## Structural and Mechanical Behavior of Layered Zirconium Phosphonate as a Distributed Phase in Polycaprolactone

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**ABSTRACT:** Mixed-surface octyl/methoxyundecyl  $\alpha$ -zirconium phosphonates (ZrPs) were investigated as distributed nanoscale fillers, in concentrations up to 50% w/w, for the purpose of increasing the elastic modulus and yield strength of polycaprolactone (PCL) without a meaningful reduction of its ductility. The volumetric nanoparticle loadings were estimated to be over 70% higher than those in nanocomposites with comparable weight fractions of nanoclay. The mechanical properties of the ZrP/PCL nanocomposite were evaluated with tensile, flexural, and dynamic mechanical testing methods. Nanocomposites containing 5% w/w ZrP showed significant increases in both the ten-

#### **INTRODUCTION**

Ductile thermoplastic additives have been shown to impart as much as an 8-fold improvement in fracture toughness to brittle thermosets while causing moderate reductions in the glass-transition temperature ( $T_g$ ) and elastic modulus.<sup>1,2</sup> For applications in dental restoration, it is highly desirable to toughen a thermosetting system without compromising its elastic modulus. Unfortunately, many thermoplastic polymers with attractive solubility parameters have especially low elastic moduli. Therefore, a means of reinforcing a low-stiffness polyester has been sought for the long-term purpose of toughening acrylic thermosetting resins.

High-aspect, platy nanoparticles or nanoplatelets, such as those derived from layered silicates (LSs), have been studied extensively in the reinforcement of polymeric structures.<sup>3–17</sup> Substantial potential for plastic deformation between nanoplatelets is indicated when the polymer successfully intercalates the nanoplatelet galleries and crystallizes upon solidifi-

sile yield stress and elastic modulus without any loss of ductility versus the unfilled polymer. Layer delamination from the ZrP tactoids was minimal. Kinetic barriers and the strong interlayer attraction between the ZrP surfaces limited intercalative penetration of the ZrP tactoids. ZrP loadings of 20% w/w or more resulted in the agglomeration of tactoids, leading to defect structures with a loss of strength and, at the highest loading, ductility. © 2009 Wiley Periodicals, Inc. J Appl Polym Sci 114: 993–1001, 2009

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cation from the melt.<sup>17</sup> Both intercalated and exfoliated systems of LS can dramatically increase elastic moduli in semicrystalline thermoplastics.<sup>4</sup> The theoretical upper boundary for the elastic modulus is given by a homogeneous dispersion of an exfoliated filler at a low concentration ( $\leq 12\% \text{ v/v}$ )<sup>11,18</sup> at which the degree of stiffening dramatically exceeds that expected from simple rules of mixture.<sup>19</sup> As the LS content exceeds 4% v/v, the rate of the increase in the elastic modulus versus the loading slows because of an increase in the relative proportion of the intercalated filler.<sup>20</sup>

Nonsiliceous nanoplatelets have also been investigated in polymer nanocomposites. In particular, Sue and coworkers<sup>21–23</sup> studied  $\alpha$ -zirconium phosphates as reinforcements for epoxy resin. Mechanically, the materials showed no improvement in fracture toughness over the unmodified epoxy because of facile delamination along the  $\alpha$ -zirconium phosphonate (ZrP) lamellar interface.<sup>22</sup> However, the tensile strength and elastic modulus were increased significantly, whereas the material's overall ductility was maintained; this indicated a high work of fracture.

Ether-functional ZrP materials were first introduced by us<sup>24</sup> as candidate fillers for thermoplastic polyesters. As part of this earlier investigation, the thermodynamics of the polymer host/guest interactions were explored by computer simulation. It has been proposed that the specific surface interactions

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of the inorganic layers within various host polymers are critically important to the enhancement of the elastic modulus because thermodynamic interactions govern both the means of polymer confinement and the polymer morphology within the interlayer galleries.<sup>5,12,17</sup> The outcome of our work<sup>24</sup> suggested that linear polyesters, such as polycaprolactone (PCL), should have favorable energies of mixing, principally through dipole–dipole interactions, by intercalating ZrP systems with mixed octyl and 11methoxyundecyl (MOUD) phosphonate ligands in a 1 : 1 ratio.

PCL is a highly crystalline polymer with high ductility and a low elastic modulus. The material is easily capped with diverse organic functionalities,<sup>25</sup> and its adaptability makes it attractive for eventual inclusion in toughened dental acrylic polymers.

Octyl/MOUD ZrP was synthesized with slight modification of the conventional method;<sup>26</sup> layered nanoplatelets were produced in a relatively high yield with few dislocation defects. PCL nanocomposites were formulated with a range of filler levels to determine the effects of the particle loading on the static and dynamic mechanical properties. The structure–property relationships are discussed accordingly.

#### **EXPERIMENTAL**

Reagents and solvents were used as purchased, without further purification, unless otherwise noted. PCL pellets (number-average molecular weight = 80,000 g/mol; Aldrich, St. Louis, MO) were cryogenically ground into a coarse powder (1-mm grain size) with a Retsch (Newtown, PA) mill by the direct addition of liquid nitrogen. Room temperature was  $20 \pm 1^{\circ}$ C. 11-Methoxyundecyl phosphonic acid was prepared as previously described by Furman.<sup>27</sup>

## Synthesis of the octyl/MOUD ZrP nanoplatelets

In a typical reaction, in air, 4.3 mmol of ZrOCl<sub>2</sub>. 8H<sub>2</sub>O (98%; Aldrich) was added to 30 mL of deionized water in a polytetrafluoroethylene digestion vessel (Savillex Corp., Minnetonka, MN) equipped with a polytetrafluoroethylene condenser and a magnetic stirring bar. Concentrated aqueous HF (48% w/w; Aldrich) was then added so that [F]/[Zr]equaled 8. After a few minutes of stirring, octylphosphonic acid (98%; Lancaster; 6.5 mmol) and MOU-DOA (6.5 mmol) powders were added to the previously acidified solution so that [P]/[Zr] equaled 3. An additional 35 mL of water was added, and the two-phase reaction mixture was heated over a 70°C oil bath for 1 week with stirring. The final product was isolated by filtration and washed with 120 mL of ethanol; a poly (ether sulfone) membrane-type filter with a pore size of 0.2  $\mu m$  was used. The yield was 91%.

Approximately 2.2 g of ZrP was dispersed in 100 mL of ethanol containing 0.3 g of a 20% tetraethyl ammonium hydroxide (TEAH) solution to neutralize  $\equiv$ PO<sup>-</sup> groups present from deprotonated dangling bonds along the edges of the nanoplatelets. The suspension was sonicated for a total of 20 min with a horn-type sonicator with 39-W power delivery (Microson XL2020, Misonix, Inc., Farmingdale, NY). After sonication, the suspended material was centrifuged, and the supernatant was poured away. The treated ZrP was dried in a vacuum oven at 120°C for 12 h.

# Preparation of the experimental composites: the counter-rotating centrifuge method

A dry mixture of the ground PCL, totaling 4 g, was formulated with up to 20% w/w TEAH-treated ZrP by agitation in a SpeedMixer (Flack Tek, Landrun, SC) at 1800 rpm. A small amount of acetone (ca. 2 mL) was then added to soften the polymer. The softened mixture was remixed with the SpeedMixer at 3500 rpm for a total of 5 min. The solvated composite was then dried at 60°C under a house vacuum. Finally, the composite was heated to 120°C and quickly transferred to the SpeedMixer for final blending at 3500 rpm.

## Compounding extrusion method

The ground PCL resin was dry-mixed with ZrP for 2 min at 2400 rpm with the SpeedMixer. Melt compounding was performed with a twin-screw extruder (MiniLab microcompounder, Thermo-Haake, Waltham, MA) with a rotational speed of 30–50 rpm. The screw and backflow chambers were filled with a total of 6 g of material. The free-flowing dry premix was added directly to the extruder hopper and circulated through the screw and backflow chambers at 110°C for 25 min. Fibers were drawn from the extruder in air through a 1.25-mm orifice onto a motorized spool, and the remaining material was recovered from the flow chambers after thermal quenching.

## Characterization: tensile mechanical testing

Extruded fibers were cut into sections approximately 15 cm long. The specimens were individually mounted onto a Sintech 20/G electromechanical test frame (MTS Systems, Eden Prairie, MN) via rubberized pneumatic grips. The specimens were tested in uniaxial tension with a 102-mm gage length, a 111-N load cell, and a 508 mm/min crosshead speed. Ductile specimens were extended until the limits of the test frame were reached. The temperature and relative humidity of the ambient test environment were  $25^{\circ}$ C and  $35^{\circ}$ , respectively.

#### Flexural mechanical testing

Rectangular beam specimens, nominally  $2 \times 2 \times 52$  mm<sup>3</sup>, were formed from the previously extruded fibers. The fibers were compressed in a stainless steel slot mold under an external load of 20,000 N while being heated to 135°C. The molded specimens were released and cut in half before testing, in three-point bending, with the Sintech 20/G electromechanical test frame and a support span of 18 mm.

Single-edge notched beams (SENBs; ASTM E 1820) were prepared by precracking of the standard test beams to a nominal depth of 1 mm with a new razor blade. They were tested under three-point bending to failure with a crosshead speed of 5 mm/min and a 111-N load cell. Elastic moduli were determined for unnotched specimens with the same crosshead speed and an 11-N load cell.

#### Dynamic mechanical analysis (DMA)

Rectangular beam specimens, nominally  $2 \times 2 \times 18$  mm<sup>3</sup>, were tested in three-point bending with a DMA 7 (PerkinElmer, Waltham, MA) with a test span of 15 mm. A fixed load of 110 mN and a dynamic load of 100 mN were applied. For temperature scans, the dynamic loading frequency was 1 Hz. Frequency scans were performed from 1 to 51 Hz at 21°C. The specimen chamber was purged continuously with nitrogen gas at a flow rate of 30 mL/min. An internal block temperature of  $-52^{\circ}$ C was maintained by refrigeration.

#### Differential scanning calorimetry (DSC)

Thermal scans were performed with a Pyris 1 differential scanning calorimeter (PerkinElmer) with a nitrogen purge flow of 30 mL/min. Specimens (10– 20 mg) of PCL and ZrP-filled PCL were tested in triplicate with a thermal cycle from 20 to  $120^{\circ}$ C at a ramp rate of  $40^{\circ}$ C/min.

## Thermogravimetric analysis (TGA)/dynamic thermal analysis

Thermal analysis was performed with a Q-series SDT-600 differential scanning calorimeter/thermogravimetric analyzer (TA Instruments, New Castle, DE). The samples, weighing approximately 10 mg each, were preconditioned at 100°C under a 100 mL/min flow of dry air. Burnout experiments were conducted in air with a temperature ramp from 100 to 1100°C at a ramp rate of 10°C/min. The materials were then held at 1100°C for 30 min to ensure complete oxidation.

#### X-ray diffraction (XRD)

XRD patterns were obtained with a D8 Advance analytical diffractometer (Bruker AXS GmbH, Karlsruhe, Germany) equipped with a Cu K $\alpha$  radiation source, a 1.0-mm fixed-divergence slit, a Johansson focusing monochromator, and a standard scintillation detector with a 0.1-mm slit. The source was operated with an acceleration voltage of 36 kV and a filament current of 20 mA. The scan rate was set to 5 s/step with a step size of  $\theta = 0.025^{\circ}$ .

#### Transmission electron microscopy (TEM)

Electron micrographs were obtained on a JEOL 1230 apparatus (JEOL, Ltd., Tokyo, Japan) equipped with an LaB<sub>6</sub> electron gun and operated at 80 kV. Images were acquired with a charged coupling device camera system (AMT Corp., Danvers, MA). A catalase crystal standard (Ted Pella, Redding, CA) was also imaged to provide an internal reference *d*-spacing of 8.75 nm. Fast Fourier transform filtering of the images was performed with the ImageJ image-processing package from the National Institutes of Health (http://rsb.info.nih.gov/ij). Simulated diffraction spots in the Fourier power spectra were compared with those of the catalase crystal, with a known spacing, to yield experimental *d*-spacings for the nanoplatelet layers.

#### **RESULTS AND DISCUSSION**

#### ZrP composition

Layered octyl/MOUD ZrP was produced through a  $ZrF_6^{2-}$ -mediated condensation reaction similar to that used by Alberti et al.<sup>26</sup> The isolated material had an (001) layer spacing of 28.4 Å, as determined by XRD. The ceramic yield (52.7% w/w) was within 1% of the theoretical value [51.7% w/w Zr(O<sub>3</sub>-POH)<sub>2</sub>], which was within the experimental error.

The theoretical density ( $\rho$ ) of octyl/MOUD ZrP could be deduced from the monoclinic unit cell values with the following formula:

$$\rho = \frac{ZM}{N(a \times b)c \, \sin\beta}$$

where *Z* is the number of formula units per unit cell; *M* is the formula weight; *N* is Avogadro's number; *a*, *b*, and *c* are lattice parameters; and  $\beta$  is the angle between the *a* and *b* unit cell axes. *a* and *b* for organic zirconium phosphonates could be estimated from zirconium bisphenyl phosphonate: *a* = 9.0985 Å and *b* = 5.4154 Å ( $\beta$  = 101.333°).<sup>28</sup>

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**Figure 1** TEM micrographs of TEAH-treated ZrP after speed mixing in molten PCL: (a) hexagonal tactoid faces, (b) tactoid edges (ca.  $20 \times 100 \text{ nm}^2$ ), (c) resolved tactoid layers, and (d) a delaminated layer pair viewed edge-on.

Meanwhile, *c* was equal to  $2d_{(001)} = 56.8$  Å. Each unit cell contained four formula units<sup>29</sup> with an average composition of CH<sub>3</sub>(CH<sub>2</sub>)<sub>7</sub>PO<sub>3</sub>ZrO<sub>3</sub>(CH<sub>2</sub>)<sub>11</sub> OCH<sub>3</sub>, which had a formula weight of 547.72 g/mol. Therefore, the density of octyl/MOUD ZrP was estimated to be 1.33 g/cm<sup>3</sup>.

Edge charges from dangling phosphoryl anions pose a potential kinetic barrier to polymer intercalation in ZrP. Therefore, TEAH pretreatment was performed on all ZrP materials before blending with PCL.

### Nanocomposite morphology

After TEAH pretreatment, the ZrP powder was blended at 20% w/w in PCL (weight-average molecular weight = 80,000 g/mol) via the SpeedMixer method. The composite showed limited evidence of delamination under TEM (Fig. 1), although the vast majority of the layers remained bound together in the tactoids (Fig. 2). XRD showed an average interlayer *d*-spacing of 27.8 Å with no indication of polymer intercalation or exfoliation (Fig. 3). The majority



**Figure 2** Agglomeration of tactoids at the 20% w/w level in extruded ZrP/PCL.

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Intensity (Arbitrary)

0

PCL

5% ZrP/PCL

20% ZrP/PCL

ZrP

30

40



20

**2**θ(°)

28.4Å

10

of nanoplatelets remained clustered into tactoids containing 7–10 individual layers with dimensions of about 20  $\times$  100 nm<sup>2</sup> [Fig. 1(b)]. Fast Fourier transform filtering was applied to four different high-resolution TEM images, providing a conservative estimate for the average intralayer *d*-spacing of 27.2 Å. A representative image used in the measurement of the spacing is provided in Figure 1(c), with the simulated diffraction pattern shown in the inset. Measurement by this method suffers from situational variability due to the uncontrolled viewing axis. If the ZrP nanoplatelets had been completely delaminated, then a typical nanoplatelet would have had an aspect ratio of 30 or more.

The same ZrP/PCL composition, when extruded, showed a similarly small number of delamination events. However, drawing, peeling, and thinning of some tactoids occurred (see Fig. 4). Once again, no exfoliation could be detected by XRD (see Fig. 3). A comparison of the integrated ZrP peak intensities with respect to the internal PCL standard did not show any extinction of the ZrP layer correlations.

The volumetric loadings of ZrP (density  $\approx 1.33$  g/cm<sup>3</sup>) were over 70% higher than those reported for organically modified clays having densities near 2.3 g/cm<sup>3</sup> at equivalent weight fractions.<sup>30–32</sup>

Figure 2 shows an increase in agglomeration due to a ZrP loading of 20% w/w in PCL. Dispersed tactoids with distorted outer layers are also visible, many of which were drawn into longer forms. Micrometer-sized agglomerates in LS/polymer systems are insufficiently loaded to cause delamination under an applied stress, and this results in embrittlement of the composites.<sup>33,34</sup> Large agglomerates in ZrP/PCL may counteract any property improvements gained from elongation and thinning of the tactoids.

The extruded ZrP/PCL formulations exhibited an intralayer *d*-spacing of 27.9 Å, as determined by XRD. This value is very close to the XRD measurement of 28.4 Å for the isolated ZrP (Fig. 3). Aggregate cohesion was evident in PCL from both the XRD results and the observation by TEM that the ZrP tactoids underwent considerable distortion without intercalation during the melt-compounding process [Fig. 4(b)].

Individual layers, or small groups of layers, appeared to be sheared or split away at the edges as



Figure 4 TEM micrographs of edge-treated ZrP/PCL (5% w/w) after compounding, extrusion, and molding: (a) edge peeling and (b) shear delamination of a tactoid's outer surface.



**Figure 5** TEM micrographs of 50% w/w edge-treated ZrP in PCL after compounding, extrusion, and molding. ZrP tactoids appear intact despite being distorted by shear flow.

they were separated from the dispersed ZrP tactoids, rather than forced apart by swelling from within. Intercalation was not detected by increased *d*-spacings in XRD and did not appear to serve a role in the delamination of the tactoids.

In ZrP/PCL loaded at 50% w/w, the aggregates were so crowded together that exfoliation or drawing by the matrix polymer was entirely prevented. The tactoids tended to coalesce rather than shear one another apart (Fig. 5).

It is possible that the acetone used to aid mixing via the SpeedMixer method also aided in the swelling of ZrP. The mixer is capable of combining very viscous materials, but it cannot develop high shear in materials that do not flow at all. Acetone was found empirically to be the most efficient solvent for plasticizing PCL and may prove to be a useful processing aid.

## Nanocomposite mechanical characterization: tensile properties

Extruded fibers were tested in uniaxial tension with the goal of determining the ultimate properties and also gaining a measure of the fracture energy. A summary of the ultimate properties is given in Table I. Young's modulus was determined from the linear portion of the stress–strain response, which typically occurred in the strain range of 0.01–0.03.

The yield strength of the 5% w/w ZrP/PCL nanocomposite was significantly increased (P = 0.01) by an average of 8% over that of the base polymer. However, the nanocomposite yield strengths were reduced with higher ZrP loadings. The tensile elastic moduli of all nanocomposites were significantly higher (P < 0.05) than that of unmodified PCL. Only the 50% w/w ZrP sample was significantly stiffer than the other nanocomposite groups, whose average improvement was 24%. Therefore, the use of more than 5% octyl/MOUD ZrP, as prepared in this study, is not recommended for improving the ultimate properties of PCL unless the application favors elastic modulus over yield strength.

The tensile characteristics of PCL nanocomposites were previously investigated with LS fillers.<sup>30–32</sup> Ductility (ca. 800% elongation) was maintained with up to 7.5% w/w Cloisite 30B in compression-molded PCL nanocomposites, whereas the tensile modulus increased by 67% and the yield strength declined by 27%.<sup>30</sup> The ductility of PCL was severely compromised with 10% w/w or more intercalated montmorillonite (equivalent to 4.4% v/v).<sup>31</sup> In comparison, our materials showed less improvement in the elastic modulus with better retention of the yield strength, and this suggested less interaction between the polymer and the ZrP tactoids in comparison with fully intercalated layered silicate (LS).

The total work of fracture, defined as the area under the load–displacement curve, could not be assessed for specimens containing up to 20% w/w ZrP ( $\approx 15\% \text{ v/v}$ ) because they did not fracture within the limits of the test frame, that is, 650% elongation. This result compares favorably with the results for intercalated montmorillonite/PCL nanocomposites, whose extensibility decreased from 550 to 350% with an increase in the filler loading from 10 ( $\approx 4.4\% \text{ v/v}$ ) to 20% w/w.<sup>31</sup> However, specimens containing 50% w/w ZrP were exceedingly brittle, and the fracture toughness was better quantified by SENB testing.

#### **Flexural properties**

Flexural testing was carried out to elucidate any differences between the elastic moduli of the

TABLE I						
Tensile Testing Data for Extruded Fibers $(n = 7)$						

Sample	Tensile yield stress (MPa)	Tensile elastic modulus (MPa)	Elongation (%)
PCL PCL + 5% ZrP PCL + 10% ZrP PCL + 15% ZrP PCL + 20% ZrP PCL + 50% ZrP	$\begin{array}{c} 15.6 \pm 1.2 \\ 16.9 \pm 0.3 \\ 14.5 \pm 0.8 \\ 14.7 \pm 0.7 \\ 14.4 \pm 0.8 \\ 11.0 \pm 3.7 \end{array}$	$\begin{array}{c} 226 \pm 30 \\ 277 \pm 38 \\ 294 \pm 35 \\ 299 \pm 12 \\ 318 \pm 42 \\ 495 \pm 101 \end{array}$	>650 >650 >650 >650 >650 <6

Tensile values plus or minus 1 standard deviation are shown.

TABLE II
Flexural and Storage Moduli with Random-Error
Probabilities for Molded Beams Tested in Pseudostatic
and Dynamic (1 Hz) Three-Point Bending at 25°C

Sample	Flexural modulus (MPa)	Р	Storage modulus (MPa)	Р
PCL	$256 \pm 13$		320 ± 29	
PCL + 5% ZrP	$310\pm65$	0.282	$360\pm38$	0.151
PCL + 10% ZrP	$358\pm23$	0.005	$486\pm46$	0.010
PCL + 15% ZrP	$332 \pm 41$	0.073	$469 \pm 91$	0.002
PCL + 20% ZrP	$359\pm17$	0.001	$464\pm15$	0.005

Modulus values plus or minus 1 standard deviation (n = 3) are shown.

nanocomposites that were not detected during tensile testing. Furthermore, a comparison was made between the Young's moduli and the dynamic storage moduli obtained at the same temperature. The results are summarized in Table II.

There was a significant increase in the quasistatic flexural moduli of the 10 and 20% filled experimental groups versus the unfilled control. However, none of the experimental groups was significantly different from any other (P < 0.05) in this testing mode. The DMA data show a similar trend. However, the 10 and 20% filled materials had significantly higher storage moduli than both the control and the 5% ZrP composite. The overall variability was high, suggesting the need for more specimens to obtain greater statistical power.

#### Fracture toughness

SENB specimens containing 0 or 20% w/w ZrP failed in a fully plastic manner, that is, with extensive crack-tip blunting and without crack extension. Therefore, fracture toughness values could not be calculated for the material. Typical load-displacement curves are shown in Figure 6. Within the limits of the test displacement, the 20% filled material exhibited a greater area under the load-displacement curve, which suggested a greater resistance to crack propagation consistent with particle reinforcement. Specimens containing 50% w/w failed in a more brittle manner with crack-tip blunting and crack extension so that the fracture toughness could be determined by Rice's J-integral approach from elastic-plastic fracture mechanics.35 The mean fracture toughness was 0.64 MPa (m<sup>2</sup>) by this method with a standard deviation of 0.19 MPa  $(m^2)$  (n = 3), which is comparable to a fracture toughness of 0.69-0.91 MPa (m<sup>2</sup>) for ZrP-filled epoxy nanocomposites.<sup>22</sup> This fracture toughness (0.64 MPa (m<sup>2</sup>)) is higher than that of a brittle thermoset, such as a cured epoxy or dimethacrylate resin, but it represents both a substantial embrittlement of the base thermoplastic and a critical transition in the failure mechanism in comparison with the lower filled PCL specimens. A possible failure mechanism responsible for the low fracture toughness may be delamination along the ZrP lamellar interfaces.<sup>22</sup>

### DMA

Beam specimens were independently tested for their responses to changes in the temperature and loading frequency. Data from the thermal scans are plotted in Figure 7, whereas the frequency spectra are shown in Figure 8.

The onset of the glass transition in PCL was below the tested temperature range; however, the tan  $\delta$ response peaked at  $-22^{\circ}$ C in Figure 7. The literature-reported value of  $T_g$  is  $-60^{\circ}$ C for PCL with a number-average molecular weight up to 42,500.<sup>36</sup> Such low-temperature responses could not be reproduced in this study, but the doubling of the molecular weight may account for the apparent increase in  $T_g$  observed here.

In DMA, the onset of melting shifted to lower temperatures with increasing ZrP. A correlated downward trend in the melting temperature with increasing filler was observed in DSC (Fig. 9); however, the onset and peak melting temperatures were not significantly different for any of the studied loading levels (P > 0.05). The peak values were in agreement with the previously reported melting range for PCL, which is 59–64°C.<sup>36</sup> The heat of melting was significantly reduced for 50% w/w ZrP (P = 0.01). This yielded a reduction in crystallinity from 48 to 29% based on a value of 136 J/g for 100% crystalline PCL<sup>37</sup> (see Fig. 9). Disturbances in the



**Figure 6** Representative load–displacement curves for SENB specimens at various ZrP filler loadings (w/w).

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**Figure 7** Thermal spectra for (a) the storage modulus (*E*') and (b) tan  $\delta$  for 0%, 5%, and 20% w/w ZrP/PCL materials loaded at a frequency of 1 Hz (n = 3). Increased stiffness, quenching of the glass transition, and reduced melting onset in the filled samples are shown.

crystalline morphology of the PCL, such as altered crystallite size, were not apparent from the wideangle XRD data presented in Figure 3. Therefore, the crystallinity of the PCL matrix appeared largely unaffected by the presence of ZrP tactoids. This is consistent with observations for LS nanoparticles, whose thorough exfoliation is required to nucleate smaller crystallites.<sup>38</sup>

There was a meaningful increase in the storage modulus after the addition of as little as 5% w/w ZrP, and the glass transition appeared to be completely quenched. The increase in the storage modulus indicates that the ZrP does not have a plasticizing effect. This suggests that there is good adhesion between the tactoids and the matrix. Furthermore, the apparent loss of  $T_g$  (Fig. 7) is attributable to a shift above the melting temperature, rather than to a lower temperature, due to the rigidifying effect of the filler. The crossover point for the storage

modulus and complex viscosity curves in the frequency spectra (Fig. 8) was identical between the nanocomposites and the PCL control, and this suggested that the effective molecular weight was not altered through physical crosslinking.<sup>39,40</sup>

#### **CONCLUSIONS**

Delamination of octyl/MOUD ZrP was very limited in the studied formulations despite careful surface design<sup>24</sup> and preparation and the use of high-shear blending equipment. Delamination in ZrP/PCL occurred principally by shearing action between the polymer and the dispersed tactoids and not by intercalative penetration of the tactoids. The thermodynamic interactions between the polymer and the basal nanoplatelet surfaces were therefore insufficient to drive intercalation.

A mobile solvent may be required to overcome kinetic barriers to intercalation. Evidence of a



**Figure 8** Log<sub>10</sub> frequency plots for ZrP/PCL at different weight fractions. The intersection of the complex viscosity ( $\eta^*$ ) and storage modulus (*E'*) at 1.8 Hz (n = 3) is shown. Characteristic relaxation frequencies increase as the filler level increases.



**Figure 9** Melt behavior of ZrP-filled PCL as determined from DSC experiments. Error bars are  $\pm 1$  standard deviation (n = 3).

beneficial solvent-swelling effect was seen in the SpeedMixer-formulated blend processed with acetone. Diffusional aids such as sonication may also be helpful. Unlike LS platelets, the acidic edges of ZrP materials cannot be silanated. Quaternary ammonium species can provide hydrophobicity to the dangling  $\equiv$ PO<sup>-</sup> bonds populating the nanoplatelet edges. Although TEAH proved insufficient to promote intercalation in this study, longer chain and mixed-tail compounds should be investigated.

Dispersed ZrP tactoids, about 100 nm in breadth, served as a useful reinforcement phase in PCL at the 5% w/w ( $\approx$  3.8% v/v) level despite minimal exfoliation of the nanoplatelet system. The yield strength and tensile modulus of the material were improved without a substantial reduction of the polymer's ductility. Layered tactoids exhibited tortuosity when combined with PCL under high-shear melt conditions. Such distortions suggest that the tactoids have the ability to undergo interlamellar shear deformation in response to the surrounding polymer despite the general coherence of the layers. The lengthening of the tactoids provided a minor improvement in the effective particle aspect ratio, and this helped to explain the improved properties of the 5% ZrP/PCL system. Crowding and agglomeration became prevalent as the tactoid level increased, resulting in defect structures and a loss of mechanical properties.

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#### References

- Murakami, A.; Saunders, D.; Ooishi, K.; Yoshiki, T.; Saitoo, M.; Watanabe, O.; Takezawa, M. J Adhes 1992, 39, 227.
- 2. Hodgkin, J. H.; Simon, G. P.; Varley, R. J. Polym Adv Technol 1998, 9, 3.
- 3. Fisher, F. T.; Brinson, L. C. Compos Sci Technol 2001, 61, 731.
- 4. Alexandre, M.; Dubois, P. Mater Sci Eng R 2000, 28, 1.
- Giannelis, E. P.; Krishnamoorti, R.; Manias, E. Adv Polym Sci 1999, 138, 107.
- Theng, B. K. G. The Chemistry of Clay–Organic Reactions; Wiley: New York, 1974.
- 7. Ogawa, M.; Kuroda, K. Bull Chem Soc Jpn 1997, 70, 2593.
- 8. Paul, D. Presented at the MRS 2002 Spring Meeting, San Francisco, CA, 2002.

- Es, M. V.; Xiqiao, F.; Turnhout, J. V.; Giessen, E. V. D. In Specialty Polymer Additives; Al-Malaika, S.; Golovoy, A.; Wilke, C. A., Eds.; Blackwell Science: Oxford, 2001; Chapter 21.
- Nielsen, L. E.; Landel, R. F. Mechanical Properties of Polymers and Composites; Marcel Dekker: New York, 1994.
- 11. Wang, J.; Pyrz, R. Compos Sci Technol 2004, 64, 935.
- Pinnavaia, T. J.; Beall, G. W. In Polymer–Clay Nanocomposites; Scheirs, J., Ed.; Wiley: New York, 2000.
- 13. Vaia, R. A.; Giannelis, E. P. Macromolecules 1997, 30, 7990.
- 14. Scheutjens, J. M. H. M.; Fleer, G. J Phys Chem 1980, 84, 178.
- Fleer, G.; Cohen-Stuart, M. A.; Scheutjens, J. M. H. M. Polymers at Interfaces; Chapman & Hall: London, 1993.
- Balazs, A.; Ginzburg, V. V.; Lyatskaya, Y.; Singh, C.; Zhulina, E. In Polymer–Clay Nanocomposites; Pinnavaia, T. J.; Beall, G. W., Eds.; Wiley: New York, 2000; p 281.
- 17. Kim, G.-M.; Lee, D.-H.; Hoffmann, B.; Kressler, J.; Stöppelmann, G. Polymer 2001, 42, 1095.
- 18. Liu, L. M.; Qi, Z. N.; Zhu, X. G. J Appl Polym Sci 1999, 71, 1133.
- Shia, D.; Hui, C. Y.; Burnside, S. D.; Giannelis, E. P. Polym Compos 1998, 19, 608.
- Manias, E.; Touny, A.; Wu, L.; Strawhecker, K.; Lu, B.; Chung, T. C. Chem Mater 2001, 13, 3516.
- 21. Sun, L.; Boo, W. J.; Sun, D.; Clearfield, A.; Sue, H.-J. Chem Mater 2007, 19, 1749.
- 22. Sue, H.-J.; Gam, K. T.; Bestaoui, N.; Spurr, N.; Clearfield, A. Chem Mater 2004, 16, 242.
- Sue, H.-J.; Gam, K. T.; Bestaoui, N.; Clearfield, A.; Miyamoto, M.; Miyatake, N. Acta Mater 2004, 52, 2239.
- Furman, B. R.; Wellinghoff, S. T.; Thompson, P. M.; Beall, G. W.; Laine, R. M.; Rawls, R. H. Chem Mater 2008, 20, 5491.
- Kweon, H. Y.; Yoo, M. K.; Park, I. K.; Kim, T. H.; Lee, H. C.; Lee, H. S.; Oh, J. S.; Akaike, T.; Cho, C. S. Biomaterials 2003, 24, 801.
- Alberti, G.; Costatino, U.; Tomassini, A. S. N. J Inorg Nucl Chem 1978, 40, 1113.
- 27. Furman, B. R. Materials Science and Engineering; University of Michigan: Ann Arbor, MI, 2007; p 179.
- Poojary, M. D.; Hu, H.-L.; Campbell, F. L., III; Clearfield, A. Acta Crystallogr B 1993, 49, 996.
- 29. Clearfield, A.; Smith, G. D. Inorg Chem 1968, 8, 431.
- Ludueña, L. N.; Alvarez, V. A.; Vazquez, A. Mater Sci Eng A 2007, 460, 121.
- 31. Chen, B.; Evans, J. R. G. Macromolecules 2006, 39, 747.
- 32. Homminga, D.; Goderis, B.; Hoffman, S.; Reynaers, H.; Groeninckx, G. Polymer 2005, 46, 9941.
- Massenelli-Varlot, K.; Vigier, G.; Vermogen, A.; Gauthier, C.; Cavaillé, J. Y. J Polym Sci Part B: Polym Phys 2007, 45, 1243.
- Cotterell, B.; Chia, J. Y. H.; Hbaieb, K. Eng Fract Mech 2007, 74, 1054.
- Meyers, M. A.; Chawla, K. K. Mechanical Behavior of Materials; Prentice Hall: New York, 1998.
- 36. Sinha, V. R.; Bansal, K.; Kaushik, R.; Kumria, R.; Trehan, A. Int J Pharm 2004, 278, 1.
- Lepoittevin, B.; Devalckenaere, M.; Pantoustier, N.; Alexandre, M.; Kubies, D.; Calberg, C.; Jerome, R.; Duboi, P. Polymer 2002, 43, 4017.
- Ray, S.; Yamada, K.; Okamoto, K.; Fujimoto, Y.; Ogami, A.; Ueda, K. Chem Mater 2003, 15, 1456.
- Menard, K. Dynamic Mechanical Analysis: A Practical Introduction; CRC: New York, 1999.
- 40. Macosko, C. Rheology; VCH: New York, 1996.