

MS DIVYANI PAUL (Orcid ID : 0000-0002-4544-1825)

DR JAMES H MORRISSEY (Orcid ID : 0000-0002-1570-1569)

Article type : Brief Report

## **Stoichiometric analysis reveals a unique phosphatidylserine binding site in coagulation factor X**

**Divyani Paul<sup>1</sup> and James H. Morrissey<sup>1,2</sup>**

<sup>1</sup>Department of Biological Chemistry and <sup>2</sup>Department of Internal Medicine, University of Michigan Medical School, Ann Arbor, MI, USA

**Running head:** Factor X binding stoichiometry

### **Correspondence**

James H. Morrissey, Department of Biological Chemistry, 4301B MSRB III, 1150 West Medical Center Drive, University of Michigan Medical School, Ann Arbor, MI 48109, USA.

Email: [jhmorris@umich.edu](mailto:jhmorris@umich.edu)

### **Essentials**

This is the author manuscript accepted for publication and has undergone full peer review but has not been through the copyediting, typesetting, pagination and proofreading process, which may lead to differences between this version and the [Version of Record](#). Please cite this article as [doi: 10.1111/JTH.15620](https://doi.org/10.1111/JTH.15620)

This article is protected by copyright. All rights reserved

- Plasma membranes have much more phosphatidylethanolamine (PE) than phosphatidylserine (PS).
- In membranes with excess PE, the minimal number of PS required to bind factor X was unknown.
- We analyzed factor X's membrane binding stoichiometry using surface plasmon resonance.
- One factor X was bound per  $1.05 \pm 0.2$  PS molecule in membranes with excess PE.

## ABSTRACT

**Background:** Cellular trauma or activation exposes phosphatidylserine (PS) and the substantially more abundant phospholipid, phosphatidylethanolamine (PE), on the outer layer of the plasma membrane, thereby allowing binding of many blood clotting proteins. We previously proposed the Anything But Choline (ABC) hypothesis to explain how PS and PE synergize to support binding of clotting proteins with gamma-carboxyglutamate (Gla)-rich domains, which posited that each Gla domain binds to a limited number of PS molecules and multiple PE molecules. However, the minimal number of PS molecules required to stably bind a Gla-domain-containing blood clotting protein in the presence of excess PE was unknown.

**Objective:** Test the ABC hypothesis for factor X by determining the threshold binding requirement of PS molecules under conditions of PS-PE synergy.

**Methods:** We used surface plasmon resonance to investigate the stoichiometry of factor X binding to nanoscale membrane bilayers (Nanodiscs) of varying phospholipid composition.

**Results and Conclusions:** We quantified  $1.05 \pm 0.2$  PS molecules per bound factor X molecule in Nanodiscs containing a mixture of 10% PS, 60% PE, and 30% phosphatidylcholine. Hence, there appears to be one truly PS-specific binding site per Gla domain, while the remaining membrane binding interactions can be satisfied by PE.

**Keywords:** factor X, membranes, phosphatidylserines, phospholipids, surface plasmon resonance

## INTRODUCTION

The anionic phospholipid, phosphatidylserine (PS), is essential for reversible membrane binding of a number of clotting proteins.<sup>1</sup> Indeed, seven clotting proteins bind to PS-containing membranes via their  $\gamma$ -carboxyglutamate (Gla)-rich domains.<sup>1</sup> The surfaces of healthy, resting cells are anticoagulant because PS and phosphatidylethanolamine (PE) are sequestered to the inner leaflet of the plasma membrane, with phosphatidylcholine (PC) and sphingomyelin being the most abundant phospholipids in the outer leaflet.<sup>2</sup> Cellular injury or platelet activation leads to loss of membrane asymmetry and externalization of PS and PE, thus creating binding sites for clotting proteins.<sup>1</sup>

Artificial membranes containing PS dramatically enhance many clotting reactions, with maximal rates seen with 20-40% PS.<sup>3,4</sup> However, mammalian plasma membranes typically have no more than about 10% PS, while the relatively more abundant glycerophospholipids, PC and PE, account for about 40% and 28%, respectively of the phospholipid content.<sup>5,6</sup> Clotting reactions on liposomes with high PS content are therefore conducted under conditions far from the true physiological membrane composition. In 1994, Smirnov and Esmon reported that PE synergizes with PS to promote factor Va inactivation by activated protein C,<sup>7</sup> a finding that was subsequently extended by us and others to show that the presence of PE allows as little as 3 to 5% PS to support maximal rates of factor X (FX) activation by the tissue factor/factor VIIa complex,<sup>8</sup> prothrombin activation by the FXa/factor Va complex,<sup>9</sup> and factor VIII binding to membranes.<sup>10</sup> These low PS percentages are much closer to those found in plasma membranes, suggesting that the ability of PS/PE synergy to promote membrane binding by clotting proteins has physiologic significance.

In quantitative binding experiments using Nanodiscs of varying PS/PC composition, we previously showed that a membrane binding site for FX consists of 6 to 8 PS molecules, presumably clustered together via contact with the Gla domain.<sup>11</sup> We examined the mechanism of PS/PE synergy and found that almost any phospholipid tested (except PC) synergizes with PS to promote FX activation by the tissue factor/factor VIIa complex.<sup>12</sup> This led us to propose what we termed the Anything But Choline (ABC) hypothesis, which states that Gla domains bind to membranes via a limited number of "PS-specific" interactions that are satisfied only by PS, plus multiple "phosphate-specific" interactions that are satisfied by the far more abundant PE.<sup>12</sup> The

idea is that a total of about 6 to 8 PS + PE molecules collaborate together to create a single FX binding site. Since structural details for Gla domain/membrane interactions are lacking, we felt it would be an important step forward to determine the minimum number of PS molecules that can constitute a FX binding site in the presence of excess PE. We hypothesized that this number would be an integer, and furthermore, that it could be as low as one PS-specific binding site per Gla domain. Accordingly, we now report the results of quantifying the stoichiometry of FX binding to Nanodiscs with a low number of PS molecules per disc and increasing PE content.

## METHODS

Phospholipids were from Avanti Polar Lipids (Alabaster, AL), as follows: PC, 1-palmitoyl-2-oleoyl-*sn*-glycero-3-phosphocholine; PS, 1-palmitoyl-2-oleoyl-*sn*-glycero-3-phospho-L-serine; and PE, 1,2-dioleoyl-*sn*-glycero-3-phosphoethanolamine. Human FX was from Haematologic Technologies (Essex Junction, VT). Membrane scaffold protein (MSP1D1) was expressed and purified as described.<sup>13</sup>

Nanodiscs were prepared by self-assembly reactions followed by purification as described,<sup>14</sup> using varying ratios of PC, PS and PE with MSP1D1. Phospholipid concentrations in samples of purified Nanodiscs were quantified by measuring total phosphate after complete hydrolysis,<sup>15</sup> while MSP1D1 protein concentrations were determined by  $A_{280}$  (extinction coefficient:  $21,000 \text{ M}^{-1} \text{ cm}^{-1}$ ).

Assuming two copies of MSP1D1 per Nanodisc,<sup>14</sup> the ratio of the molar concentration of phospholipid to MSP1D1 represents the number of phospholipid molecules per leaflet. This ratio was used to calculate the molecular mass (MW) of the entire Nanodisc from the MW of MSP1D1 (24.6 KDa) and the component phospholipids. Table 1 gives calculations for a typical set of Nanodisc preparations in this study.

FX binding to Nanodiscs of varying phospholipid composition was quantified via Surface Plasmon Resonance (SPR) as described,<sup>11</sup> using a Biacore T-200 instrument (Cytiva, formerly GE Healthcare). Briefly, Nanodiscs were immobilized by flowing in Loading Buffer (20 mM HEPES pH 7.4, 100 mM NaCl, 0.02% sodium azide) over Ni-NTA Series S Sensor chips, and recording the net change in response units (RU) due to Nanodisc immobilization ( $\text{RU}_{\text{ND}}$ ). For most experiments, this was about 770 to 1390 RU. Increasing FX concentrations were then flowed

over Nanodisc-containing sensorchips at 30  $\mu\text{L}/\text{min}$  in Loading Buffer plus 5 mM  $\text{CaCl}_2$  and 0.2% bovine serum albumin. The maximal steady-state RU level was recorded at each input FX concentration ( $\text{RU}_{\text{FX}}$ ), then divided by  $\text{RU}_{\text{ND}}$  to yield the  $\text{RU}_{\text{FX}}/\text{RU}_{\text{ND}}$  ratio (from which background binding to a parallel flow cell with 100% PC Nanodiscs was subtracted). Binding isotherms were generated by plotting  $\text{RU}_{\text{FX}}/\text{RU}_{\text{ND}}$  versus FX concentration, to which the single-site ligand binding equation (Equation 1) was fitted using Graph Pad Prism 8.0:

$$(1) \quad \text{RU}_{\text{FX}}/\text{RU}_{\text{ND}} = (\text{B}_{\text{max}} * x)/(\text{K}_d + x)$$

where  $\text{B}_{\text{max}}$  is the calculated maximal  $\text{RU}_{\text{FX}}/\text{RU}_{\text{ND}}$  ratio at saturation,  $x$  is the FX molar concentration, and  $\text{K}_d$  is the equilibrium dissociation constant. Phospholipid bilayers and proteins have equivalent refractive indices in solution.<sup>16,17</sup> Therefore, by utilizing  $\text{B}_{\text{max}}$  from Equation 1, we calculated the number of FX molecules bound per membrane leaflet ( $\text{N}_{\text{FX}}$ ) at saturation as shown in Equation 2:

$$(2) \quad \text{N}_{\text{FX}} = ((\text{B}_{\text{max}})*(\text{MW}_{\text{ND}}/\text{MW}_{\text{FX}}))/2$$

in which  $\text{MW}_{\text{ND}}$  is the MW of the Nanodisc,  $\text{MW}_{\text{FX}}$  is the MW of human FX (58.9 kDa), and division by 2 reflects two membrane leaflets per Nanodisc.

## RESULTS AND DISCUSSION

Our goal was to determine the minimum number of PS molecules required to bind a FX molecule on nanoscale membrane bilayers in the presence of excess PE. We reasoned that limiting PS would minimize steric hindrance between bound FX molecules at saturation. We previously found that 100% PS Nanodiscs could bind 8.4 FX molecules per bilayer, which is close to the theoretical maximum number of Gla domains that could occupy the bilayer surface (about 10 FX Gla domains, based on cross-sectional area).<sup>11</sup> We therefore considered creating Nanodiscs with 10% PS. Given that Nanodiscs typically have 50 to 60 phospholipid molecules per leaflet, this should result in Nanodiscs with about 5 to 6 PS molecules per leaflet. Thus, if the minimum number of PS molecules that constitutes a FX binding site in the presence of excess PE turned out to be one, we would expect approximately 5 to 6 FX molecules bound per leaflet at saturation, which is less than the maximal packing of bound FX molecules previously measured on Nanodiscs. If the minimum number of PS molecules necessary to constitute a FX

binding site (in the presence of excess PE) were greater than one, then we would expect even fewer FX molecules bound per leaflet at saturation.

Accordingly, we prepared Nanodiscs with 10% PS and increasing PE content (20, 40 or 60% PE, with the balance being PC). As a comparator, we prepared Nanodiscs with 50% PS but no PE (balance = PC). After carefully quantifying the phospholipid and MSP1D1 content of these preparations, we calculated the number of phospholipid molecules per leaflet and MW of each Nanodisc preparation (typical results in Table 1). The calculated numbers of PS molecules per Nanodisc were within the predicted range of 5 to 6 per leaflet. Note that these calculations assume that the PS content of Nanodiscs reflects the input PS content. We previously quantified this using  $^3\text{H}$ -labeled PS and showed that the final PS content faithfully recapitulated the percent PS in self-assembly reactions, over a wide range of input PS contents.<sup>11</sup>

### **SPR-based binding analyses of FX with Nanodiscs**

We next quantified FX binding to this range of Nanodisc preparations using SPR, with the resulting binding isotherms shown in Figure 1. Saturable, steady-state binding of FX was observed, as shown in a representative raw sensorgram of FX binding to Nanodiscs containing 10% PS, 20% PE, 70% PC (Figure 1A). The binding affinities of FX to Nanodiscs containing 10% PS and varying PE (Figure 1B) were somewhat weaker than that observed with Nanodiscs containing 50% PS (Figure 1C). Thus, the  $K_d$  value for FX binding to 50% PS Nanodiscs was  $0.31 \pm 0.14 \mu\text{M}$ , in close agreement with our previously reported  $K_d$  of  $0.38 \pm 0.005 \mu\text{M}$  for FX binding to such Nanodiscs.<sup>18</sup> For Nanodiscs with 10% PS and varying PE, the  $K_d$  values were:  $1.57 \pm 0.19 \mu\text{M}$  for 10% PS, 20% PE;  $1.51 \pm 0.54 \mu\text{M}$  for 10% PS, 40% PE; and  $1.28 \pm 0.20 \mu\text{M}$  for 10% PS, 60% PE (compared graphically in Figure 1D).

### **Stoichiometry of FX binding**

Table 2 summarizes the results of FX binding experiments to the range of Nanodiscs listed in Table 1, using three separate Nanodisc preparations for each experiment. For discs containing 50% PS, 50% PC, we found one FX binding site per  $7.53 \pm 1.3$  PS molecules, in good agreement with our previous determination of one FX binding site per 7.97 PS molecules using Nanodiscs composed of binary mixtures of PS and PC.<sup>11</sup> When we examined FX binding to Nanodiscs

containing 10% PS and varying PE, we found that the number of PS molecules per FX binding site decreased from  $1.73 \pm 0.4$  with 20% PE down to  $1.05 \pm 0.2$  with 60% PE.

These results indicate that the FX Gla domain requires just a single PS molecule to bind to membranes in the presence of excess PE, consistent with the ABC hypothesis<sup>12</sup> and extending it to state that there is only one truly PS-specific binding site in the FX Gla domain. Membranes consisting of binary PE/PC mixtures do not appreciably support FX binding or FX activation by the tissue factor/factor VIIa complex,<sup>8,12</sup> which is also consistent with the notion that at least one PS molecule is required to create a Gla-domain binding site on the membrane, even in the presence of a large excess of PE.

Although there is weak but detectable binding of FX to PE/PC discs,<sup>19</sup> we chose to subtract background binding from 100% PC discs instead of PE/PC discs for the following reason. Nanodiscs with 10% PS, 60% PE, 30% PC have 48.4 phospholipids per leaflet (Table 1), which translates to 4.84 PS molecules and 29.0 PE molecules per leaflet. For such discs, we quantified 5.19 FX molecules bound per leaflet at saturation, meaning one FX molecule bound per 0.93 PS + 5.60 PE molecules (= 6.53 non-PC phospholipid molecules). As discussed above, one FX molecule binds for every 6 to 8 non-PC lipids, so it follows that virtually all the PE molecules are engaged with FX when it binds at saturation to these discs. Since there should be insufficient free PE molecules left to create another FX binding site under such conditions, we did not subtract FX binding to 60% PE, 40% PC discs.

We currently lack direct structural information on how Gla domains bind to membranes, although molecular dynamics simulations of Gla domain binding to PS-containing bilayers have provided tantalizing clues.<sup>12,20,21</sup> These simulations show Gla domains interacting with PS headgroups in multiple ways, sometimes involving just one charged group on the PS headgroup (such as the carboxylate or the phosphate), and other times involving interactions between multiple atoms in the PS headgroup and a combination of amino acid residues and bound  $\text{Ca}^{2+}$  in the Gla domain. Interestingly, binding of Gla domain-containing proteins to membrane surfaces requires PS with a headgroup composed of L-serine, not D-serine.<sup>1,12</sup> This suggests that this one truly PS-specific binding site in the FX Gla domain is likely to bind the PS headgroup in a stereospecific manner, although this idea was not tested specifically in the present study. It will

be interesting to further identify and characterize the unique PS binding site in the FX Gla domain, perhaps by mutagenesis or structural studies.

### **Acknowledgments**

This work was supported by grant R01 GM123455 from the NIH Common Fund and grant R35 HL135823 from the National Heart, Lung and Blood Institute of NIH.

### **Conflict of Interest**

Both authors declare no relevant conflicts of interest.

### **Author Contributions**

D.P. performed the experiments, analyzed the results, and wrote the report. J.H.M conceptualized and designed the study, helped in data interpretation and wrote the report.

### **ORCID**

Divyani Paul <https://orcid.org/0000-0002-4544-1825>

James H. Morrissey <https://orcid.org/0000-0002-1570-1569>

### **References**

1. Zwaal RFA, Comfurius P, Bevers EM. Lipid-protein interactions in blood coagulation. *Biochim Biophys Acta*. 1998; 1376: 433-453.
2. Bevers EM, Comfurius P, Dekkers DW, Harmsma M, Zwaal RF. Transmembrane phospholipid distribution in blood cells: Control mechanisms and pathophysiological significance. *Biol Chem*. 1998; 379: 973-986.
3. Neuenschwander PF, Morrissey JH. Roles of the membrane-interactive regions of factor VIIa and tissue factor. The factor VIIa Gla domain is dispensable for binding to tissue factor but important for activation of factor X. *J Biol Chem*. 1994; 269: 8007-8013.
4. Kung C, Hayes E, Mann KG. A membrane-mediated catalytic event in prothrombin activation. *J Biol Chem*. 1994; 269: 25838-25848.
5. O'Donnell VB, Murphy RC, Watson SP. Platelet lipidomics: modern day perspective on lipid discovery and characterization in platelets. *Circulation research*. 2014; 114: 1185-1203.



6. Bevers EM, Comfurius P, Zwaal RFA. Changes in membrane phospholipid distribution during platelet activation. *Biochim Biophys Acta*. 1983; 736: 57-66.
7. Smirnov MD, Esmon CT. Phosphatidylethanolamine incorporation into vesicles selectively enhances factor Va inactivation by activated protein C. *J Biol Chem*. 1994; 269: 816-819.
8. Neuenschwander PF, Bianco-Fisher E, Rezaie AR, Morrissey JH. Phosphatidylethanolamine augments factor VIIa-tissue factor activity: enhancement of sensitivity to phosphatidylserine. *Biochemistry*. 1995; 34: 13988-13993.
9. Smeets EF, Comfurius P, Bevers EM, Zwaal RF. Contribution of different phospholipid classes to the prothrombin converting capacity of sonicated lipid vesicles. *Thromb Res*. 1996; 81: 419-426.
10. Gilbert GE, Arena AA. Phosphatidylethanolamine induces high affinity binding sites for factor VIII on membranes containing phosphatidyl-L-serine. *J Biol Chem*. 1995; 270: 18500-18505.
11. Shaw AW, Pureza VS, Sligar SG, Morrissey JH. The local phospholipid environment modulates the activation of blood clotting. *J Biol Chem*. 2007; 282: 6556-6563.
12. Tavoosi N, Davis-Harrison RL, Pogorelov TV, et al. Molecular determinants of phospholipid synergy in blood clotting. *J Biol Chem*. 2011; 286: 23247-23253.
13. Ritchie TK, Grinkova YV, Bayburt TH, et al. Chapter 11 - Reconstitution of membrane proteins in phospholipid bilayer nanodiscs. *Methods Enzymol*. 2009; 464: 211-231.
14. Bayburt TH, Grinkova YV, Sligar SG. Self-assembly of discoidal phospholipid bilayer nanoparticles with membrane scaffold proteins. *Nano Lett*. 2002; 2: 835-856.
15. Fiske CH, Subbarow Y. The colorimetric determination of phosphorus. *J Biol Chem*. 1925; 66: 375-400.
16. Terrettaz S, Stora T, Duschl C, Vogel H. Protein binding to supported lipid membranes: investigation of the cholera toxin-ganglioside interaction by simultaneous impedance spectroscopy and surface plasmon resonance. *Langmuir : the ACS journal of surfaces and colloids*. 1993; 9: 1361-1369.
17. Heyse S, Vogel H, Sanger M, Sigrist H. Covalent attachment of functionalized lipid bilayers to planar waveguides for measuring protein binding to biomimetic membranes. *Protein Sci*. 1995; 4: 2532-2544.

18. Tavoosi N, Smith SA, Davis-Harrison RL, Morrissey JH. Factor VII and protein C are phosphatidic acid-binding proteins. *Biochemistry*. 2013; 52: 5545-5552.
19. Medfisch SM, Muehl EM, Morrissey JH, Bailey RC. Phosphatidylethanolamine-phosphatidylserine binding synergy of seven coagulation factors revealed using Nanodisc arrays on silicon photonic sensors. *Sci Rep*. 2020; 10: 17407.
20. Muller MP, Wang Y, Morrissey JH, Tajkhorshid E. Lipid specificity of the membrane binding domain of coagulation factor X. *J Thromb Haemost*. 2017; 15: 2005-2016.
21. Ohkubo YZ, Morrissey JH, Tajkhorshid E. Dynamical view of membrane binding and complex formation of human factor VIIa and tissue factor. *J Thromb Haemost*. 2010; 8: 1044-1053.

## TABLES AND FIGURE LEGEND

**TABLE 1** Calculations for a typical set of Nanodisc preparations used in this study

Nanodisc lipid composition	Phospholipid [ $\mu\text{M}$ ]*	MSP1D1 [ $\mu\text{M}$ ]*	Phospholipid molecules/leaflet <sup>†</sup>	$N_{\text{PS}}^{\ddagger}$	$\text{MW}_{\text{ND}}$ [kDa]
100% PC	550	9.59	57.4	0	136
50% PS, 50% PC	640	10.6	60.4	30.2	142
10% PS, 20% PE, 70% PC	680	11.9	57.1	5.71	136
10% PS, 40% PE, 60% PC	542	9.92	54.6	5.46	140
10% PS, 60% PE, 30% PC	451	9.31	48.4	4.84	122

\*Phospholipid and MSP1D1 concentrations in purified Nanodisc preparations were quantified as described in Methods.

<sup>†</sup>Calculated as the ratio of the molar concentrations of phospholipid to MSP1D1.

<sup>‡</sup> $N_{\text{PS}}$  (the number of PS molecules per leaflet) is the number of phospholipid molecules per leaflet multiplied by the fraction of the input phospholipid that was PS (i.e., 0, 0.5 or 0.1).

**TABLE 2** Stoichiometry of FX binding to Nanodiscs

Nanodisc lipid composition	$N_{\text{PS}}^*$	$N_{\text{FX}}^{\dagger}$	$N_{\text{PS}}/N_{\text{FX}}$
----------------------------	-------------------	---------------------------	-------------------------------

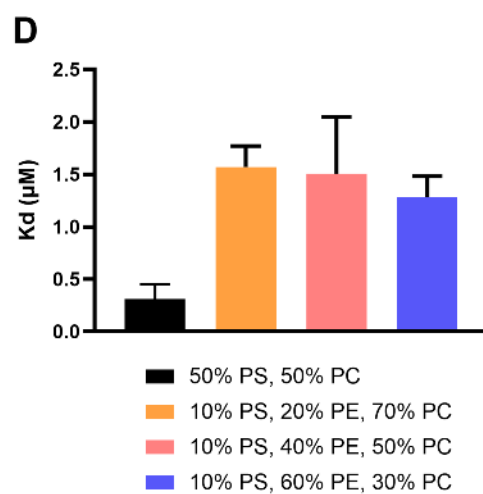
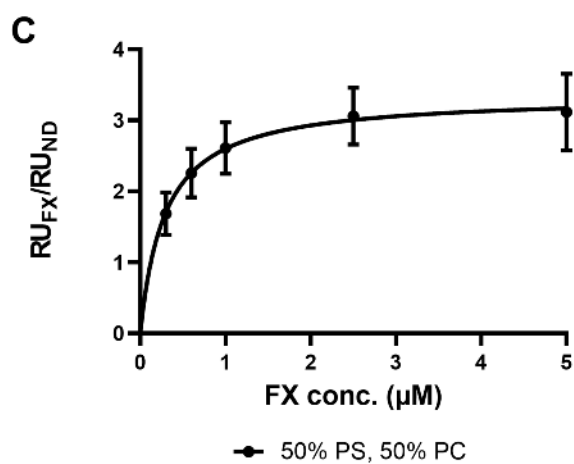
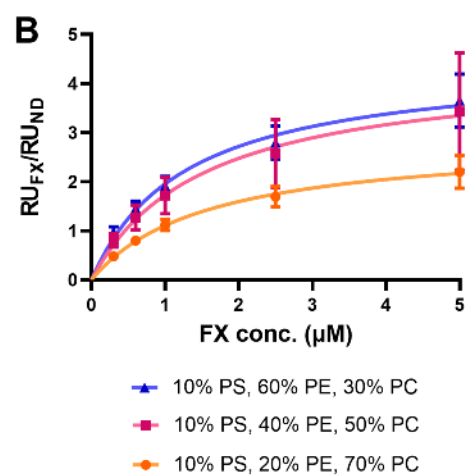
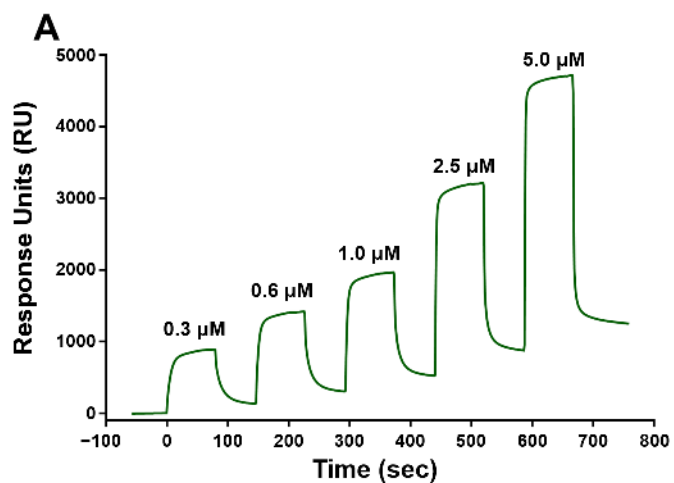
50% PS, 50% PC	30.4 ± 2.7	4.09 ± 0.4	7.53 ± 1.3
10% PS, 20% PE, 70% PC	5.31 ± 0.6	3.13 ± 0.6	1.73 ± 0.4
10% PS, 40% PE, 50% PC	4.74 ± 0.6	4.60 ± 2.0	1.16 ± 0.4
10% PS, 60% PE, 30% PC	4.64 ± 0.5	4.50 ± 0.7	1.05 ± 0.2

\*N<sub>PS</sub>, number of PS per leaflet.

†N<sub>FX</sub>, number of FX molecules bound per leaflet at saturation.

Data are mean ± standard error; n = 3.

**FIGURE 1** Binding of FX to Nanodiscs of varying phospholipid composition, quantified by SPR. (A) Raw sensorgram of FX binding to 10% PS, 20% PE, 70% PC Nanodiscs. (B) Binding isotherms of the association of FX with Nanodiscs of the following lipid compositions: 10% PS, 20% PE; 10% PS, 40% PE; and 10%PS, 60% PE. (C) Binding isotherm of the association of FX with Nanodiscs containing 50% PS. (In all cases, the balance is PC.) In panels B and C,  $RU_{FX}/RU_{ND}$  is plotted on the y-axis, which represents saturating RU values for FX binding ( $RU_{FX}$ ) divided by the RU values for Nanodisc immobilization ( $RU_{ND}$ ), after subtraction of background binding to a reference cell with 100% PC Nanodiscs. (D) Bar graphs of  $K_d$  values obtained by fitting equation 1 to the data in panels B and C. In panels B-D, error bars are standard error from three independent experiments.



jth\_15620\_f1.tif