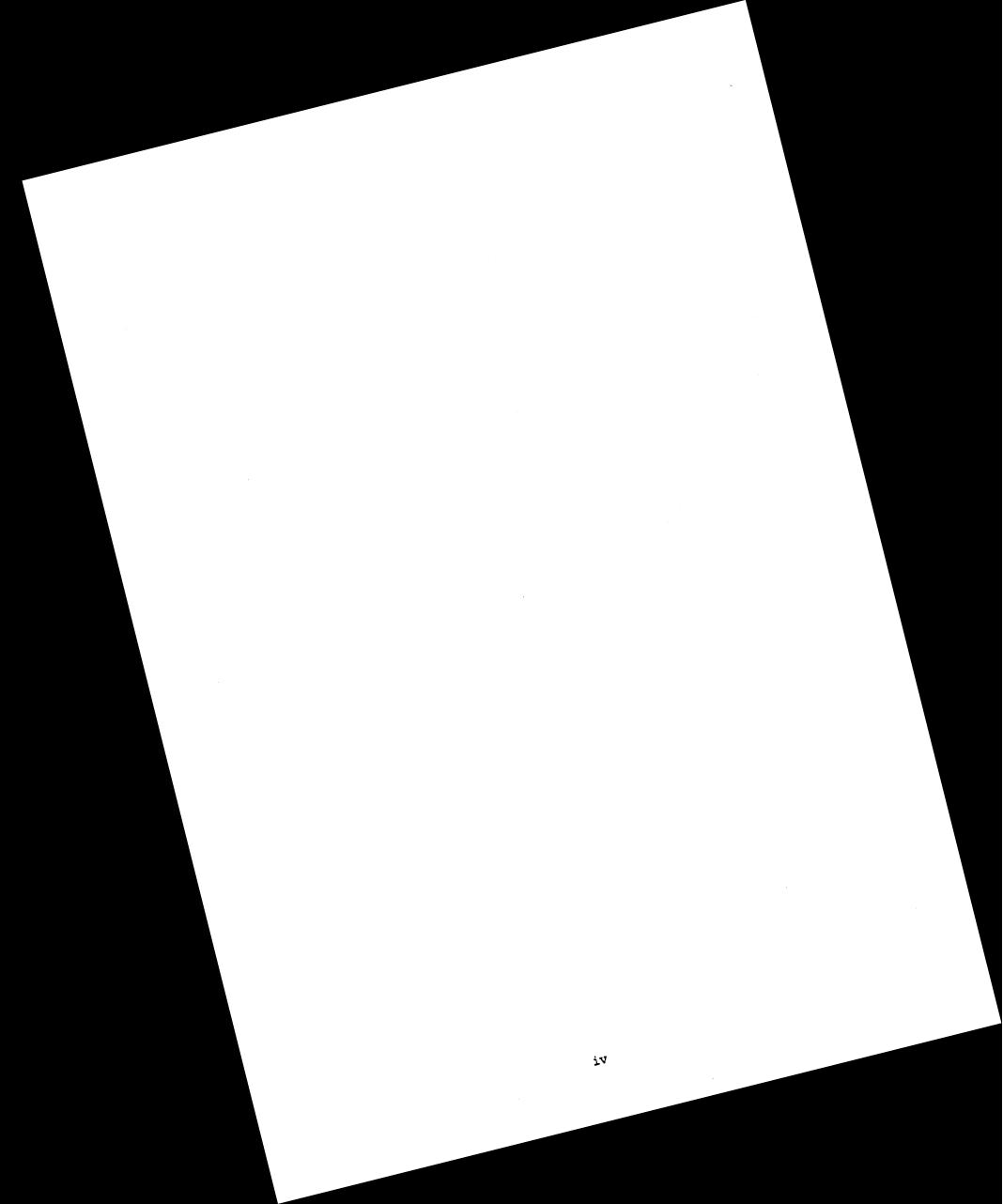
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16. Abstract

The heads of two different dummies, the Part 572 and the Hybrid III, were subjected to frontal and lateral impacts from baseballs to determine whether any significant difference may exist between test results due solely to the dummy used. Secondarily, tests were conducted with the HSRI dummy in order to compare these results with a previous test series. Variability related to dummy head construction and impact location is discussed. It was concluded that, for the impact conditions in these tests, i.e., a low mass, high velocity, hard impacting object, there was no significant difference between the Part 572 and Hybrid III dummies in frontal impact, and that the peak acceleration and HIC values obtained in direct hits to the front and side are consistent with our understanding of head tolerance due to direct rigid impact.

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Introduction

There are many situations in which accidental head injury can occur. Most of these events involve impact conditions that lack definition in terms of object contacted, velocity of contact, and attitude of the body at impact. The striking of a professional baseball batter's head by a pitched ball, however, represents a situation in which there is a demonstrated potential for head injury, such as skull fracture, concussion, and/or more serious brain damage, under narrowly defined conditions, in terms of impactor (ball) weight, velocity range, and distance of impactor travel.

Recognizing this unique situation, UMTRI conducted a series of baseball/head impacts in 1978 using regulation hard balls (5.25 oz) fired from a pitching machine at the HSRI dummy (see Jones and Mohan 1984). The primary purpose of the study was to duplicate a known injury-producing environment with a biomechanically realistic dummy and to compare the resulting head acceleration data with our understanding of human head impact tolerance. Tests included front and side impacts to the unprotected head as well as impacts to helmeted heads, to study the efficacy of various head protection devices. The speed of the baseballs was in the 80- to 100-mph range, and results were reported in terms of peak resultant acceleration and Head Injury Criterion (HIC). Our conclusions from this study were that, for the particular impact conditions simulated, i.e., small, hard, high-velocity impactor, the results were compatible with previous rigid-impact studies that suggest a HIC of 1000 indicates the likelihood of skull fracture and/or concussion.

In the current study, the impact response of the heads of two different dummies, the Part 572 and the Hybrid III, were compared to determine whether any significant difference may exist between test results due solely to the dummy used. Secondarily, tests were conducted with the HSRI dummy in order to compare these results with the previous test series. Both frontal and lateral head impacts were included.

Methodology

Fifty-one successful head impact tests were conducted using the Part 572, Hybrid III, and HSRI dummies in both forehead and temple impact locations. A baseball pitching machine was used to propel the ball at maximum speed toward each dummy head, but only direct hits were counted as successful tests. Each dummy was seated in turn in a wheelchair with its wheels locked and anchored to the ground. Table 1 summarizes the tests in terms of dummy type and impact location.

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Dummy	Frontal Impacts	Side Impacts
Part 572	10	10
Hybrid III	10	12
HSRI	4	5
TOTAL	24	27

SUMMARY OF TEST CONDITIONS

Endevco piezoresistive accelerometers (7264-2000) secured inside the dummy head at the CG site measured the triaxial accelerations. Computer analysis of the accelerations was performed to obtain the resultant acceleration-time histories and HIC values. High-speed movies at 1000 frames per second were taken of the tests with the Part 572 and Hybrid III dummies, but not with the tests of the HSRI dummy.

Test Results

Tables 2 through 7 contain the summary experimental data for all tests. The baseball velocities were derived from analysis of the highspeed films. Peak resultant head acceleration is given along with the HIC interval and finally the HIC value. The triaxial and resultant accelerations plotted versus time are included in the Appendix. The last row of each table gives the average velocity, average peak acceleration, and average HIC value with its calculated standard deviation.

Test Number	Ball Number*	Baseball Velocity (mph)	Peak Head Accel. (G)	HIC Interval (ms)	HIC
84BF13 84BF14 84BF15 84BF16 84BF17 84BF18 84BF19 84BF20 84BF21 84BF21	5-3 5-4 8-1 8-2 8-3 8-4 13-1 13-2 13-3 13-4	81.8 86.2 87.1 90.8 88.4 91.1 78.8 78.7 76.7 79.3	269 229 437 484 537 462 341 434 295 381	0.55 0.45 0.50 0.45 0.45 0.50 0.50 0.50	400 257 1127 1399 1799 1320 644 1164 459 831
AVERAGE		83.9	387	0.49	940 SD=502

TABLE 2BASEBALL IMPACT TEST SUMMARY FOR PART 572 DUMMYFRONTAL HEAD IMPACT

*The first number refers to the ball number and the second number refers to the pitch number. For example, 1-1 translates to Ball 1, pitch 1 (a new ball), while 5-4 translates to Ball 5, pitch 4.

			TABLE 3				
BASEBALL	IMPACT	TEST	SUMMARY	FOR	PART	572	DUMMY
	S	SIDE I	HEAD IMP	ACT			

Test Number	Ball Number	Baseball Velocity (mph)	Peak Head Accel. (G)	HIC Interval (ms)	HIC
84BS03 84BS04 84BS05 84BS06 84BS07 84BS08 84BS09 84BS10 84BS11 84BS12	3-2 6-1 6-2 6-3 4-1 4-2 4-3 4-4 5-1 5-2	89.30 85.2 83.2 85.7 82.9 82.9 84.0 85.2 82.0 83.3	192 167 221 212 163 176 199 168 178	0.60 0.60 0.60 0.55 0.60 0.55 0.60 0.55 0.60 0.65	179 124 151 245 211 126 140 174 131 152
AVERAGE		84.5	185	0.60	163 SD=38

TABLE 4

Test Number	Ball Number	Baseball Velocity (mph)	Peak Head Accel. (G)	HIC Interval (ms)	HIC
84BF23 84BF24 84BF25 84BF26 84BF28 84BF29 84BF30 84BF31 84BF32 84BF33 AVERAGE	14-1 14-2 15-1 15-2 16-2 17-1 17-2 18-1 19-1 19-2	83.6 82.2 82.0 85.2 83.9 82.8 81.2 81.8 87.9 85.2 83.6	280 446 311 250 430 292 263 385 438 387 348	0.60 0.70 0.55 0.60 0.50 0.65 0.60 0.55 0.55 0.5	471 1659 553 336 1156 589 391 896 1341 927 832 SD=443

BASEBALL IMPACT TEST SUMMARY FOR HYBRID III DUMMY FRONTAL HEAD IMPACT

TABLE 5

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BASEBALL IMPACT TEST SUMMARY FOR HYBRID III DUMMY SIDE HEAD IMPACT

Test Number	Ball Number	Baseball Velocity (mph)	Peak Head Accel. (G)	HIC Interval (ms)	HIC
84BS34 84BS35 84BS36 84BS37 84BS40 84BS41	20-1 20-2 21-1 21-2 23-1 23-2	85.2 88.3 81.6 81.2 87.9 85.2	257 410 214 313 407 207	0.50 0.50 0.70 0.55 0.50 1.50	320 962 297 587 922 422
84B542 84B543 84B544 84B545 84B545 84B545 84B547	23 2 24-1 24-2 24-3 17-3 14-3 14-4	84.1 80.6 81.7 85.2 83.9 85.7	334 281 186 353 356 240	0.55 0.55 0.65 0.55 0.55 0.65	654 434 169 755 755 328
AVERAGE		84.4	297	0.65	550 SD=249

TABLE 6

Test Number	Ball Number*	Baseball Velocity (mph)**	Peak Head Accel. (G)	HIC Interval (ms)	HIC
84BF53 84BF54 84BF56 84BF57 AVERAGE			446 324 285 383 359	1.8 1.8 1.0 1.8 1.6	1499 777 454 1282 1003 SD=411

BASEBALL IMPACT TEST SUMMARY FOR HSRI DUMMY FRONTAL HEAD IMPACT

TABLE 7

Test Number	Ball Number*	Baseball Velocity (mph)**	Peak Head Accel. (G)	HIC Interval (ms)	ніс
84B548			425	2.30	1590
84BS49			425	1.10	1357
84BS50			442	1.80	1694
84BS51			375	1.70	387
84BS52			422	2.35	1896
AVERAGE			418	1.85	1385 SD=49

BASEBALL IMPACT TEST SUMMARY FOR HSRI DUMMY SIDE HEAD IMPACT

*Not recorded.

**No high-speed movies were taken of these tests, therefore no velocities could be calculated.

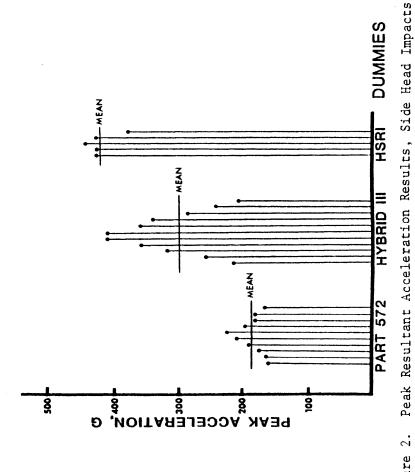
Discussion

This discussion addresses the question of whether there are differences in head response among the three dummies in these impact tests, and, if so, what the sources of these differences might be.

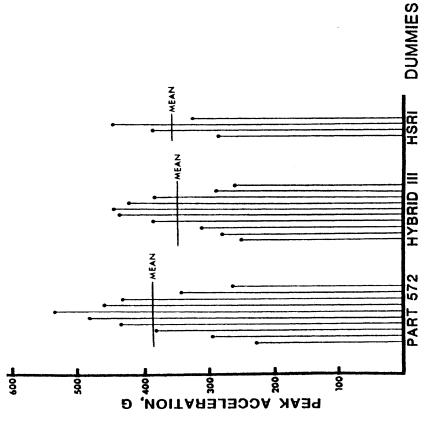
Looking first at frontal impact, Tables 2 and 4 indicate a range of peak acceleration of from 209 to 537 G for the Part 572 dummy and from 250 to 446 G for the Hybrid III. Peak acceleration is a measure of response, whereas HIC, which is a function of both acceleration and time, relates to injury potential and tends to exaggerate variations in response. A brief comment should be made at this point about the wide range of peak Gs and associated HICs within each dummy series. The reasons will be discussed in more detail with reference to the side impact tests, but basically there is a problem with hitting one curved surface with another curved surface. Small changes in impact location are likely to occur from one test to the next, which can result in large changes in the transfer of momentum to the CG of the head.

A statistical analysis (t-test) of the data from the Part 572 and Hybrid III frontal test series indicates that there was no significant difference between the mean values of the peak accelerations (p>0.35) or the mean values of the HIC numbers (p>0.65). Further, the mean of the HSRI dummy test series fell between those of the other dummies. The peak accelerations and means for all three frontal impact test series are plotted in Figure 1. Although there was a statistically significant difference between the mean HIC intervals of the first two dummies (p<0.01), this difference of less than 0.1 ms has no practical significance.

Next we look at Tables 3 and 5 and find an apparent difference between the Part 572 (mean G=185) and Hybrid III (mean G=297) results in the side head-impact condition. The HSRI dummy registered even higher peak accelerations (mean G=418). The peak accelerations and means for the side impact test series are plotted in Figure 2. Two factors are most likely responsible for these differences. One is the head construction differences among the three dummies, and the other is the problem of impact location mentioned above.



Peak Resultant Acceleration Results, Frontal Head Impacts Figure 1.





The lateral scalp characteristics and skull structures are different in all three designs. The Part 572 head features a firm, relatively thick (0.3 to 0.4 inch) vinyl scalp over a rigid cast aluminum skull. The Hybrid III head has a thicker (0.41-0.49 inch) soft vinyl scalp over a rigid cast aluminum skull. The HSRI head has a thinner (0.250-0.270 inch) soft urethane scalp over a deformable cast urethane skull, with the skull urethane being harder than the scalp material. The surface geometries of the sides of the head of each dummy differ also. The HSRI dummy head is flatter vertically over a larger area, making a direct hit easier to achieve, while both the Hybrid III and Part 572 heads have a more pronounced curvature, particularly in the upper half. In the case of the Hybrid III and Part 572 dummies, the curvature of the side of the head varies with position strongly enough to cause significantly different responses to impact for small changes in the ball contact point, either up/down or fore/aft. A test in which the only variable would be the material properties of the scalp/skull combination would require very precise control of the impactor path, impact location, and impactor properties.

The side impacts to the head of the Part 572 dummy were the first test series run in the current study. Comparison of points of ball contact for the Part 572 and Hybrid III tests from the film data indicates that the contacts were consistently higher on the head of the Part 572 dummy by about 0.5 to 0.75 inch. This resulted in consistently lower head accelerations due to a decreased transfer of momentum from the ball to the head. Similar impacts occurred in some of the Hybrid III side impact tests with similar results. Other impact sites, however, were more in line with the head center of gravity, and high head accelerations were produced.

Finally, an examination of the HIC intervals listed in Tables 2 through 7 indicates that the durations for the HSRI dummy head are three times as great as those for the other two dummies, while the corresponding average peak acceleration values for frontal head impacts are similar in all three dummies. The head acceleration traces for the HSRI dummy (see Appendix) reveal a marked oscillatory characteristic not found in the traces from the other two dummies. This is most likely due

to the unusual mounting arrangement for the accelerometers in the HSRI dummy head. This design uses a cantilevered box structure cast into the skull from the rear. Vibration of this structure, particularly in side impacts, can cause an oscillation in the head acceleration trace. Such an oscillation following the initial impact acceleration spike will cause the HIC function to converge on a longer time interval, thereby producing an erroneously high HIC value. Since the average acceleration values of the Part 572 and Hybrid III dummies bracket the HSRI dummy value, simple linear interpolation of the HIC values would indicate an estimated HIC for a non-oscillating waveform to be 862 for frontal impacts. Using the same reasoning, the side impact data must be extrapolated due to the higher average head acceleration value of the HSRI head (417 G). This results in an estimated non-oscillating waveform HIC value of 1025. Using these estimated values, the average results of the tests for all three dummies are listed in Table 8.

TABLE 8

<u></u>	Frontal Head Impact		Head Side Impact	
Dummy	Peak Accel. (G)	HIC	Peak Accel. (G)	HIC
Part 572 Hybrid III HSRI	386.8 348.3 359.0	940 832 862*	185.2 296.7 417.9	163 550 1025*

SUMMARY OF AVERAGE BASEBALL IMPACT TEST RESULTS FOR ALL DUMMIES

*Estimated.

Conclusion

For the impact conditions in these tests, i.e., a low mass, high velocity, hard impacting object, there was no significant difference between the Part 572 and Hybrid III dummies in frontal impact. For side impact, when a direct transfer of the momentum of a ball occurs, the results from both the Hybrid III and HSRI dummies indicate that baseball impacts to a batter's temple area are capable of producing 400-G accelerations with associated HIC values near 1000. These values are consistent with our understanding of head impact tolerance due to direct rigid impact, as are the values from the frontal head impact tests with all three dummies.

Reference

Jones, I.S.; and Mohan, D. (1984) <u>Head impact tolerance: Correlation</u> <u>between dummy impacts and actual head injuries</u>. Insurance Institute for Highway Safety, Washington, D.C.

APPENDIX

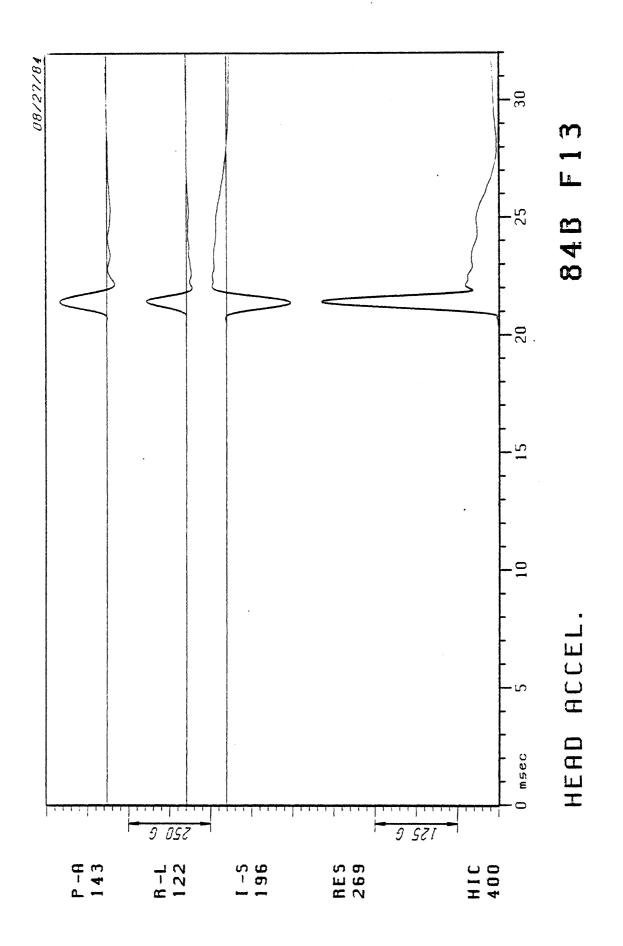
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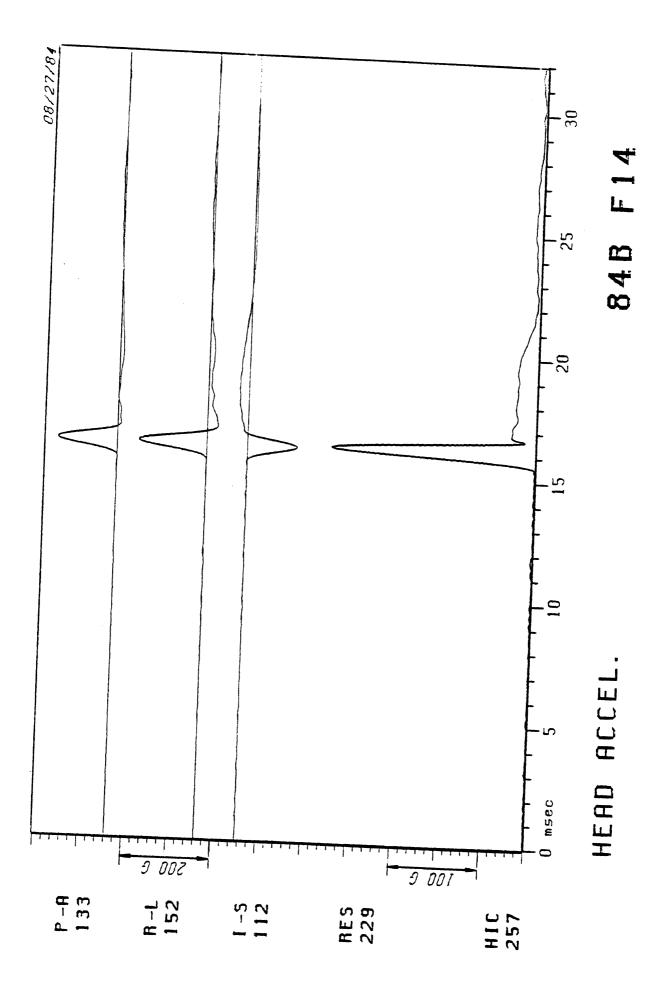
Dummy Head Acceleration Data

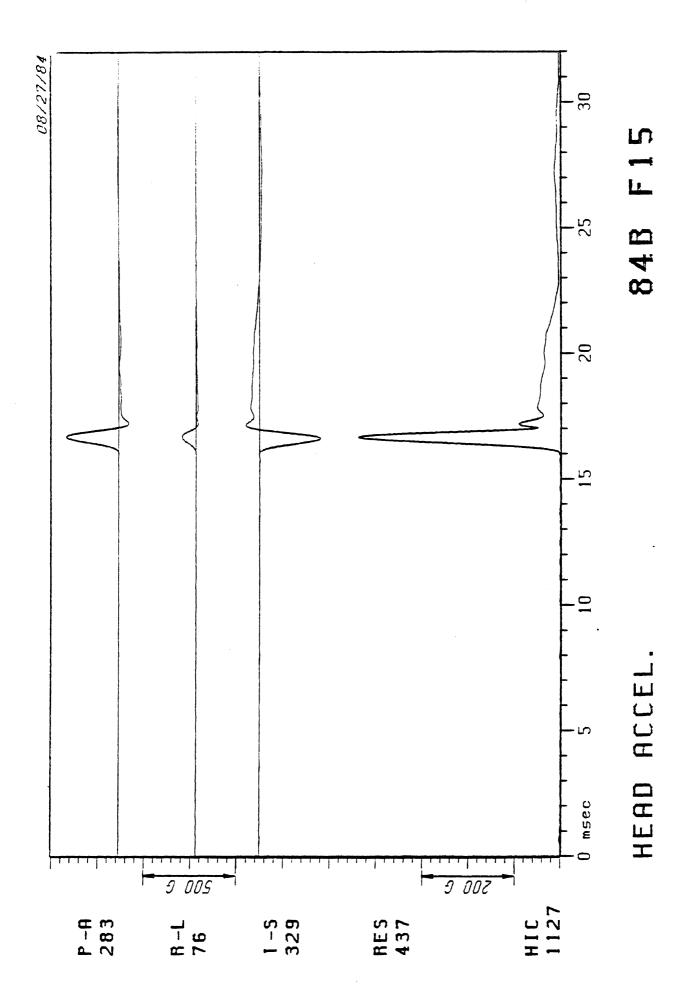
Part 572 Dummy Results

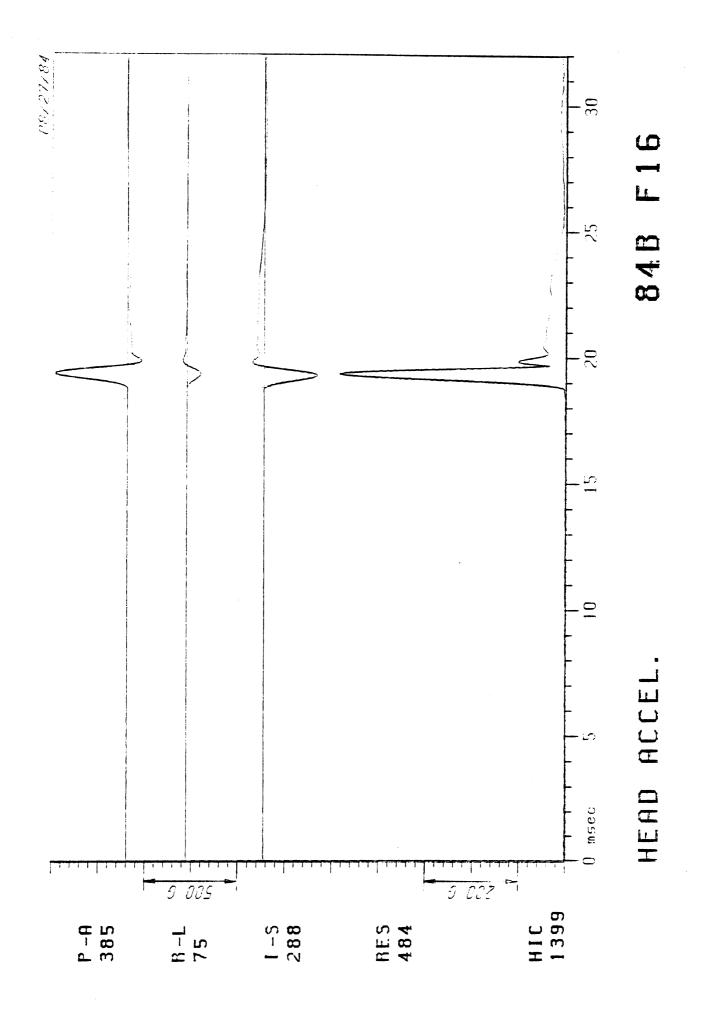
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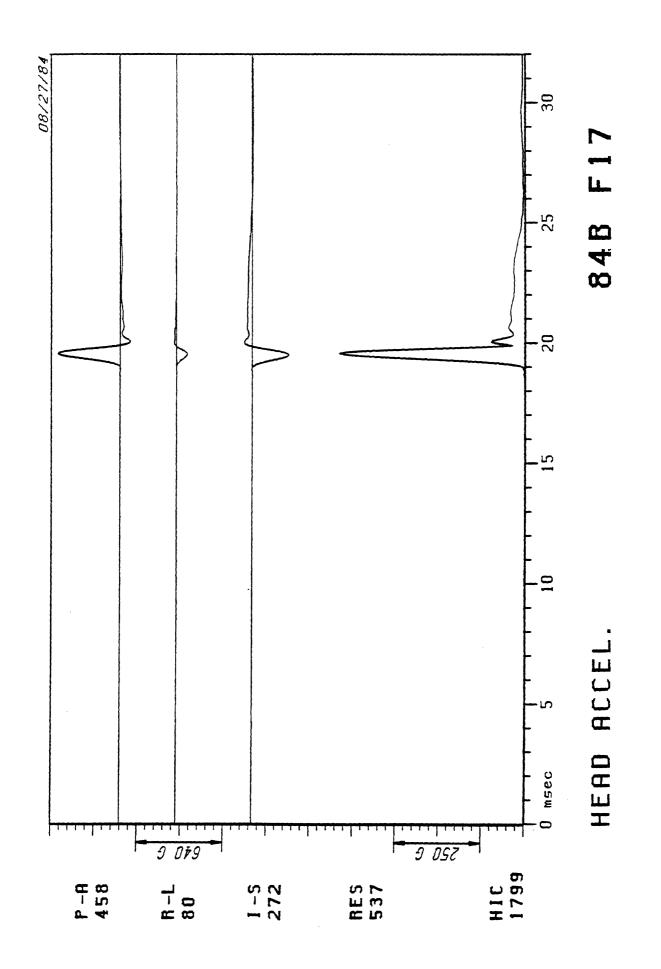
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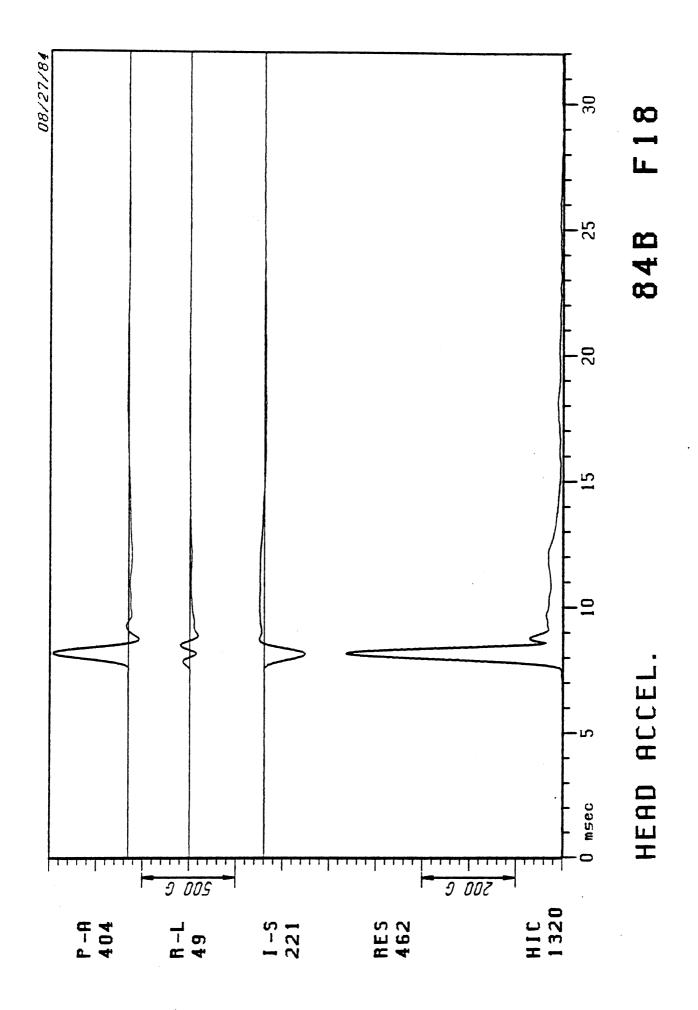


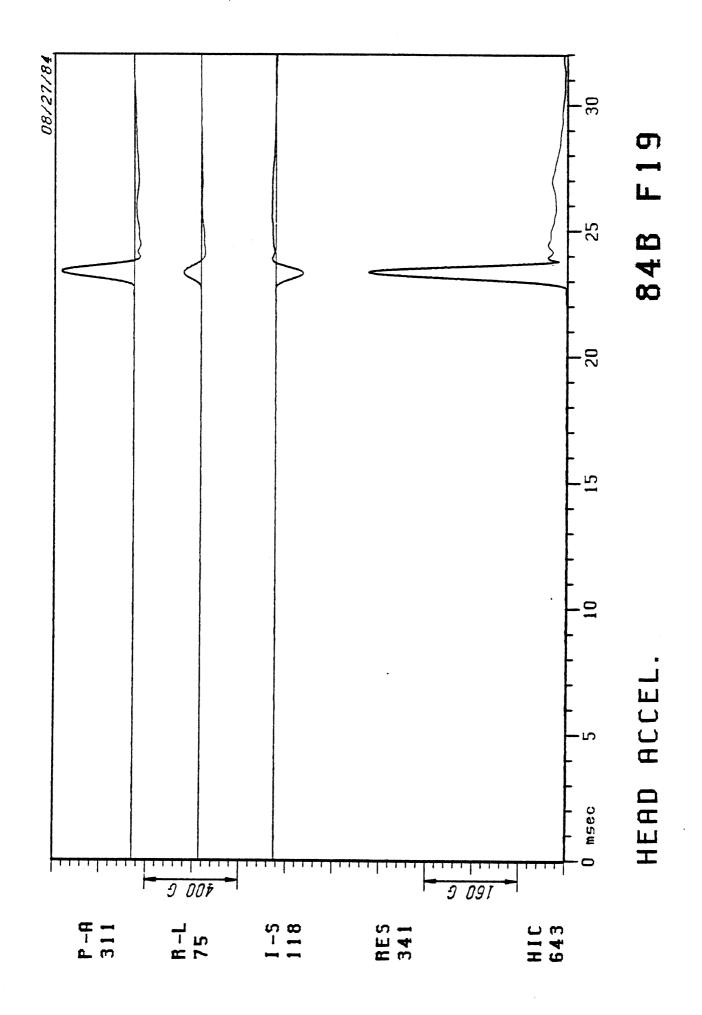


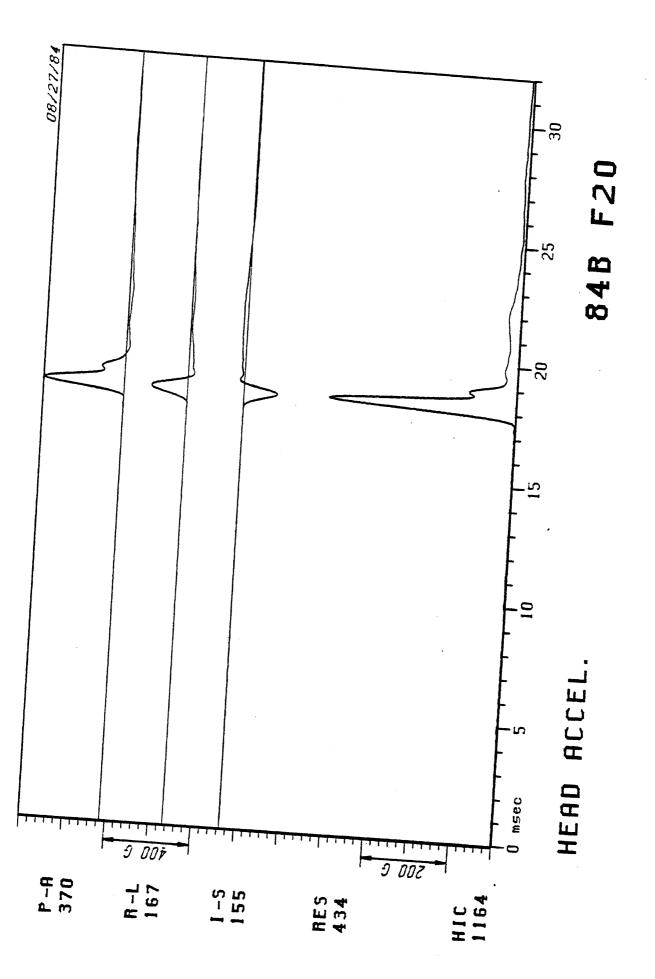


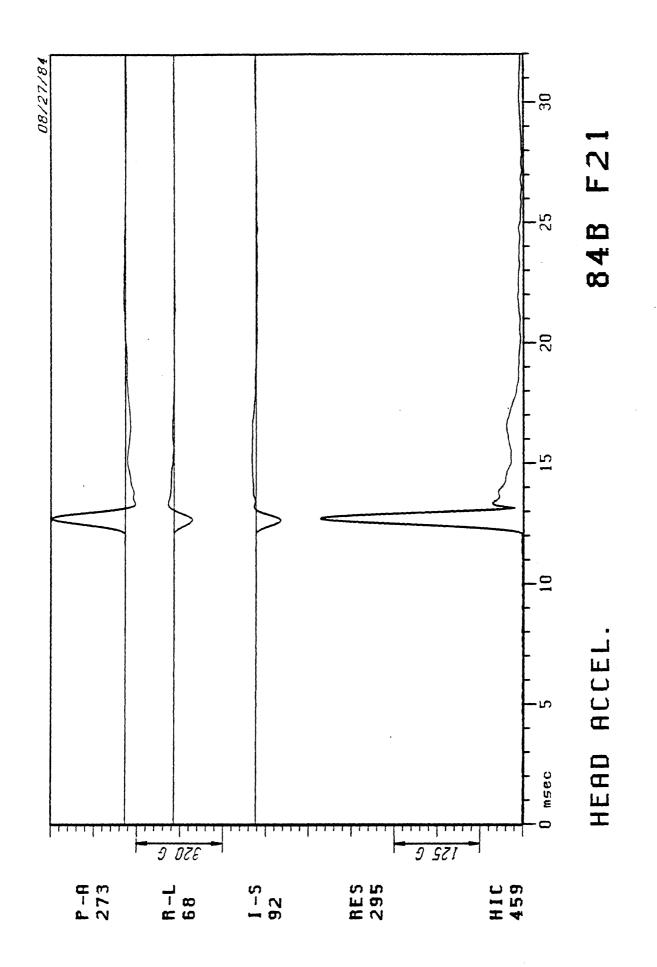


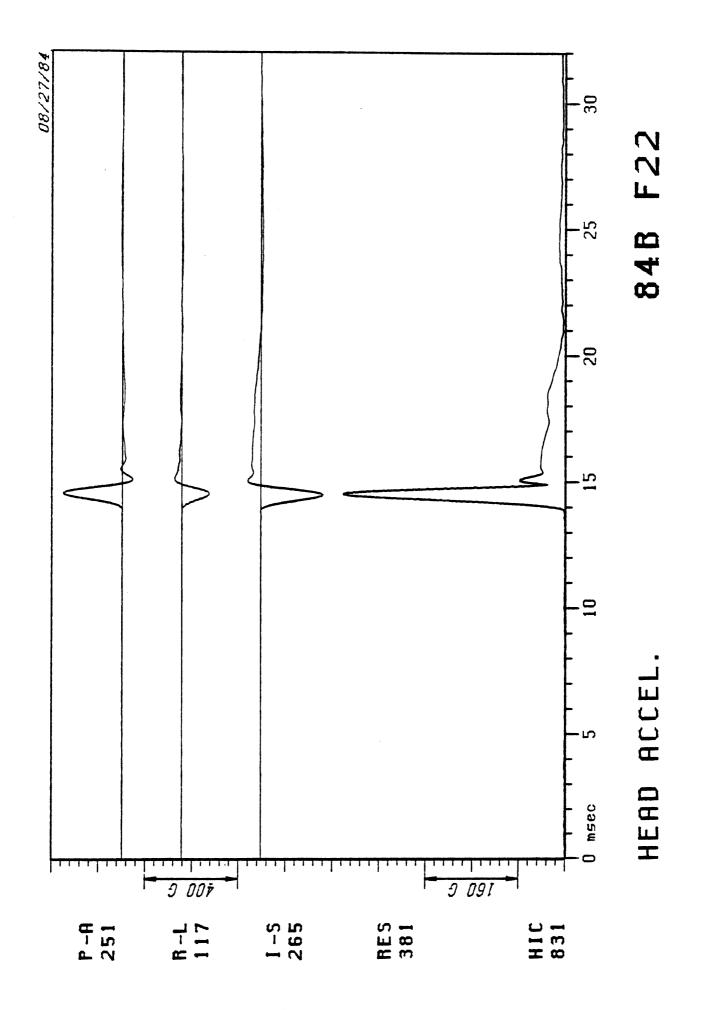


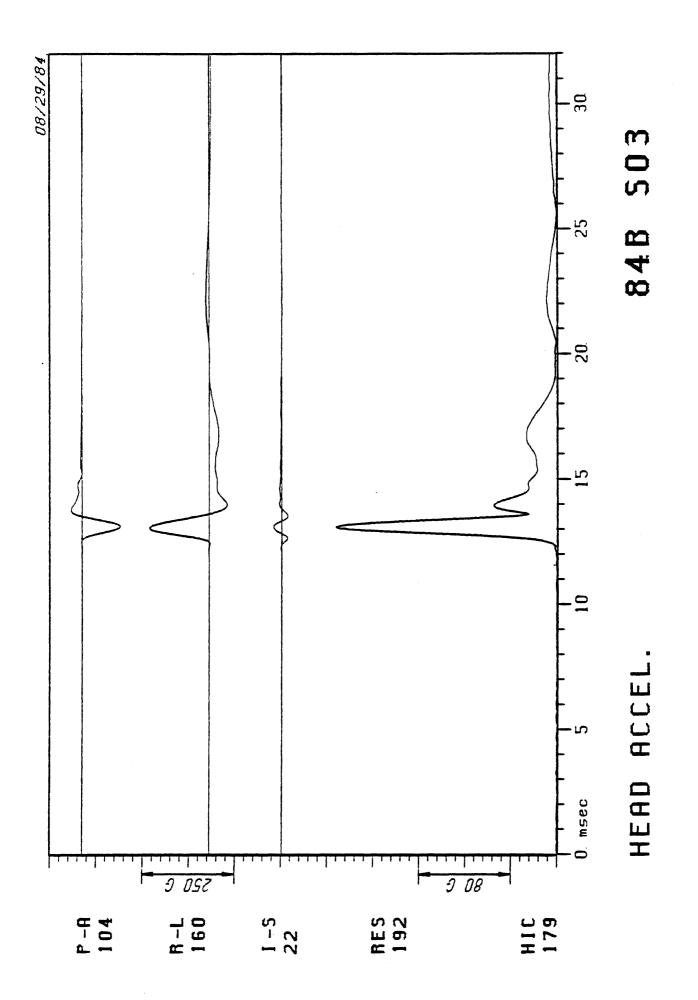


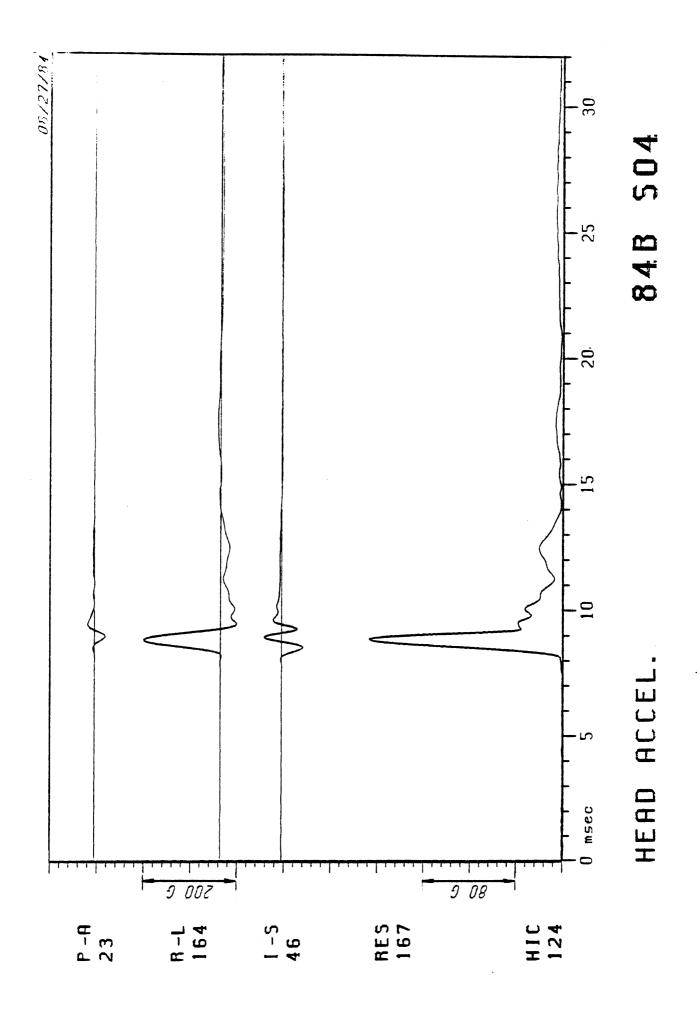


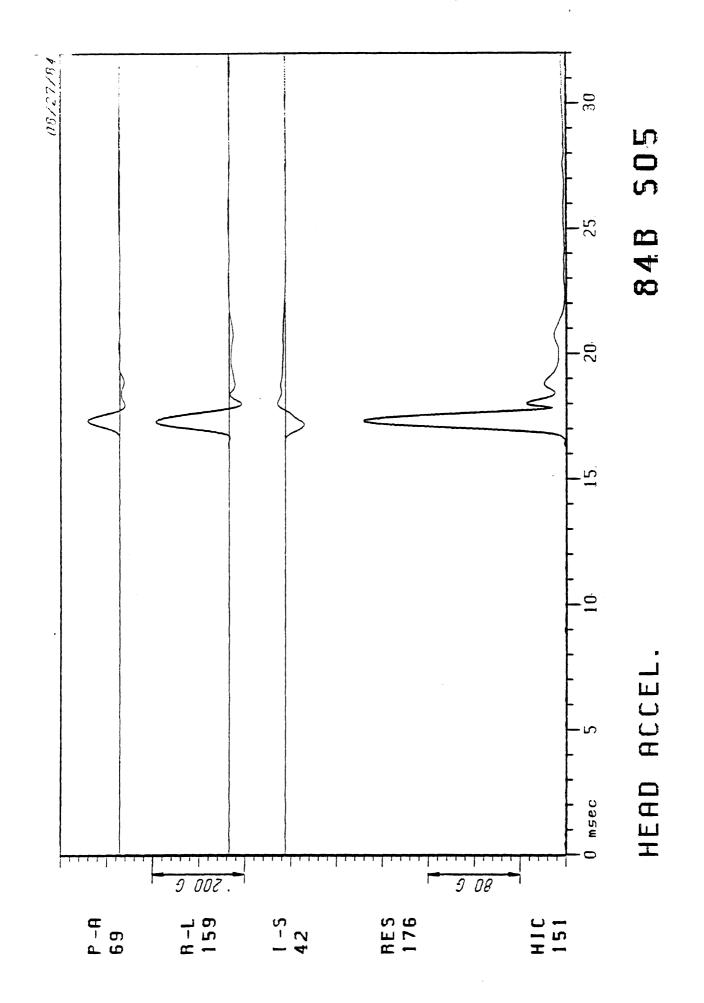


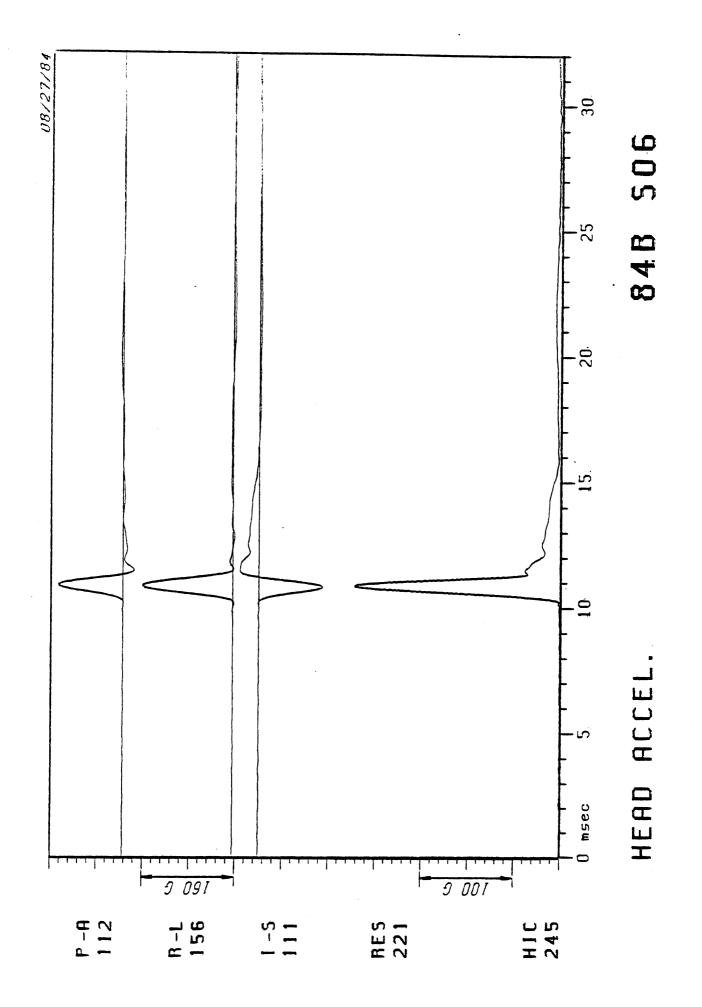


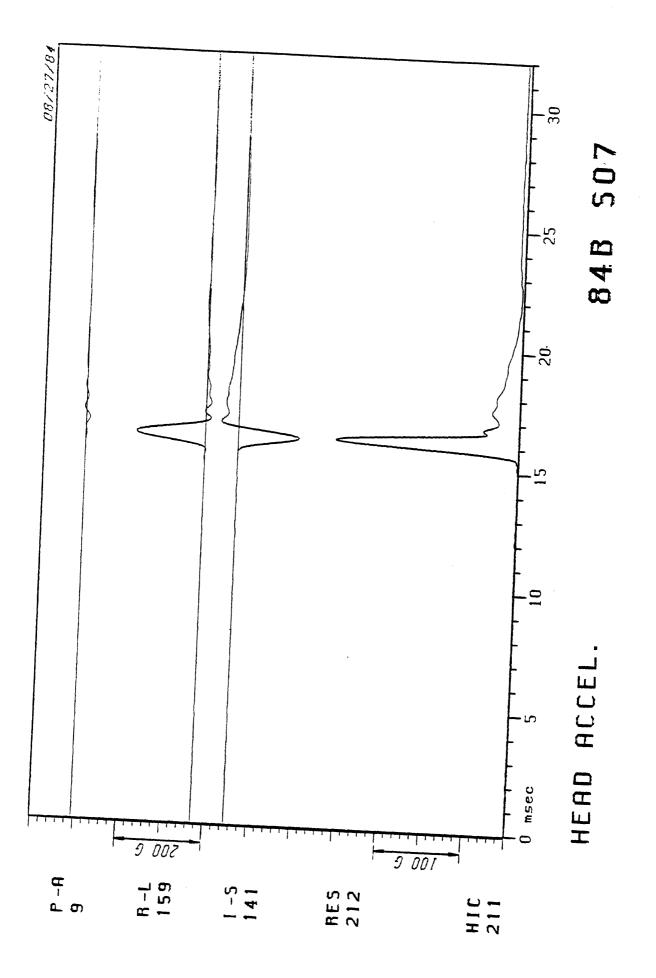


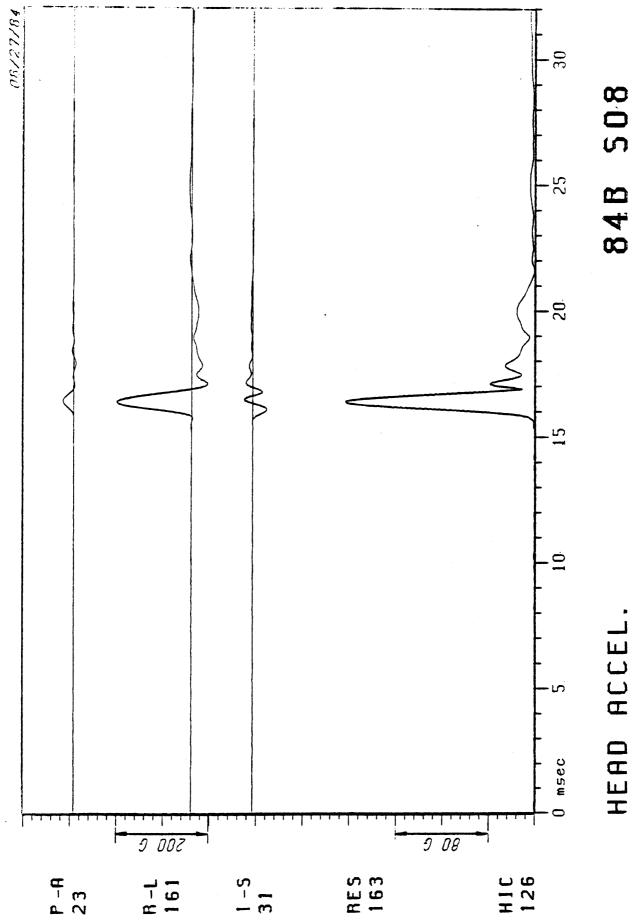


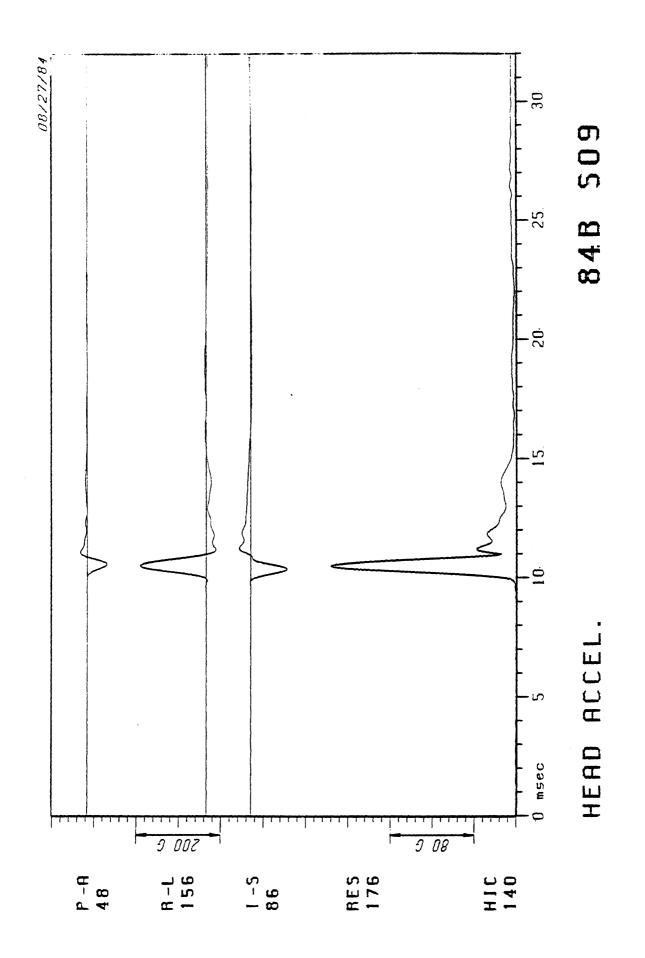


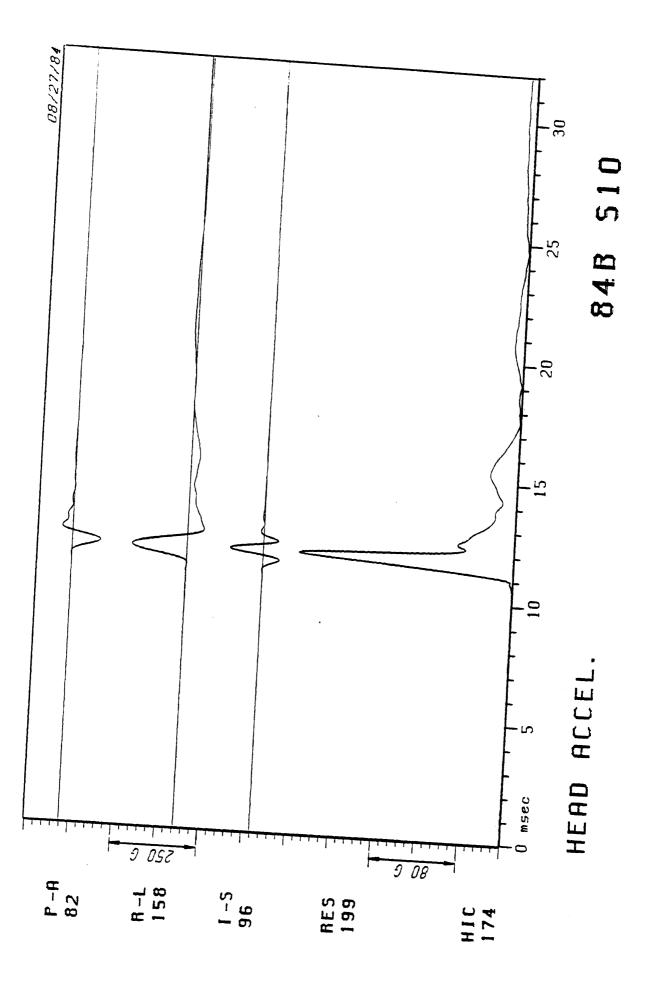


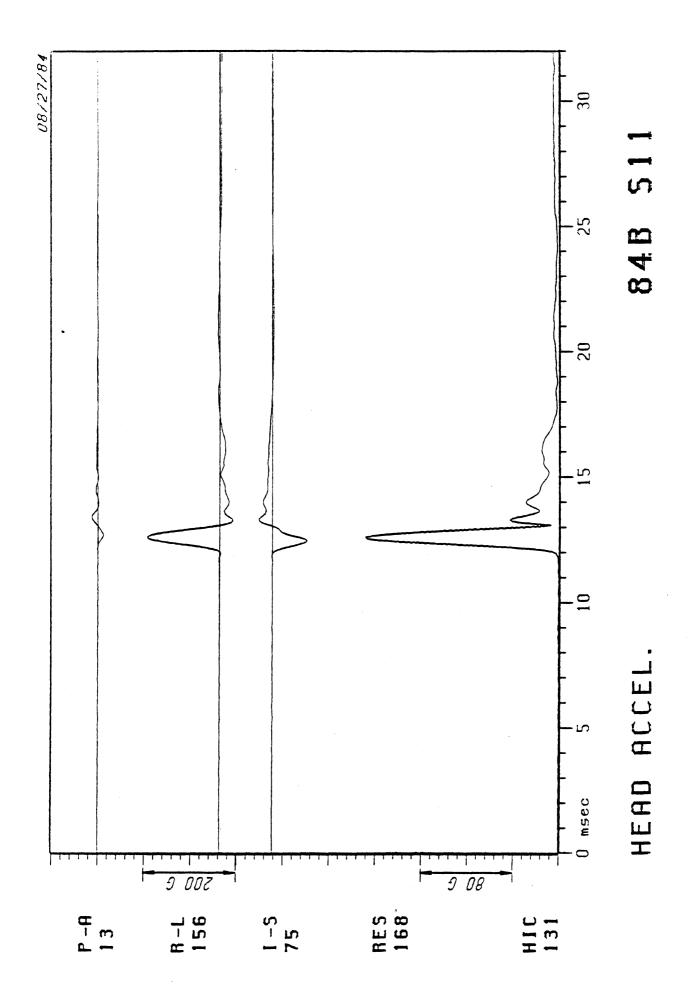


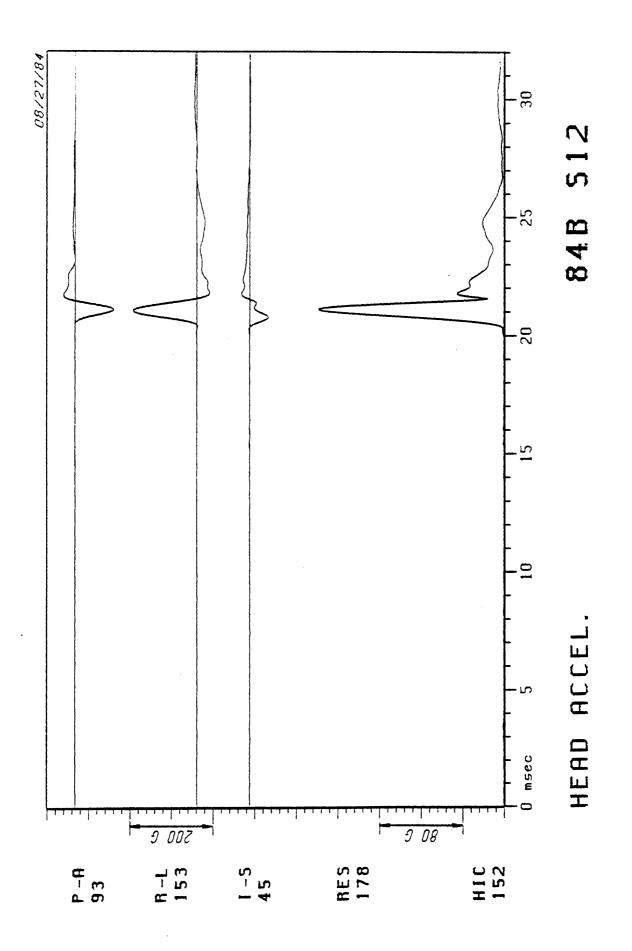








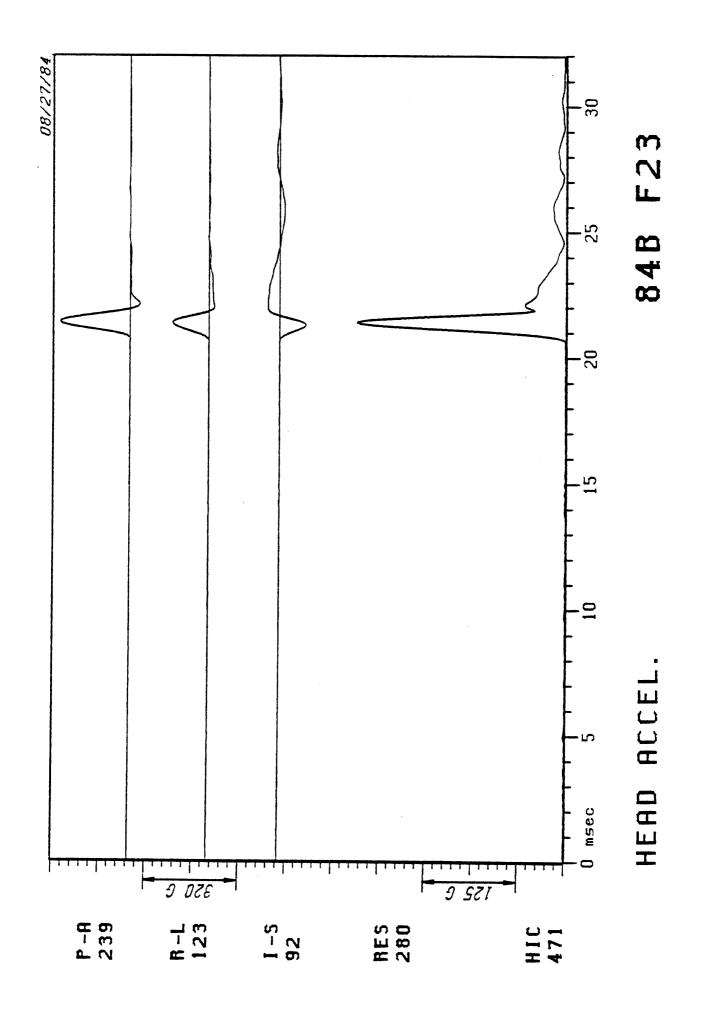


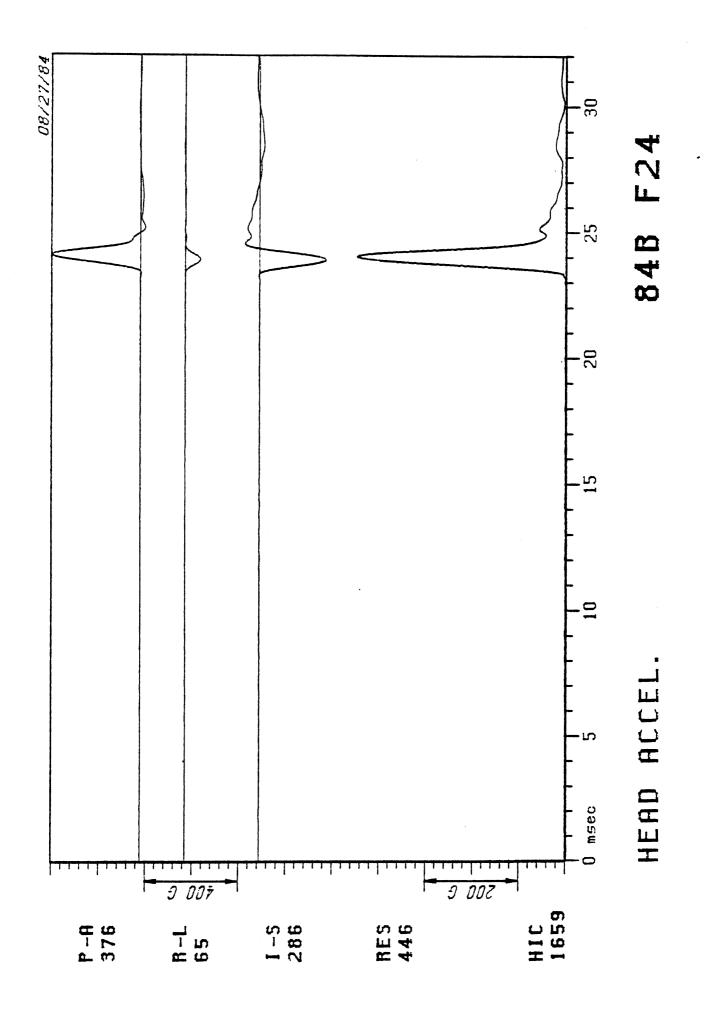


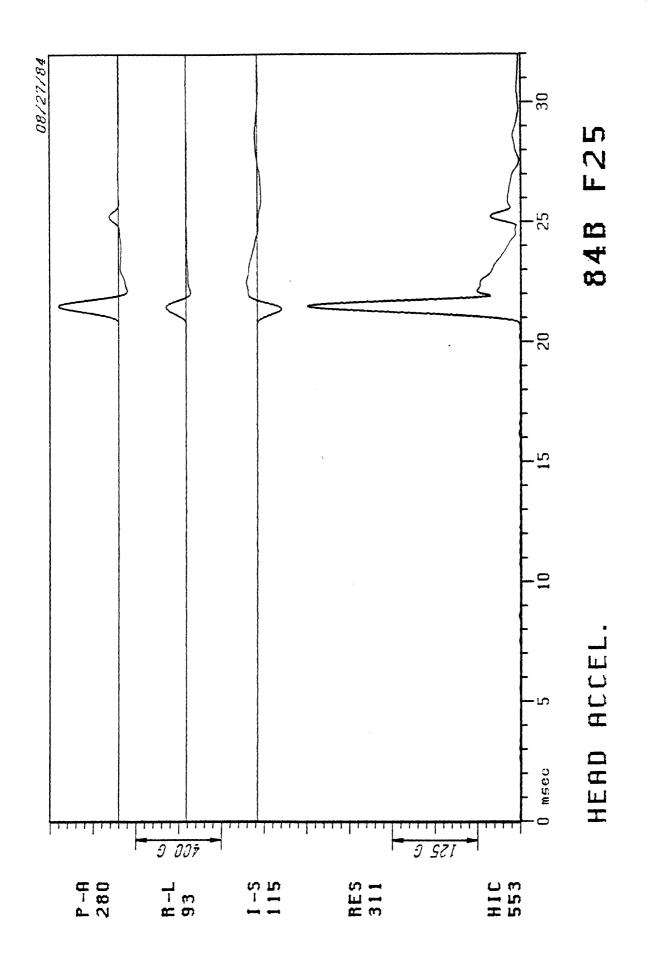
Hybrid III Dummy Results

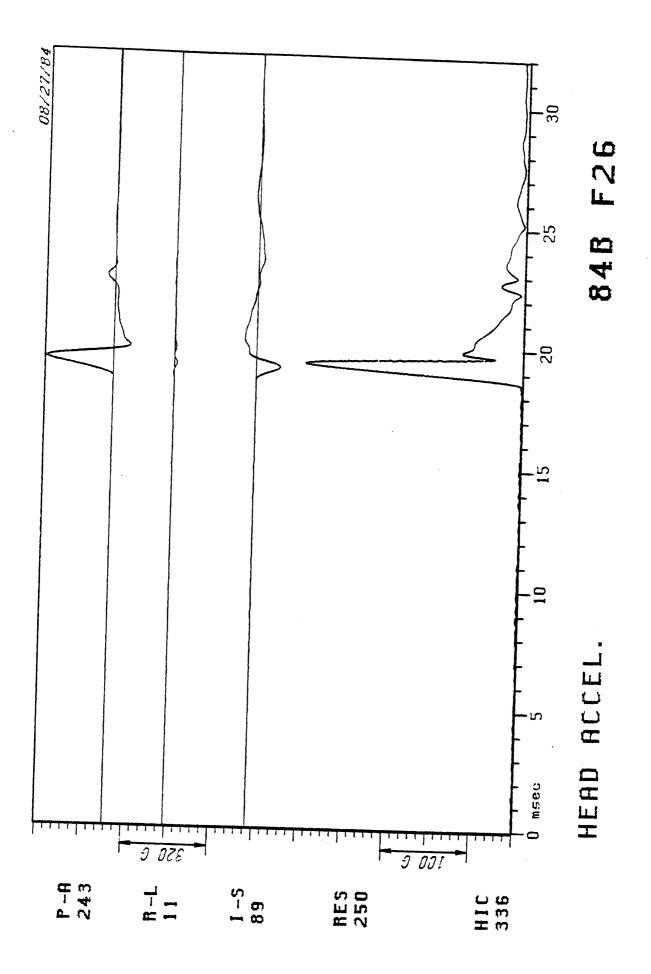
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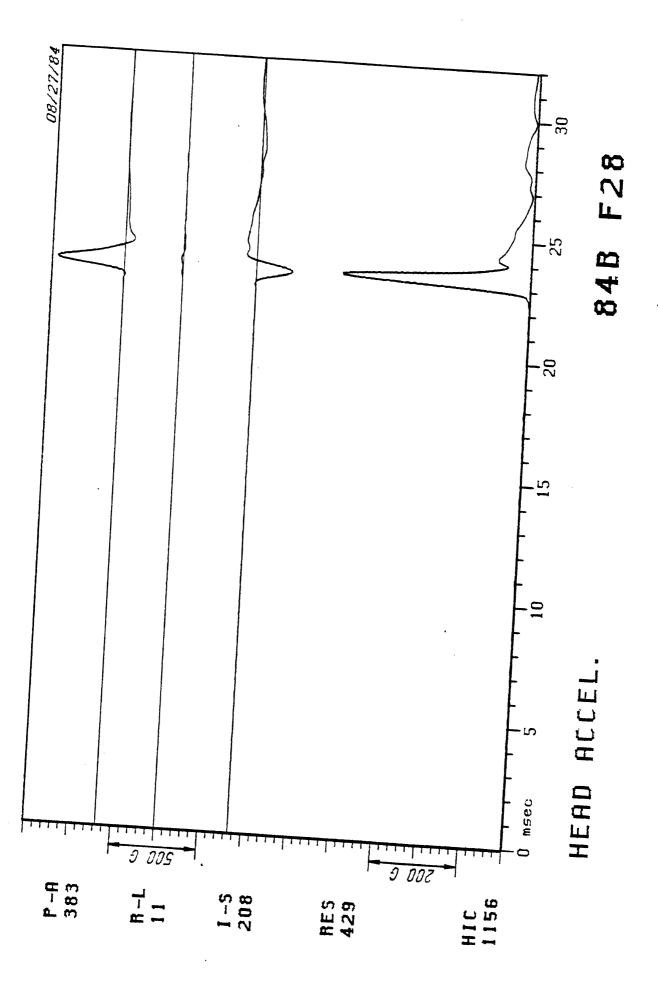
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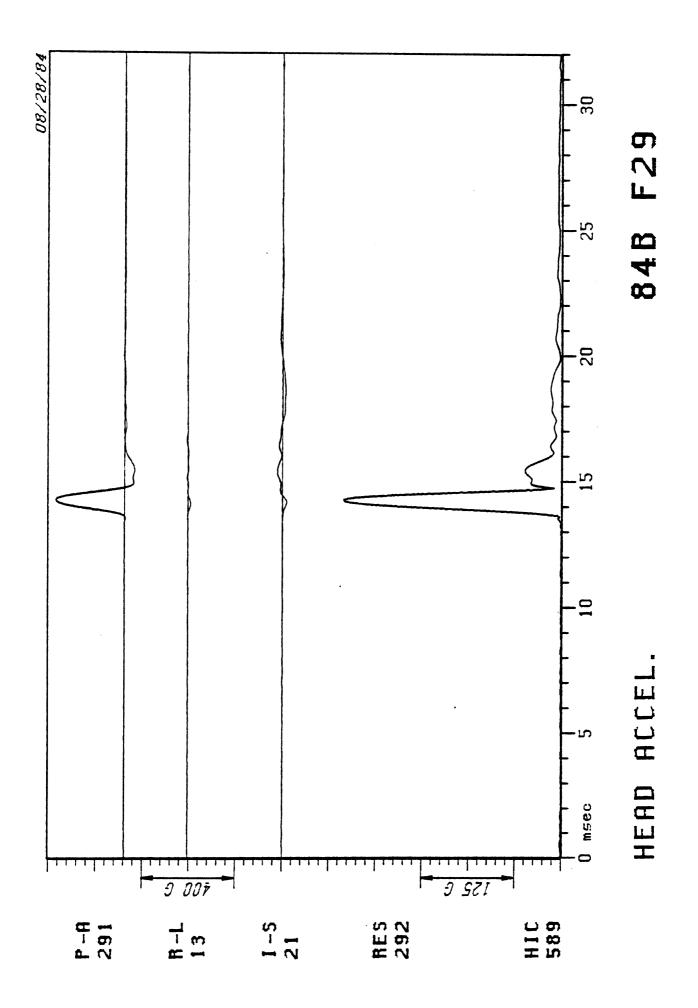


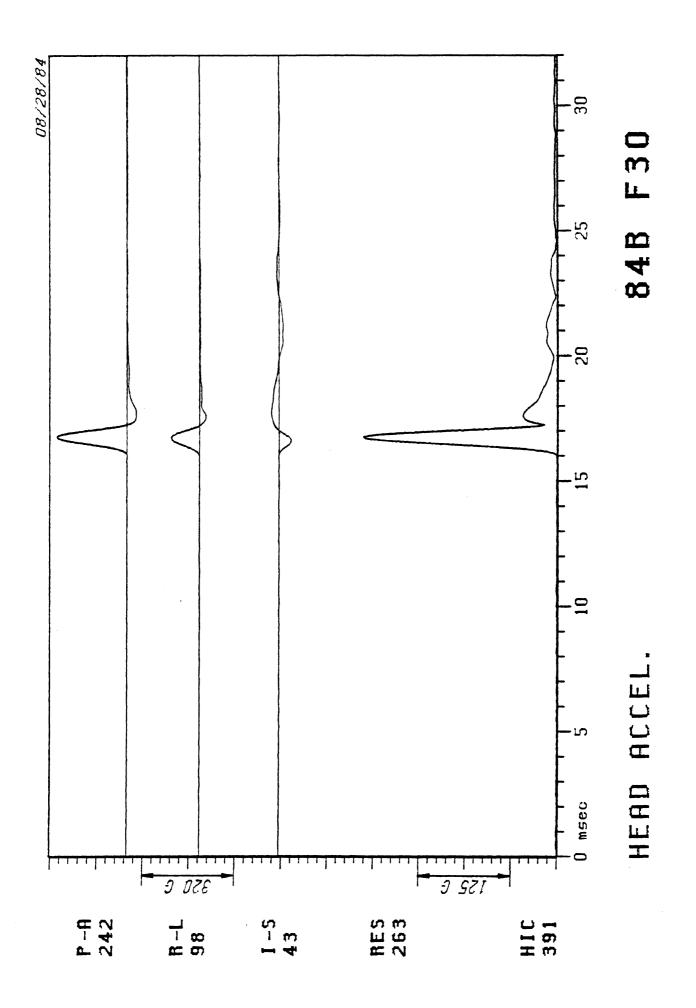


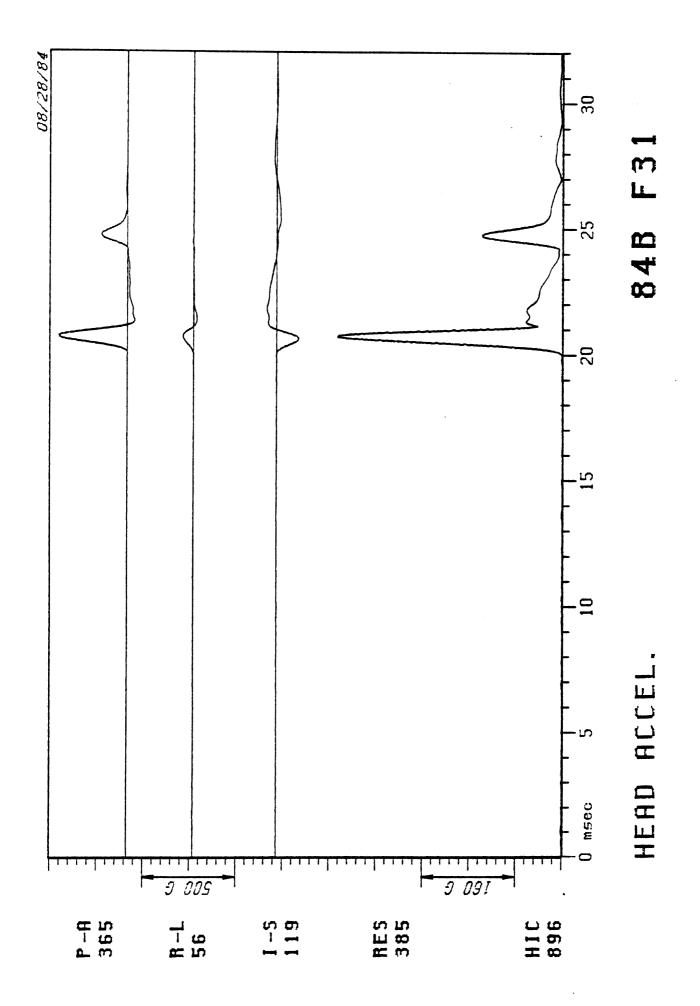


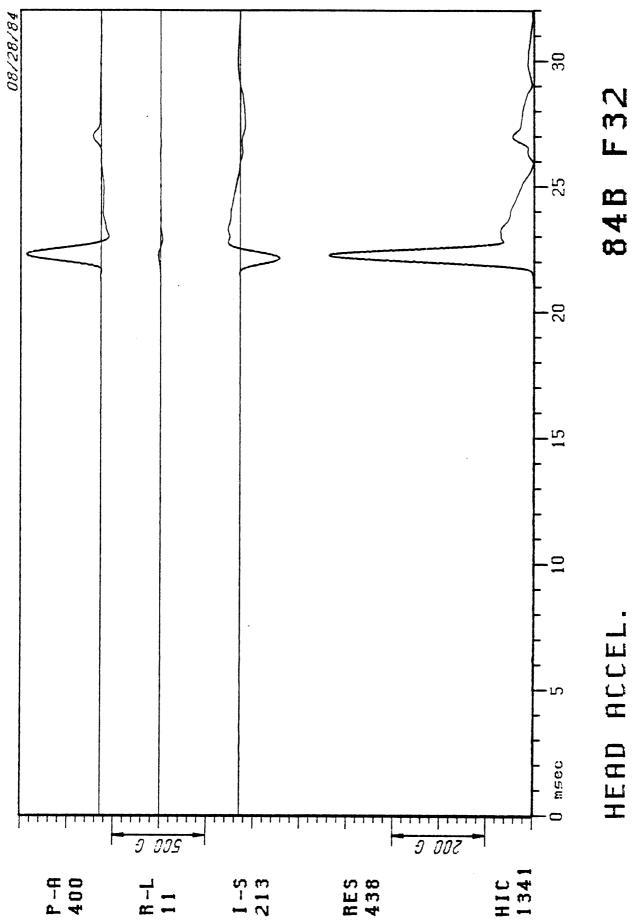


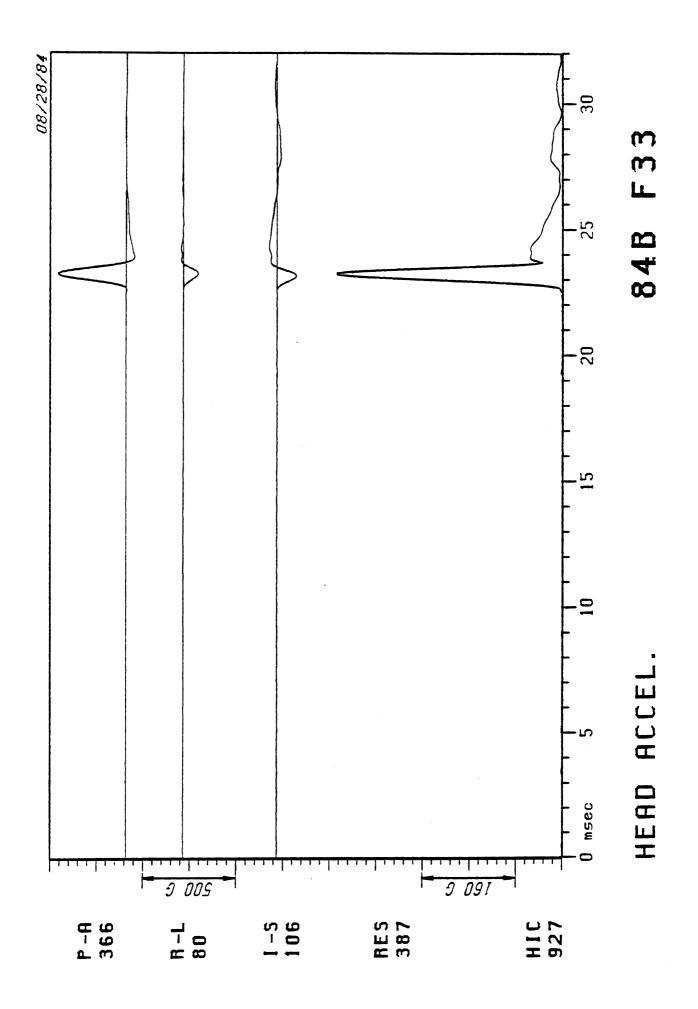


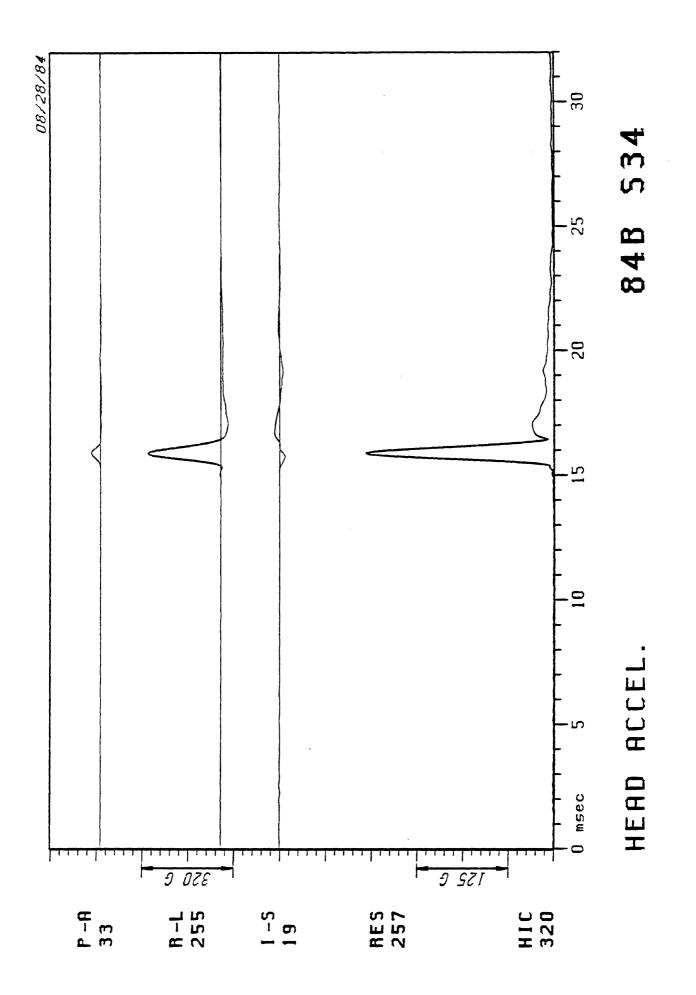


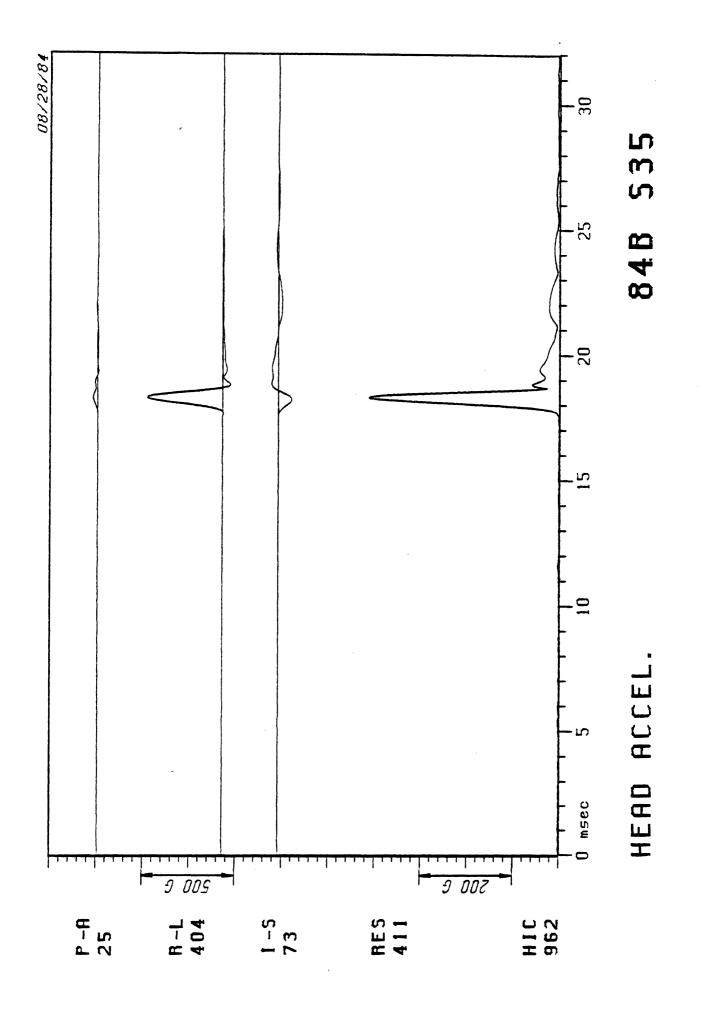


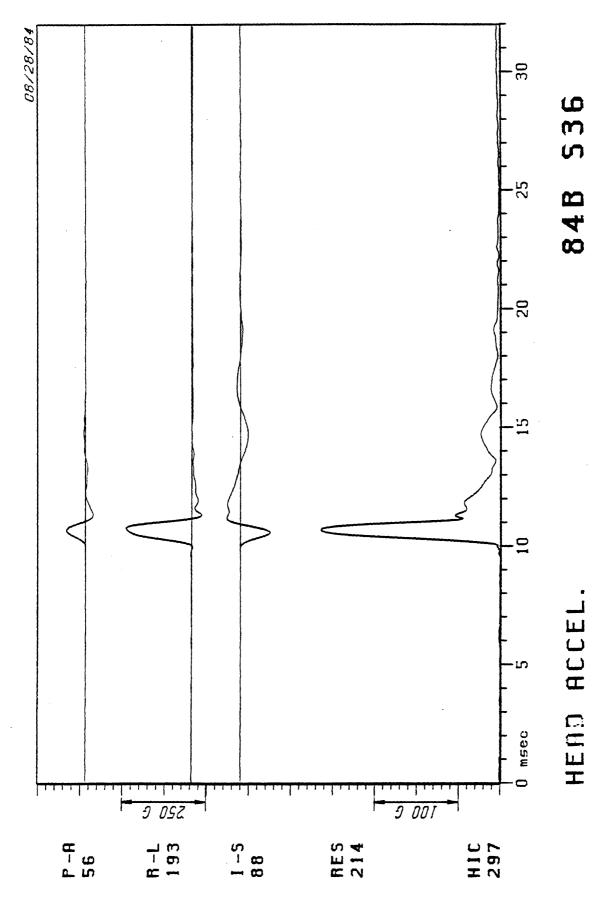


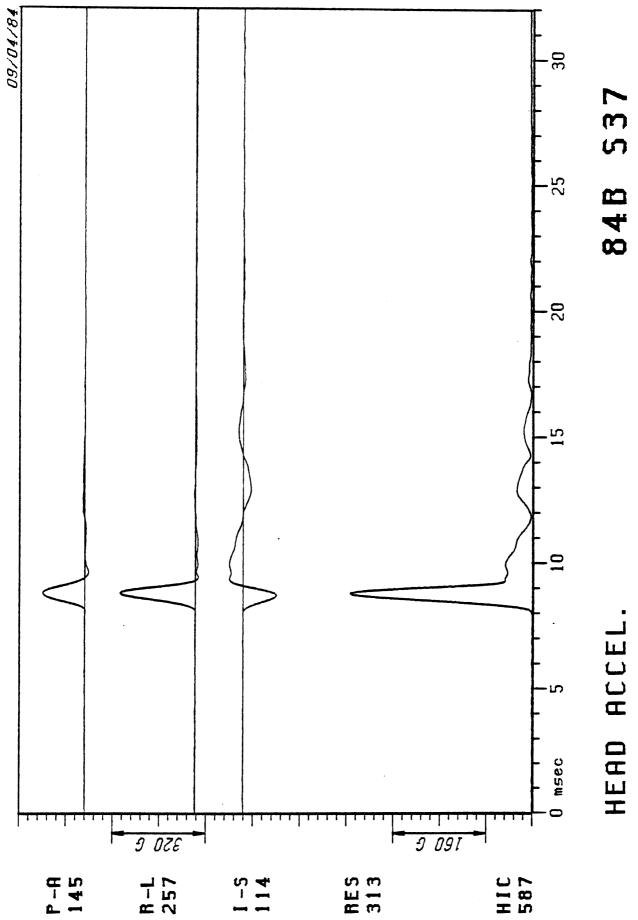


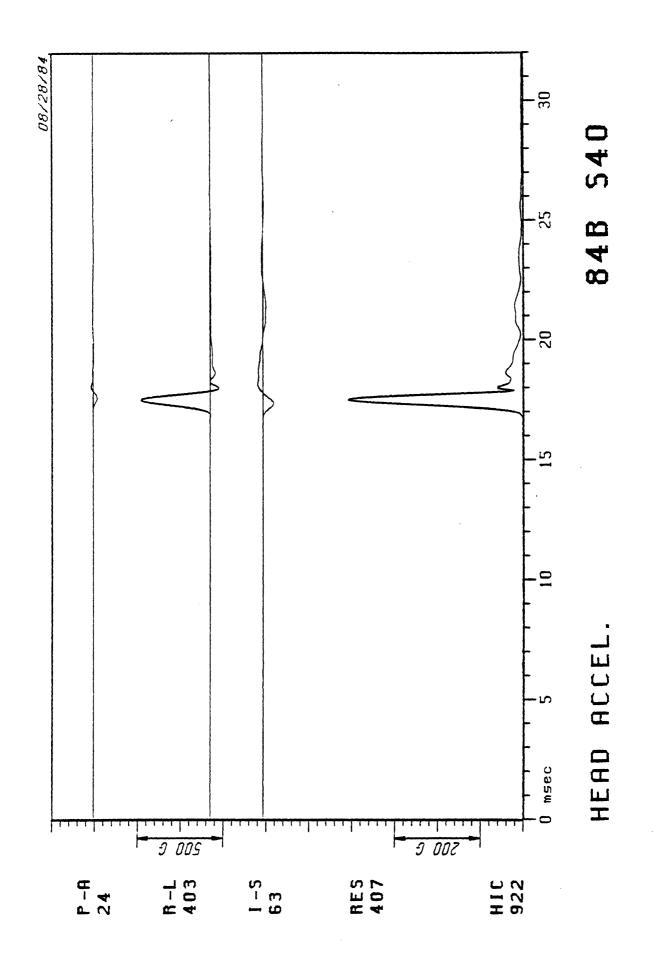


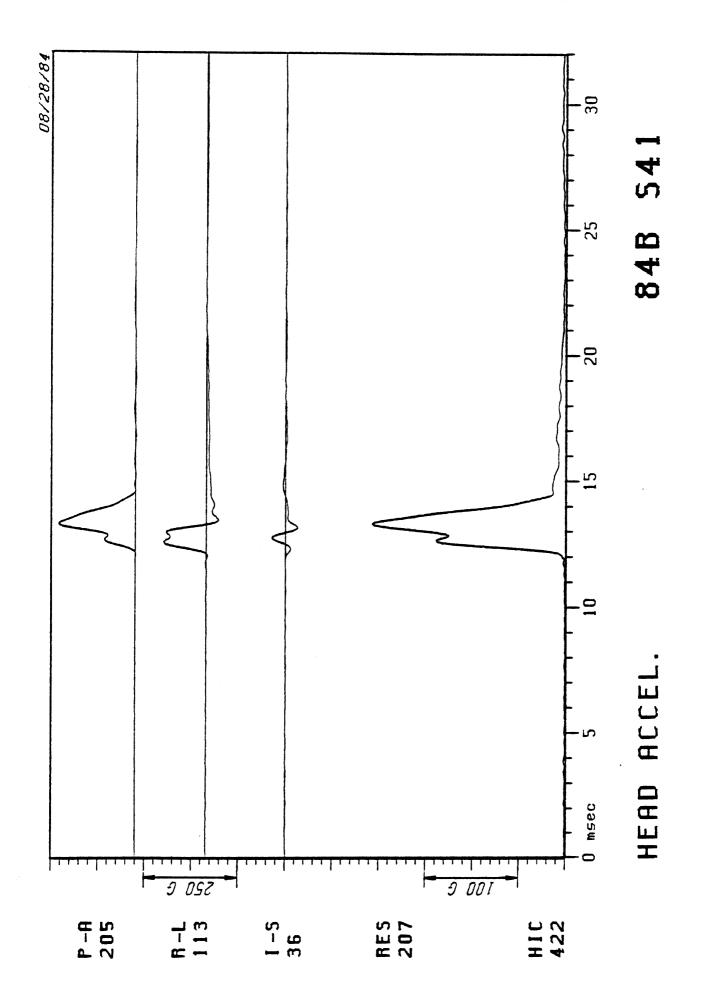


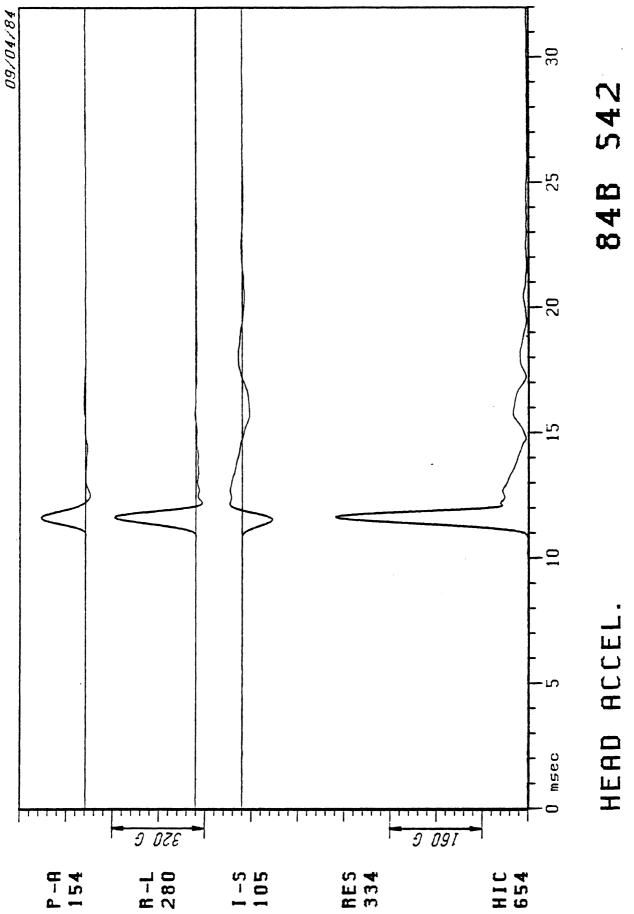


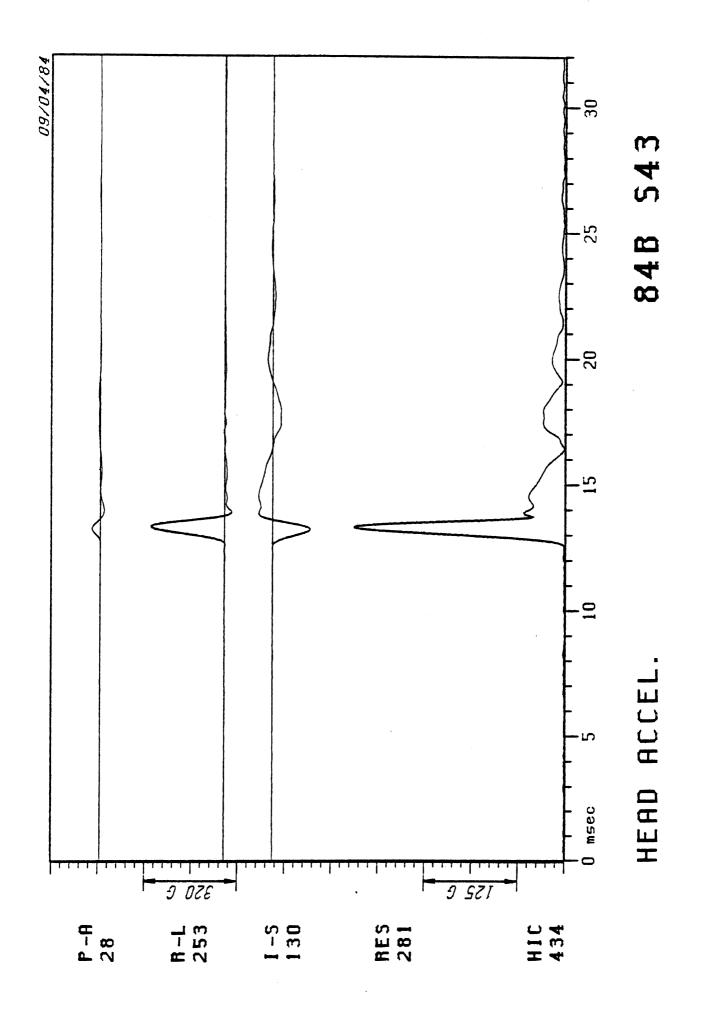


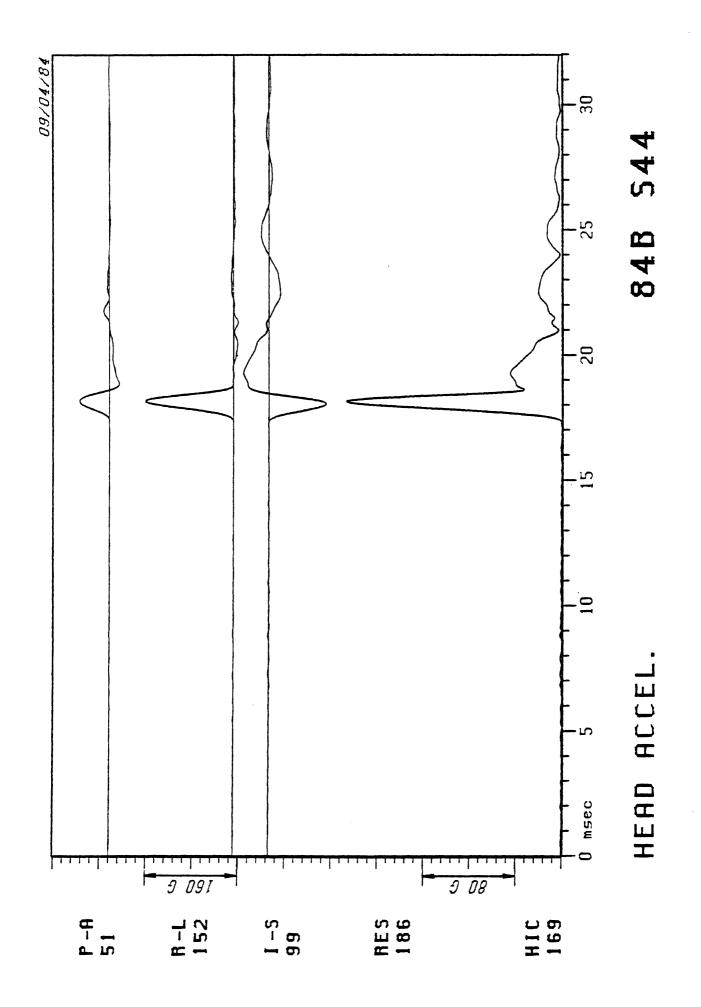


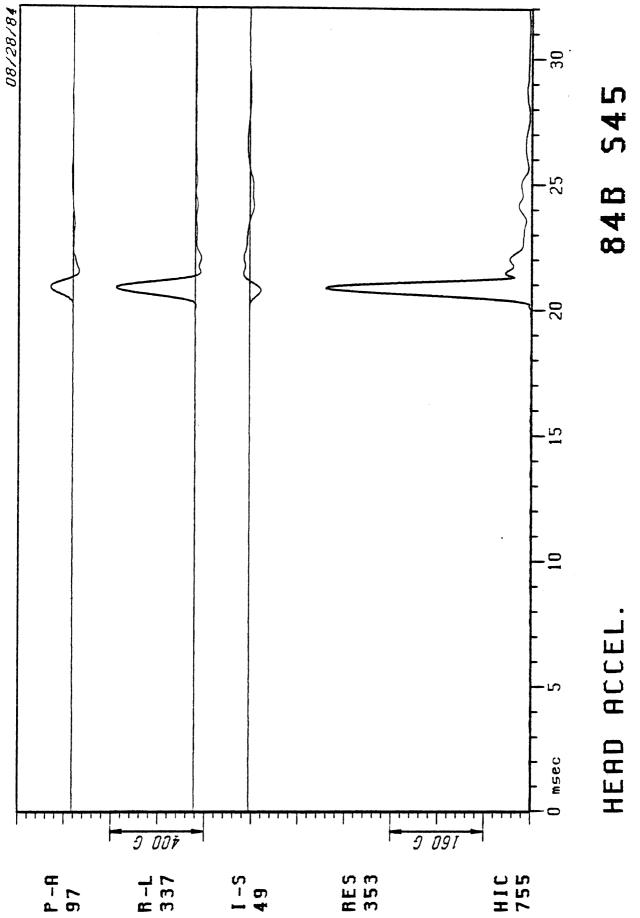






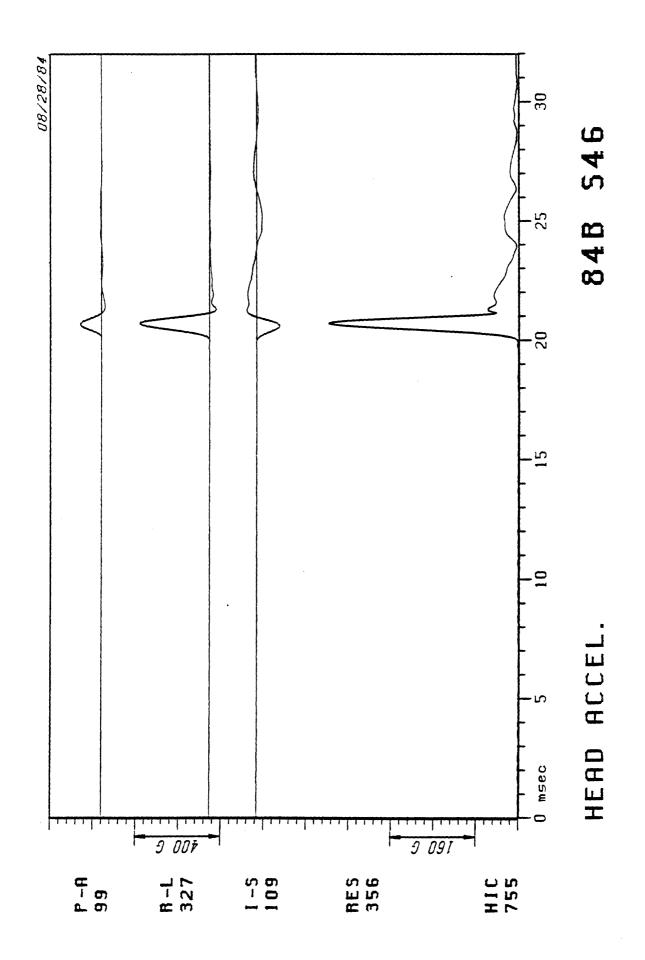


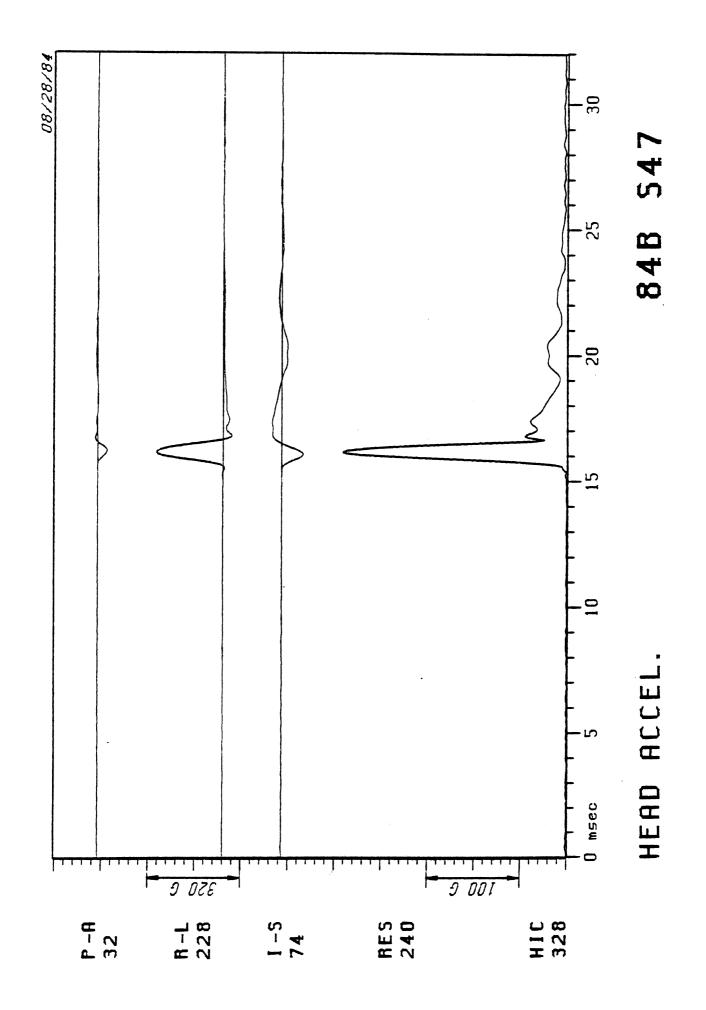












HSRI Dummy Results

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