

Rib cortical bone thickness variation in adults by age and sex

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Abstract

Rib fractures are a common and serious outcome from blunt thoracic trauma and their likelihood is greater in older individuals. Osteoporotic bone loss is a well-documented aging phenomenon with sex-specific characteristics, but within rib bones neither baseline maps of regional thickness nor the rates of bone thinning with age have been quantified across whole ribs. This study presents such data from 4,014 ribs of 240 adult subjects aged 20-90. A validated cortical bone mapping technique was applied to clinical computed tomography scans to obtain local rib cortical bone thickness measurements over the surfaces of ribs 2 through 11. Regression models to age and sex gave rates of cortex thinning in local zones and aggregated across whole ribs. Statistical parametric mapping provided these relationships regionally as a function of rib surface location. All models showed significant reductions in bone thickness with age ($p < 0.01$). Average whole-rib thinning occurred at between 0.011 to 0.032 mm/decade (males) and 0.035 to 0.043 mm/decade (females), with sex and age accounting for up to 37% of population variability (R^2). Rates of thinning differed regionally and by rib, with highest bone

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loss of up to 0.074 mm/decade occurring in mid-rib cutaneous and superior regions of ribs 2-6. Rates were consistently higher in females than males (significantly so across whole ribs but not all local regions) and were more pronounced in cutaneous, superior, and inferior rib aspects (average 0.025 mm/decade difference in ribs 4-8) compared to pleural aspects which had the thickest cortices but saw only minor differences in thinning rates by sex (0.045 mm/decade for females and 0.040 mm/decade for males). Regional analysis showed males and female bone thickness differences that were not statistically significant at 20 years of age ($p > 0.05$ across practically all regions) but subsequent cortex thinning meant that substantial pleural and cutaneous regions were thinner ($p < 0.05$) in females than males by 55 years of age. The techniques and results from this study can be applied to assess rib bone content loss in clinical settings across wide populations. Additionally, average cortex thickness results can be mapped directly to finite element models of the thorax, and regression results used to modify such models to represent ribs of men and women across their full adult lifespan.

Keywords: Cortical bone, Rib, Computed Tomography, Cortical thickness, Computational models

1. Introduction

2 Thoracic injuries are a major concern in trauma and the ribs play a key
protective and structural role. Rib fractures are the most commonly occur-
4 ring thoracic injury, and their presence acts as a sentinel for further injury to
critical organs in the chest and abdomen ([Witt & Bulger, 2017](#); [Talbot et al.,](#)
6 [2017](#); [Dogrul et al., 2020](#)). Occupant protection in motor vehicle crashes

(MVCs) has improved considerably over previous eras, but rib fracture rates
8 have seen only marginal reductions during this time and remain as the most
common serious injury in multiple crash scenarios (Forman et al., 2019; Pip-
10 korn et al., 2020). With changing population demographics there is further
concern not just with increased rib fracture frequency with age, but also with
12 higher resulting mortality and morbidity in the elderly and other vulnerable
populations (Sirmali et al., 2003; Stawicki et al., 2004). Osteoporosis is a
14 skeletal disorder seen in all populations but with highest incidences among
older people, Caucasians, and women (Sozen et al., 2017; Alswat, 2017). It is
16 characterized by decreased bone mass and a deteriorated bone microstructure
that results in reduced bone strength, elevated bone fragility, and increased
18 fracture risk (Chen, 2014). Bone loss mechanisms and rates with aging are
well documented at multiple body regions including the pelvis, femoral heads,
20 vertebrae, and wrists, and similar trends are expected to be found in the ribs
(Pignolo et al., 2021; Telfer et al., 2021; Poole et al., 2012; Eftekhar-Sadat
22 et al., 2016).

Computational human body models (HBMs) are a tool for simulating and
24 predicting injury under a wide range of loading conditions. They are gen-
erally built to target one specific demographic (e.g., 50th percentile male),
26 and most efforts to broaden their applicability to better represent subjects
of varying sex and age involve post-hoc morphing of their geometry based on
28 reference literature (Hwang et al., 2020; Chen et al., 2018; Schoell et al., 2015;
Shi et al., 2014; Holcombe et al., 2017; Vavalle et al., 2014). Predicting rib
30 fracture events with HBMs is a particularly difficult task, and rib-only models
that introduce detailed rib-specific geometry and bone thickness have found

32 improved accuracy in such predictions (Iraeus et al., 2019; Li et al., 2010).
Most full body HBMs, however, have simplified rib geometry that deviates
34 substantially from typical anatomy of their target demographic (Holcombe
et al., 2020), stemming in part from insufficiently detailed anatomical refer-
36 ence data at the time of construction.

Rib bone properties including cortex thickness play a key role in fracture
38 events and show large inter-subject variation as well as regional variation
across the rib cage (Agnew et al., 2018; Murach et al., 2017; Kemper et al.,
40 2007, 2005). Rib cortical thickness has been measured to span approximately
0.1–2.6 mm (Mohr et al., 2007; Choi & Kwak, 2011; Agnew et al., 2018;
42 Holcombe et al., 2019a), but these data are limited to individual rib levels or
sites, or have been aggregated across broad regions containing wide ranges
44 of variation. To date, thickness measurements across multiple levels and in
sufficient detail for direct application to HBMs has not yet been expounded
46 in the literature. This study aims firstly to address this knowledge gap, and
secondly to investigate regional relationships between cortex thickness and
48 subject age and sex.

2. Materials and methods

50 Chest CT scans of 240 females and males between 20 to 90 years of age (15
or more subjects per sex per decade) were obtained from within the Univer-
52 sity of Michigan morphomics database under IRB HUM00041441. Subject
demographic distributions in age (avg \pm SD of 55 ± 19 years), height, weight,
54 and BMI are shown in Figure 1. Self-reported subject race or ethnicity
was Caucasian (80%), African American (10%), Asian (2%), Hispanic or

56 Latino (2%), or unreported (6%). All scans were acquired as part of stan-
 58 dard trauma diagnosis and care at 0.625 mm slice spacing using a standard
 reconstruction kernel optimized for visualizing soft tissue. Axial resolution
 60 within each scan ranged between 0.50 mm/px and 0.97 mm/px. Subjects had
 normal thoracic skeletal anatomy and fractured ribs were excluded from the
 study.

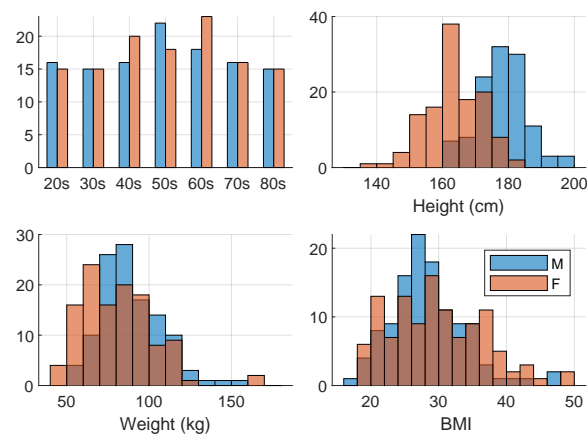


Figure 1: Histogram distributions of subject demographics.

62 2.1. Image processing

3D centerline curves were placed along all ribs within each scan and a
 64 series of planar rectangular patch areas (10 mm by 20 mm) were defined per-
 pendicular to each rib at 2.5% intervals along its central curve (Figure 2).
 66 The local X-axis of each patch was oriented to best align to the local pleural-
 to-cutaneous direction (i.e., perpendicular to the chest wall), defined by the
 68 normal direction of a 3D spline surface fitted to the collection of all rib curves
 in each scan.

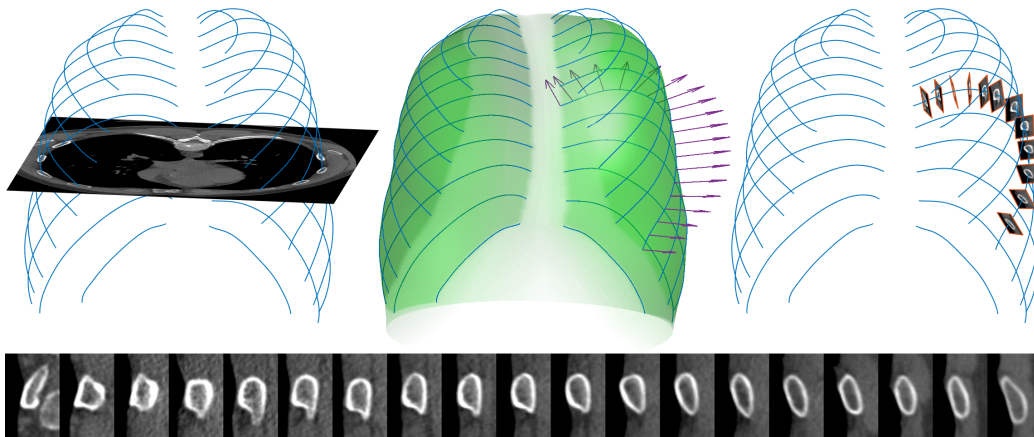


Figure 2: 3D rib curves (top left) with fitted chest wall surface normals used to align local patch X-axes (top middle), and resulting sampled rib patches (top right and bottom row).

70 The sequence of steps illustrated in Figure 3 were applied to each individual patch as described below. Firstly, thresholding and morphological opera-

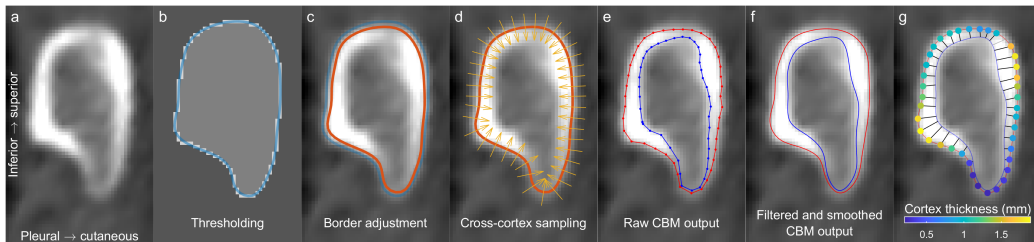


Figure 3: Image processing steps from input image patch (a) through to periosteal and endosteal borders (f) and viable cortex thickness measurements (g).

72 tions produced an initial binary segmentation, and a periodic spline was fitted to its outer perimeter (Figure 3b). To counter known over-segmentation issues arising from thresholding (Holcombe et al. (2019a,b)), an initial pass of

74

the cortical bone mapping algorithm (CBM, see [Treece & Gee \(2015\)](#); [Hol-](#)
76 [combe et al. \(2018\)](#) for details) was applied perpendicular to points along this
spline to shift it along its normal direction to better align with the true cortex
78 border (Figure 3c). A second CBM pass was then performed on cross-cortex
samples (Figure 3d) at 40 equally spaced points around the rib to provide
80 initial estimates of periosteal and endosteal borders (Figure 3e). This out-
put was filtered to avoid dual-cortex issues prevalent near the costal groove
82 ([Holcombe et al. \(2019a\)](#)), and a smoothing spline was fitted to provide final
periosteal and endosteal borders (Figure 3f). The shortest distance between
84 these borders gave the the local cortical bone thickness (CT.TH) as a con-
tinuous function around the rib. CT.TH measures were retained only when
86 the vector from the periosteal border to its nearest location on the endosteal
border matched the normal direction of the periosteal border to within 20
88 degrees.

Four landmarks were identified on each patch to provide inter-subject reg-
90 istration in the around-rib direction. These started with an inferior landmark
at the inferior-most point of the periosteal border (as defined from within the
92 in-patch view). A superior landmark was then placed at the average between
the superior-most border position and the position intersected by a ray ex-
94 tending from the inferior landmark and passing through the periosteal area
centroid. Pleural and cutaneous landmarks were placed co-linear with the
96 area centroid and perpendicular to the inferior-superior landmark direction.
Along-rib registration between ribs was given directly by the curvilinear per-
98 centage length along each rib.

All image processing, data processing, and statistical analyses were per-

100 formed in MATLAB 2022a (The Mathworks, Natick, MA).

2.2. Zonal analysis

102 Cortical thickness measurements were collected into per-rib maps (indi-
vidual grids of CT.TH values registered by along-rib percentage and around-
104 rib location as above). One-dimensional along-rib gaussian smoothing was
applied using a symmetric window of 5 % of the rib's length. Missing CT.TH
106 values at those regions identified above (4.6 % of surface locations) were im-
puted separately for each rib level using a trimmed scored regression algo-
108 rithm implemented in the Missing Data Imputation Toolbox (v1.0) (Folch-
Fortuny et al., 2016). Discrete zones within these maps were identified on
110 each rib corresponding to regional maxima or minima features. These in-
cluded pleural, cutaneous, inferior, and superior zones all taken from a mid-
112 rib region, as well as a sternal zone covering the full circumference of the
distal-most 15% of ribs. Finally, a zone encompassing the rib's full surface
114 was chosen. Average CT.TH values within each zone were calculated and
linear regression was performed to explore the associations between CT.TH
116 and subject sex and age (along with age*sex interaction) for each zone and
each rib number, with significance assessed at the $p < 0.01$ level to account
118 for repeat analyses.

2.3. Regional surface analysis

120 Statistical Parametric Mapping (SPM) was performed on whole rib CT.TH
surface maps at each rib level using SurfStat (v1.0, (Worsley et al., 2009))
122 with linear model terms corresponding to subject age, subject sex, and the

age*sex interaction. Clusters within each map of significant main effects of
124 each term were assessed at the adjusted significance level of $p < 0.05$.

2.4. Sixth rib validation

126 To assess compatibility of results here with past work, the current results
for sixth rib CT.TH values were compared to those previously reported in
128 [Holcombe et al. \(2019a\)](#). Both studies share a similar CBM methodology
but the past results from [Holcombe et al. \(2019a\)](#) were obtained from higher
130 resolution CT scans of 33 excised cadaveric sixth ribs compared to the live
subject CT scans that were used here. The previous results were validated
132 against ground truth histological measurements which are unavailable for the
live subjects as used in the current study. Therefore the presence or absence
134 of systematic measurement error in current results was explored by compar-
ing them to results from this validated past work via histogram distributions
136 of whole rib CT.TH measurements and average CT.TH values within each
discrete rib zone. Subjects from [Holcombe et al. \(2019a\)](#) were on average 10
138 years older (65 ± 21 years) than the current study cohort so comparisons of
average CT.TH within each zone were adjusted for the expected difference
140 due to age as predicted by regression analyses from within that same zone.

3. Results

142 All pre-processing and CBM was successfully run on 160K image patches
from 4,014 ribs. Figure 4 shows exemplar results for image patches from the
144 youngest and oldest female subjects.

Average CT.TH maps from all subjects grouped by rib level are presented
146 in Figure 5 with maps of CT.TH standard deviation across the population

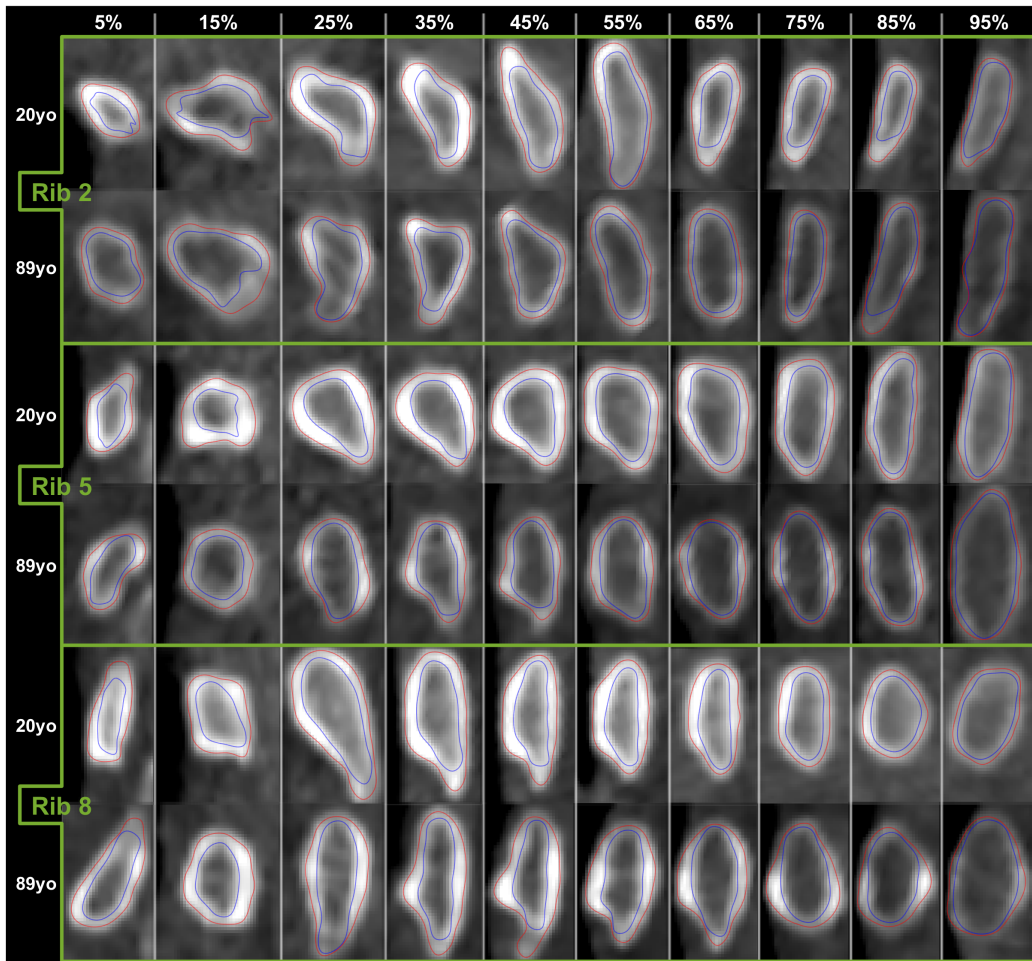


Figure 4: Smoothed periosteal and endosteal borders from the youngest and oldest female subjects.

given in Figure A.1. Figure 6 shows those same average CT.TH maps projected onto exemplar 3D rib geometry. Figures 5 and A.1 also show the superimposed positions of each discrete zone used in subsequent zonal analyses. Each of these CT.TH maps (and also those separated by sex) including

152 polygon coordinates designating each discrete zone are provided as supplementary data. Ribs 4 through 8 showed largely equivalent patterns in bone
154 thickness maps across each rib, but with variations in the magnitudes of that thickness. Rib 6 had the thickest cortices of up to 1.6 mm along the pleural aspect. The thinnest cortices were consistently found at the sternal
156 end in all ribs, reaching minimum average values of 0.35 mm in all ribs and as low as 0.30 mm in ribs 2 through 5. Ribs 2 and 3 saw regional CT.TH
158 maxima that were closer to the vertebral rib ends than for other ribs, and these regional maxima shifted position from a superior rib aspect (nearer to the mid-rib) towards a more pleural rib aspect (nearer to the vertebral end).
160 Figure 6 shows each average CT.TH map projected onto exemplar 3D rib cage geometry using bi-linear interpolation.
162

Average CT.TH values per rib and subject from within each analysis zone
164 are plotted against subject age in Figure 7. Male and female regression lines are included along with each line's slope indicating the mm change in CT.TH per decade. Predicted CT.TH values by each regression model at the ages of
166 20 and 90 years are provided for all ribs and zones in Table 1. Surface maps of the main effects identified from statistical parametric mapping are given
168 in Figure 8. These show the regional variation in the influences of age, sex, and age*sex interaction model terms on rib surface CT.TH.
170

Both zonal (summarized in Figure 7) and regional (summarized in Figure
172 8) analyses show clear reductions in rib bone thickness with age. In zonal regression models the independent effect of age on CT.TH is negative and significant ($p < 0.01$) in all discrete zones of all ribs. This is reflected
174 by large and contiguous clusters of significantly negative regions across rib

176 surfaces in age effect results derived from SPM regional analysis. Typical

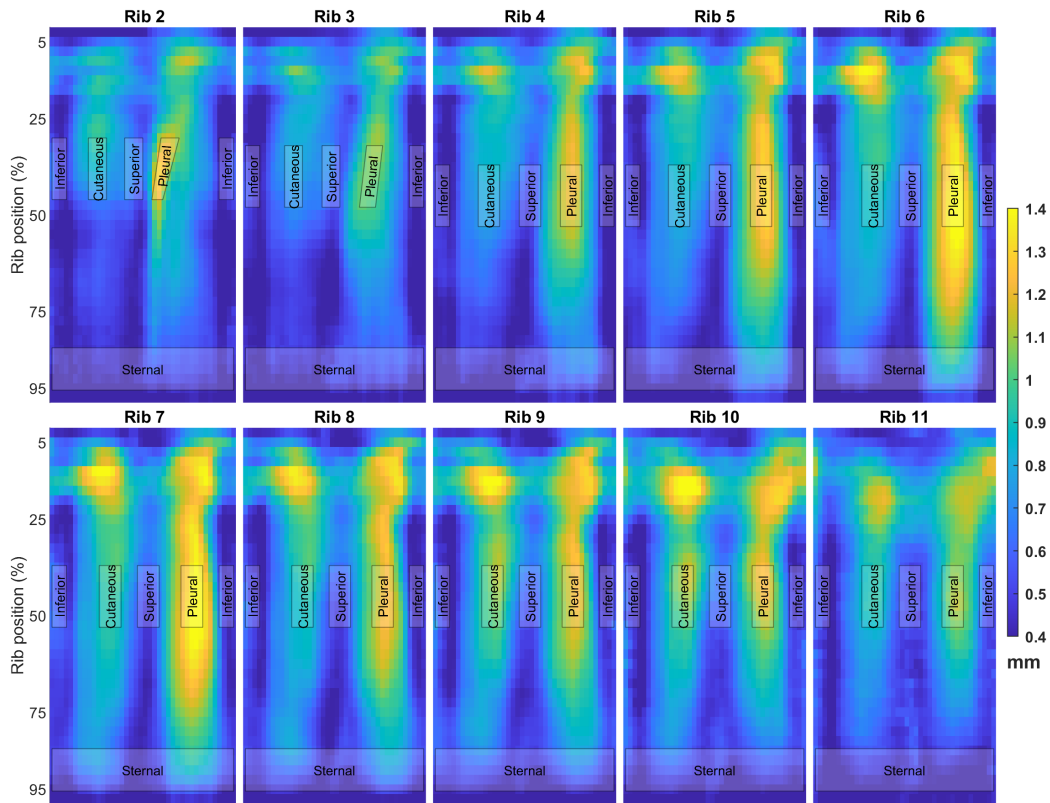


Figure 5: Average cortical thickness maps for ribs 2-11 showing the discrete zones chosen for regression analysis.

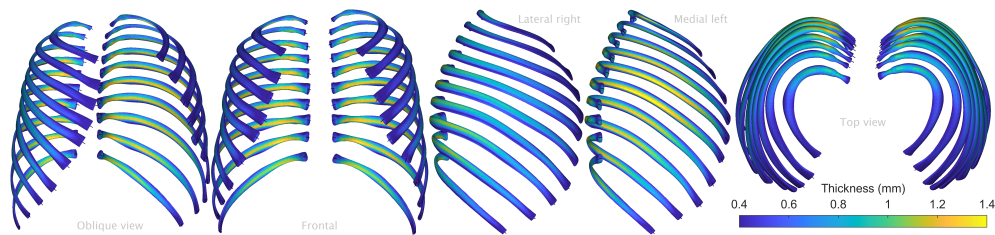


Figure 6: CT.TH maps projected onto exemplar 3D rib cage anatomy.

reduction rates were highest (up to approximately 0.07 mm/decade) in cutaneous and superior rib zones. Reduction rates were lowest in sternal zones, which corresponded with regional analyses showing change with age falling into insignificance towards the sternal extremities of most ribs.

Zonal analysis showed CT.TH loss with age was higher for females than males in all ribs and all zones, but this difference only reached statistical significance when assessing whole rib zones (all ribs), and cutaneous zones (ribs 2, 6-11) along with scattered rib levels for other zones (see markers on Figure 7). Regional results were similarly mixed with only scattered clusters for sex-based differences in the rates of CT.TH loss reaching significance. Across whole rib zones, female CT.TH loss occurred at rates approximately 0.015 mm/decade higher than for males ($p < 0.01$ for each rib). This sex-based rate difference was not uniform across all regions, however, with differential CT.TH loss small (and not significant) along pleural rib aspects and higher (over 0.03 mm/decade, $p < 0.01$) along cutaneous aspects in ribs 6-11.

Generally speaking, zonal regression trend lines (Figure 7) showed that women tended to have thicker cortices than men in the superior and inferior aspects at younger adult ages, and the increased rate of cortical thinning produced a convergence in CT.TH values at older ages with those from men. Conversely, CT.TH along the cutaneous aspect was similar in younger men and women, but the higher rate of thinning in women produced a divergence with age which resulted in thinner cortices in older women than in older men. This phenomenon is further illustrated in Figure 9 showing the main sex effect (after accounting for age*sex interactions) at 20, 55, and 90 years of age. Sex-based differences in CT.TH at 20 years of age generally



Figure 7: CT.TH regression models by age for each rib and zone highlighting cortex thinning with senescence. Predicted CT.TH change per decade is shown for males (blue) and females (red) alongside overall model explanatory power (adjusted R^2 , %). Age was a significant independent predictor of CT.TH in all models ($p < 0.01$). Rates of cortex thinning were significantly higher in females than males in models marked with (*).

Table 1: Predicted cortical thickness values (mm) for males and females at 20 and 90 years of age by rib number and zone

Rib	Sex	Pleural		Cutaneous		Superior		Inferior		Sternal		Whole rib	
		20	90	20	90	20	90	20	90	20	90	20	90
2	F	1.40	0.94	1.08	0.60	0.95	0.45	0.67	0.39	0.54	0.44	0.76	0.51
	M	1.27	1.01	0.93	0.71	0.81	0.54	0.59	0.45	0.45	0.48	0.68	0.56
3	F	1.25	0.79	0.95	0.48	0.88	0.40	0.60	0.34	0.57	0.45	0.75	0.46
	M	1.19	0.89	0.98	0.61	0.76	0.52	0.52	0.37	0.49	0.46	0.71	0.53
4	F	1.33	0.94	1.00	0.52	0.84	0.35	0.60	0.30	0.55	0.43	0.81	0.51
	M	1.31	0.97	1.00	0.64	0.77	0.41	0.53	0.32	0.53	0.47	0.79	0.56
5	F	1.36	1.03	1.04	0.54	0.84	0.35	0.60	0.34	0.55	0.39	0.85	0.54
	M	1.43	1.10	1.04	0.69	0.77	0.36	0.55	0.34	0.57	0.51	0.83	0.62
6	F	1.48	1.13	1.10	0.58	0.86	0.37	0.68	0.39	0.59	0.44	0.90	0.59
	M	1.53	1.25	1.06	0.79	0.78	0.39	0.61	0.43	0.62	0.53	0.88	0.68
7	F	1.46	1.13	1.12	0.65	0.81	0.40	0.66	0.40	0.63	0.50	0.89	0.63
	M	1.51	1.29	1.07	0.87	0.71	0.42	0.57	0.45	0.66	0.57	0.87	0.71
8	F	1.26	0.96	1.07	0.61	0.78	0.41	0.57	0.37	0.60	0.42	0.85	0.57
	M	1.33	1.12	1.05	0.87	0.71	0.43	0.52	0.46	0.63	0.54	0.82	0.69
9	F	1.22	0.90	1.13	0.71	0.82	0.45	0.58	0.39	0.57	0.39	0.84	0.57
	M	1.31	1.12	1.18	1.07	0.77	0.46	0.55	0.46	0.58	0.55	0.83	0.71
10	F	1.22	0.88	1.12	0.70	0.83	0.52	0.56	0.42	0.52	0.37	0.85	0.58
	M	1.24	1.11	1.11	1.17	0.79	0.48	0.51	0.44	0.54	0.51	0.78	0.71
11	F	1.17	0.74	0.83	0.60	0.66	0.43	0.63	0.43	0.44	0.38	0.75	0.51
	M	1.25	0.93	0.94	1.02	0.61	0.45	0.62	0.44	0.46	0.44	0.75	0.64

202 trend towards thicker superior/inferior regions in females and thicker cuta-
 203 neous/pleural regions in males, but none of these differences are statistically
 204 significant at this age apart from small and isolated regions of rib 6. At 55
 205 years, CT.TH reductions result in cutaneous and pleural regional differences
 206 (thinner in females than males) reaching statistical significance across large
 207 and connected portions of most ribs. At this age female ribs still still main-
 208 tain some inferior and superior rib regions that are thicker than males but
 209 this difference remains statistically insignificant. By 90 years of age females
 210 tend to have either thinner or near to equal cortices to males across most of
 211 each rib's surface, with this difference still only significant in some pleural
 212 and cutaneous regions.

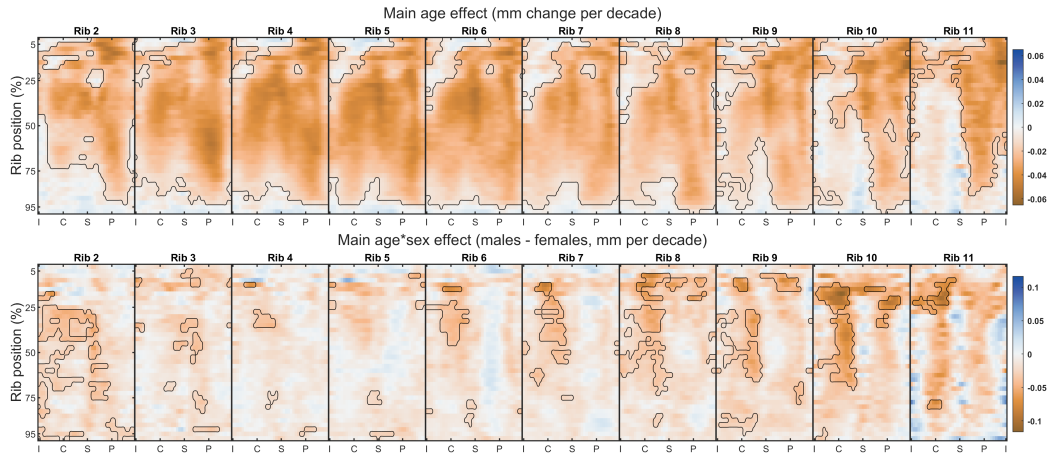


Figure 8: Main age and age*sex effects on regional Ct.Th. Rib surface clusters exhibiting effects significantly different to zero ($p < 0.05$) are delineated by black contours.

Taken across whole ribs, age and sex explained between 22 % (rib 10) and
 214 37 % (rib 2) of the population variability in Ct.Th (Figure 7). Age and sex
 held most explanatory power in superior (average R^2 across all ribs of 29 %)
 216 and cutaneous (avg. $R^2=25$ %) rib regions, whereas associations in pleural,
 inferior, and sternal regions were less strong (avg. R^2 around 12 %).

218 The zonal regression models presented above each included a linear age
 term and an interaction term between age and sex. Inspection of residu-
 220 als from these fitted models did not show trends with subject age, and the
 addition of quadratic regression terms (i.e., squared-age) offered little to no
 222 improvement in adjusted R^2 model explanatory power. This indicates that
 the rate of cortical thinning per decade remained constant. In other words,
 224 while bone content loss was higher for females than for males, the data did
 not suggest an acceleration in this loss with advancing age for either sex.

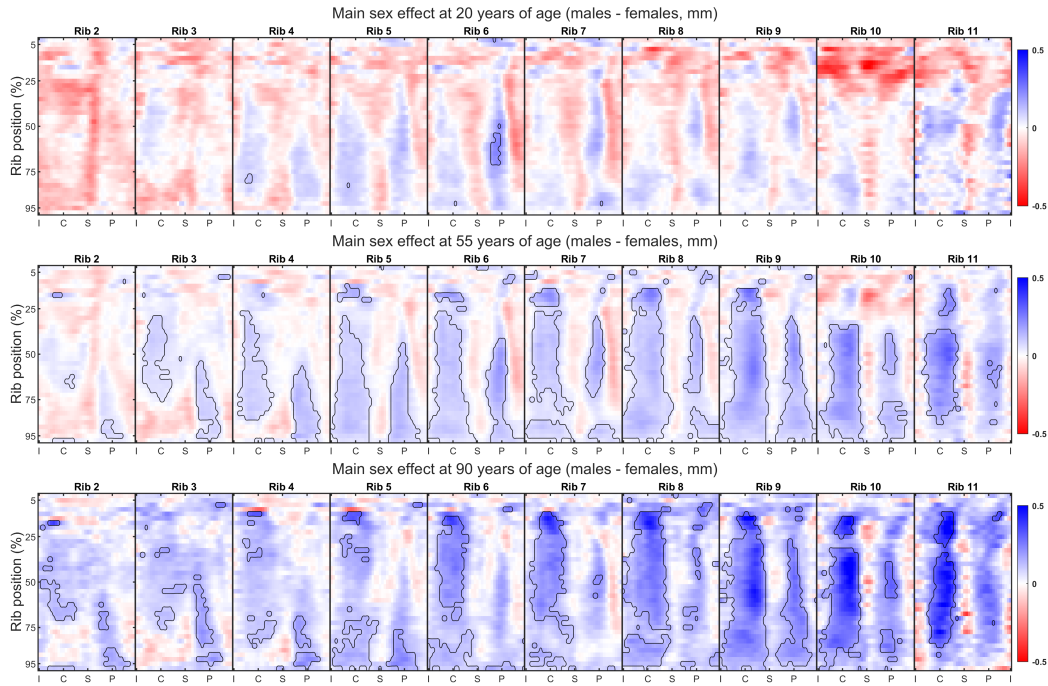


Figure 9: Main sex effects on regional CT.TH at 20, 55, and 90 years of age. Rib surface clusters exhibiting significant differences ($p < 0.05$) are delineated by black contours.

226 The average sixth rib CT.TH map from this study (Figure 5) shared over-
all patterns with a previously published rib 6 thickness map from [Holcombe](#)
228 [et al. \(2019a\)](#). Figure 10 presents a comparison histograms and cumulative
density function plots of all CT.TH values from these two maps. These show
230 current CT.TH results being between 0.02 mm higher (at thinner regions) and
0.08 mm higher (at thicker regions) than the established reference. Given the
232 10 year difference in cohort ages between the two studies (which from [Figure 7](#)
corresponds to between 0.01 mm and 0.06 mm difference in CT.TH),
234 current results are seen to match well with this previously validated study.

Further zonal-based comparison is provided in Figure 11 which shows that
 236 average Ct.TH values found within every zone match - particularly after
 adjustment for cohort age - to within 1 standard deviation as determined by
 238 the current study.

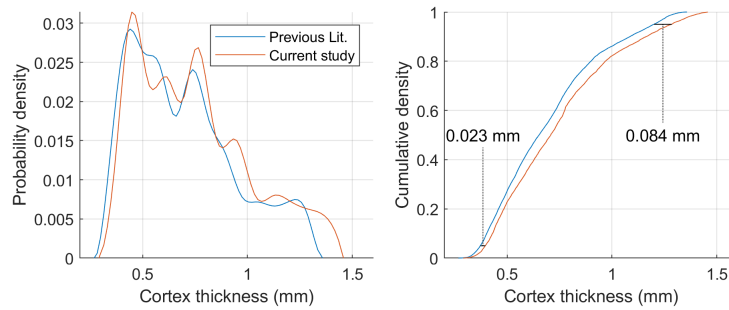


Figure 10: Histogram (left) and cumulative density function (right) of average sixth Ct.TH map values compared to past literature (Holcombe et al., 2019a). The current study shows a thickness increase comparable to that expected from subjects who are on average 10 years younger than the reference cohort.

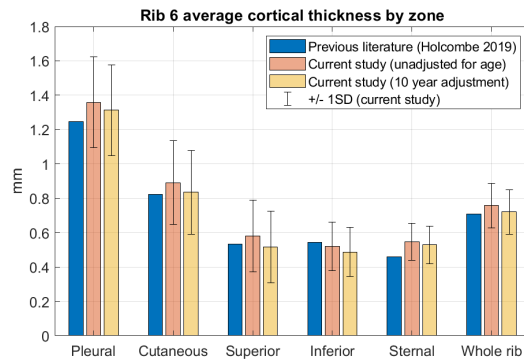


Figure 11: Comparison by zone of average rib 6 Ct.TH in previously validated literature (Holcombe et al., 2019a) to current results.

4. Discussion

240 Here we have assessed cortical bone thickness from over 4,000 ribs of
242 240 adult subjects and analyzed thickness associations with sex, age, and
anatomic location. To the authors knowledge this is the largest subject pool
from which detailed average thickness values have been drawn, and the first
244 to quantify regional rates of bone loss in the ribs with advancing age.

The measurement techniques used in this study are adapted from [Hol-](#)
246 [combe et al. \(2019a\)](#) with additional pre-processing steps to obtain consistent
and registered patch images from live-subject clinical scans, and additional
248 post-processing steps to output smoothed periosteal and endosteal borders.
That previous study used excised sixth ribs scanned at a high resolution
250 ($0.15 \times 0.15 \times 0.67$ mm), and showed mean/sd error of the CBM technique
compared to histological measurements of -0.013 ± 0.167 mm. Results in
252 Figures [10](#) and [11](#) show regional trends and overall CT.TH magnitudes that
are compatible with this previously validated use of CBM methodology, par-
254 ticularly after accounting for population age differences between the two stud-
ies. When contrasting these result differences (usually between 0.01 mm to
256 0.05 mm) to our overall population standard deviation (0.11 mm to 0.26 mm,
[Figure 11](#)) we can be reassured that systematic biases due to methodological
258 factors like changing CT resolutions, smoothing techniques, and scanning of
live subjects are likely small when compared to overall population variance
260 due to individuality. Similarly, previous experimental studies ([Agnew et al.,](#)
[2015, 2018](#); [Kemper et al., 2009](#)) are seen to be compatible with current
262 results having measured average rib thicknesses (albeit aggregated across
multiple ribs and from varying positions along and around those ribs) at

264 pleural, cutaneous, inferior and superior areas to be approximately 1.15 mm,
0.75 mm, 0.43 mm, and 0.46 mm, respectively.

266 Results from Figure 5 show distinct patterns in cortical bone thickness
that differ even between adjacent ribs, particularly for higher ribs 2 and 3. A
268 unique aspect of the second rib is a tuberosity on its superior surface which
forms part of the origin for the serratus anterior muscle which inserts onto
270 the upper part of the scapula as well as the posterior scalene muscle which
connects to cervical vertebrae (Safarini & Bordoni, 2022). A well-established
272 mechanism for bone adaptation is the cyclic forces exerted on muscle origin
and insertion sites from muscle activation, and the regional maxima in rib 2
274 CT.TH values corresponds well with this attachment site. For consistency,
the second rib regional CT.TH maxima (demarcated as pleural zone) was
276 shifted superiorly to match this local rib 2 feature. Overall, all results from
the current study should be taken in context with each rib's muscle attach-
278 ment sites and their potential effect on local bone thickness in mind. In ribs
4-9 the overall patterns in thickness maps were largely consistent albeit with
280 inter-rib variations in CT.TH magnitude. These ribs saw mid-rib maxima at
both pleural and cutaneous aspects and minima along superior and inferior
282 aspects. These ribs also follow largely similar patterns in muscle attach-
ments via the intercostal muscle layers and two or more of the pectoralis
284 minor muscles, external abdominal oblique muscles, and serratus anterior
muscles (De Troyer et al., 2005; Safarini & Bordoni, 2022). It should also
286 be noted that CT.TH measurements along the inferior aspect of a rib can
be complicated by the presence of an elongated costal groove. This inferior
288 elongation was observed between approximately 20-60% along the lengths of

ribs 3-10 with greatest prominence at the 30% location, but showed wide
290 variation both regionally and between subjects. It is commonly thought to
protect the neurovascular bundle running along its deep surface. In the cur-
292 rent study the full periosteal border was used, but in rib patches where this
groove is particularly pronounced the underlying assumption that the cortex
294 is comprised of two approximately concentric borders breaks down. Steps
were taken to discard CT.TH observations crossing the full groove cortex
296 in such cases, but this variation led to greater CT.TH variability along the
mid-rib inferior aspect (Figure 7). Care should be taken when applying rib
298 CT.TH results in these regions to generalized rib geometry as measurements
are likely biased towards those found in subjects with less prominent costal
300 grooves.

A notable result from the current study is that while rates of bone thin-
302 ning varied regionally, they did not do so simply as a percentage of local
thickness. For example, at up to 1.6 mm the average cortices along pleural
304 rib aspects were over twice as thick as those along superior rib aspects, yet
their rates of thinning were lower than those seen along superior and cuta-
306 neous aspects in both men and women. Furthermore, males (who were both
heavier and taller) did not generally possess thicker rib cortices than females
308 except in older cohorts. In fact, in younger cohorts and at some locations
(primarily superior and inferior aspects), female rib cortices tended to be
310 thicker on average than male cortices. This goes some way to explain the
high inter-subject variability and lack of clear trends with age ([Agnew et al.,](#)
312 [2018](#)) and sex ([Holcombe et al., 2019a](#)) that were found in previous studies.

The along-rib registration used in this study is a simple and repeatable

314 normalization of ribs along their curvilinear length. It should be noted
though the potential for systematic misregistration ([Gee & Treece, 2014](#))
316 if ribs of certain population subgroups have topology discordance with this
linear scheme in a systematic way. For example, males or females may sys-
318 tematically differ in the relative along-rib positions of their costal grooves
such that misalignment of this anatomical feature occurs after normalizing
320 by rib length. Similarly, rotational alignment is based partly on the cross-
sectional shape of ribs which may also have systematic differences across the
322 population. While attempts have been made in the current study to pro-
duce repeatable registration procedures to normalize inter-subject anatomy,
324 such systematic misregistration has not been fully investigated and should
be considered when applying the current results.

326 The sex-based, region-based, and age-based differences in CT.TH found
here have implications for future modeling of rib fractures and subsequent
328 thoracic injuries. For example, [Palanca et al. \(2022\)](#) found that ribs with
thicker cortices were more likely to exhibit a brittle break (which can further
330 damage surrounding tissues) rather than buckle during compressive loading.
[Iraeus et al. \(2019\)](#) also found that better cortex definitions offered improve-
332 ments in predicting the force required and resulting locations of rib fractures.
Results here can inform representative sex- or age-specific models and do so
334 with greater detail than has previously been available in full-body HBMs.

It is important to also consider limitations with the present work. Firstly,
336 the study is designed to infer longitudinal changes with age, but does so via
cross-sectional observations of different individuals at various single points
338 during their lifetime. This is a necessary compromise to make given the

absence of appropriate and repeated CT scans available from healthy subjects
340 across spans of many decades. Secondly, the adult cohort was drawn from a
Midwestern US population, so there was limited ability to explore potential
342 variation associated with subject ancestry. We also chose to exclude the first
and twelfth ribs from the current analysis. While the first rib is important
344 and plays a key role in interaction with safety systems, its morphology is
entirely distinct from other ribs and does not directly lend itself to the same
346 registration techniques used here so should be addressed separately. Twelfth
ribs were excluded due to their small but varied size, and they are also
348 not thought to play a substantial structural role during loading from blunt
trauma events.

350 5. Conclusion

Here we have applied a cortical bone mapping methodology to ribs in
352 clinical CT scans taken from a US adult population of broadly sampled ages.
The resulting maps of cortical thickness across the surfaces of ribs 2-11 can
354 be directly applied to improve the biofidelity of current finite element hu-
man body models. Results also highlight the regional variation in cortical
356 bone thinning that occurs with advancing age, allowing for further specifica-
tion of such models to represent males or females across full adult lifespans.
358 Given appropriate CT availability, the techniques used in this study can fur-
ther be applied clinically to assess specific rib bone characteristics and their
360 relationships with injury risk, disease progression, or therapy response.

Disclosures

362 The authors report that there are no conflicts of interest which might
affect this work. The anonymized and retrospective scan data used in this
364 study was obtained under IRB HUM00041441.

Data Availability Statement

366 The data that supports the findings of this study are available in the
supplementary material of this article.

References

368 Agnew, A. M., Murach, M. M., Dominguez, V. M., Sreedhar, A., Misicka,
370 E., Harden, A., Bolte, J. H., Kang, Y.-S., Stammen, J., & Moorhouse, K.
(2018). Sources of variability in structural bending response of pediatric
372 and adult human ribs in dynamic frontal impacts. *Stapp car crash journal*,
62. Tex.citeulike-article-id: 14648756 tex.posted-at: 2018-10-27 04:59:47
374 tex.priority: 2.

Agnew, A. M., Schafman, M., Moorhouse, K., White, S. E., & Kang,
376 Y.-S. (2015). The effect of age on the structural properties of human
ribs. *Journal of the Mechanical Behavior of Biomedical Materials*, *41*,
378 302–314. URL: <http://dx.doi.org/10.1016/j.jmbbm.2014.09.002>.
doi:10.1016/j.jmbbm.2014.09.002. Tex.citeulike-article-id: 13692594
380 tex.citeulike-linkout-0: <http://dx.doi.org/10.1016/j.jmbbm.2014.09.002>
tex.posted-at: 2015-08-01 19:49:00 tex.priority: 4.

- 382 Alswat, K. A. (2017). Gender Disparities in Osteoporosis. *Journal of Clinical
384 Medicine Research*, 9, 382–387. URL: [http://www.jocmr.org/index.
php/JOCMR/article/view/2970](http://www.jocmr.org/index.php/JOCMR/article/view/2970). doi:10.14740/jocmr2970w.
- Chen, H. (2014). Bone three-dimensional microstructural features of the
386 common osteoporotic fracture sites. *World Journal of Orthopedics*, 5,
486. URL: <http://www.wjgnet.com/2218-5836/full/v5/i4/486.htm>.
388 doi:10.5312/wjo.v5.i4.486.
- Chen, H., Poulard, D., Forman, J., Crandall, J., & Panzer, M. B. (2018).
390 Evaluation of geometrically personalized THUMS pedestrian model re-
sponse against sedan–pedestrian PMHS impact test data. *Traffic Injury
392 Prevention*, 19, 542–548. URL: [https://www.tandfonline.com/doi/
full/10.1080/15389588.2018.1450979](https://www.tandfonline.com/doi/full/10.1080/15389588.2018.1450979). doi:10.1080/15389588.2018.
394 1450979.
- Choi, H.-Y., & Kwak, D.-S. (2011). Morphologic characteristics of ko-
396 rean elderly rib. *Journal of Automotive Safety and Energy*, 2, 112–
127. Tex.citeulike-article-id: 14362451 tex.posted-at: 2017-05-24 20:17:20
398 tex.priority: 2.
- De Troyer, A., Kirkwood, P. A., & Wilson, T. A. (2005). Respira-
400 tory Action of the Intercostal Muscles. *Physiological Reviews*, 85,
717–756. URL: [https://www.physiology.org/doi/10.1152/physrev.
402 00007.2004](https://www.physiology.org/doi/10.1152/physrev.00007.2004). doi:10.1152/physrev.00007.2004.
- Dogrul, B. N., Kiliccalan, I., Ascı, E. S., & Peker, S. C. (2020).
404 Blunt trauma related chest wall and pulmonary injuries: An overview.

- 406 *Chinese Journal of Traumatology*, 23, 125–138. URL: <https://linkinghub.elsevier.com/retrieve/pii/S1008127520301103>. doi:10.1016/j.cjtee.2020.04.003.
- 408 Eftekhari-Sadat, B., Ghavami, M., Toopchizadeh, V., & Ghahvechi Akbari, M. (2016). Wrist bone mineral density utility in diagnosing hip osteoporosis in postmenopausal women. *Therapeutic Advances in Endocrinology and Metabolism*, 7, 207–211. URL: <http://journals.sagepub.com/doi/10.1177/2042018816658164>. doi:10.1177/2042018816658164.
- 414 Folch-Fortuny, A., Arteaga, F., & Ferrer, A. (2016). Missing Data Imputation Toolbox for MATLAB. *Chemometrics and Intelligent Laboratory Systems*, 154, 93–100. URL: <https://linkinghub.elsevier.com/retrieve/pii/S0169743916300557>. doi:10.1016/j.chemolab.2016.03.019.
- 418 Forman, J., Poplin, G. S., Shaw, C. G., McMurry, T. L., Schmidt, K., Ash, J., & Sunnevang, C. (2019). Automobile injury trends in the contemporary fleet: Belted occupants in frontal collisions. *Traffic Injury Prevention*, 20, 607–612. URL: <https://www.tandfonline.com/doi/full/10.1080/15389588.2019.1630825>. doi:10.1080/15389588.2019.1630825.
- 422 Gee, A. H., & Treece, G. M. (2014). Systematic misregistration and the statistical analysis of surface data. *Medical Image Analysis*, 18, 385–393. URL: <https://linkinghub.elsevier.com/retrieve/pii/S1361841513001783>. doi:10.1016/j.media.2013.12.007.
- 426 Holcombe, S. A., Agnew, A. M., Derstine, B., & Wang, S. C. (2020). Comparing FE human body model rib geometry to

428 population data. *Biomechanics and Modeling in Mechanobiology*, 19, 2227–2239. URL: <https://link.springer.com/10.1007/s10237-020-01335-2>. doi:10.1007/s10237-020-01335-2.

430
Holcombe, S. A., Hwang, E., Derstine, B. A., & Wang, S. C. (2018). Measuring rib cortical bone thickness and cross section from CT. *Medical Image Analysis*, 49, 27–34. URL: <http://dx.doi.org/10.1016/j.media.2018.07.003>. doi:10.1016/j.media.2018.07.003. Tex.citeulike-article-id: 14629449 tex.citeulike-linkout-0: <http://dx.doi.org/10.1016/j.media.2018.07.003> tex.posted-at: 2018-08-26 14:53:34 tex.priority: 2.

438 Holcombe, S. A., Kang, Y., Derstine, B. A., Wang, S. C., & Agnew, A. M. (2019a). Regional maps of rib cortical bone thickness and cross-sectional geometry. *Journal of Anatomy*, 235, 883–891. URL: <https://onlinelibrary.wiley.com/doi/10.1111/joa.13045>. doi:10.1111/joa.13045.

440
Holcombe, S. A., Kang, Y.-S. S., Wang, S. C., & Agnew, A. M. (2019b). The accuracy of local rib bone geometry measurement using full body ct images. *International Research Council On the Biomechanics of Injury*, 19, 64.

448
Holcombe, S. A., Wang, S. C., & Grotberg, J. B. (2017). The effect of age and demographics on rib shape. *Journal of Anatomy*, 231, 229–247. URL: <http://dx.doi.org/10.1111/joa.12632>. doi:10.1111/joa.12632. Tex.citeulike-article-id: 14416505 tex.citeulike-linkout-

0: <http://dx.doi.org/10.1111/joa.12632> tex.posted-at: 2017-08-20 20:30:18
452 tex.priority: 2.

Hwang, E., Hu, J., & Reed, M. P. (2020). Validating diverse human body models against side impact tests with post-mortem human subjects. *Journal of Biomechanics*, *98*, 109444. URL: <https://linkinghub.elsevier.com/retrieve/pii/S0021929019306918>. doi:10.1016/j.jbiomech.2019.109444.

Iraeus, J., Lundin, L., Storm, S., Agnew, A., Kang, Y.-S., Kemper, A., Albert, D., Holcombe, S., & Pipkorn, B. (2019). Detailed subject-specific FE rib modeling for fracture prediction. *Traffic Injury Prevention*, *20*, S88–S95. URL: <https://www.tandfonline.com/doi/full/10.1080/15389588.2019.1665649>. doi:10.1080/15389588.2019.1665649.

Kemper, A. R., McNally, C., Kennedy, E. A., Manoogian, S. J., Rath, A. L., Ng, T. P., Stitzel, J. D., Smith, E. P., Duma, S. M., & Matsuoka, F. (2005). Material properties of human rib cortical bone from dynamic tension coupon testing. *Stapp Car Crash Journal*, *49*, 199–230.

Kemper, A. R., McNally, C., Pullins, C. A., Freeman, L. J., Duma, S. M., & Rouhana, S. M. (2007). The biomechanics of human ribs: material and structural properties from dynamic tension and bending tests. *Stapp Car Crash Journal*, *51*, 235–273. URL: <http://view.ncbi.nlm.nih.gov/pubmed/18278600>. Tex.citeulike-article-id: 14127065 tex.citeulike-linkout-0: <http://view.ncbi.nlm.nih.gov/pubmed/18278600> tex.citeulike-linkout-1: <http://www.hubmed.org/display.cgi?uids=18278600> tex.posted-at: 2016-08-30 18:14:59 tex.priority: 2.

- 476 Kemper, A. R., Stitzel, J. D., McNally, C., Gabler, H. C., & Duma,
S. M. (2009). Biomechanical response of the human clavicle: The ef-
fects of loading direction on bending properties. *Journal of Applied*
478 *Biomechanics*, *25*, 165–174. URL: [http://dx.doi.org/10.1123/jab.
25.2.165](http://dx.doi.org/10.1123/jab.25.2.165). doi:10.1123/jab.25.2.165. Tex.citeulike-article-id: 14347407
480 tex.citeulike-linkout-0: <http://dx.doi.org/10.1123/jab.25.2.165> tex.posted-
at: 2017-05-01 16:57:43 tex.priority: 2.
- 482 Li, Z., Kindig, M., Subit, D., & Kent, R. (2010). Development of finite
element model of 50th percentile male using multiblock hex meshing ap-
484 proach. In *Proc. 6th annual world congress on biomechanics*. Tex.citeulike-
article-id: 13345550 tex.posted-at: 2014-09-03 16:57:47 tex.priority: 2.
- 486 Mohr, M., Abrams, E., Engel, C., Long, W. B., & Bottlang, M. (2007).
Geometry of human ribs pertinent to orthopedic chest-wall reconstruc-
488 tion. *Journal of Biomechanics*, *40*, 1310–1317. URL: [http://dx.
doi.org/10.1016/j.jbiomech.2006.05.017](http://dx.doi.org/10.1016/j.jbiomech.2006.05.017). doi:10.1016/j.jbiomech.
490 [2006.05.017](http://dx.doi.org/10.1016/j.jbiomech.2006.05.017). Tex.citeulike-article-id: 13345564 tex.citeulike-linkout-0:
<http://dx.doi.org/10.1016/j.jbiomech.2006.05.017> tex.posted-at: 2014-09-
492 03 16:57:47 tex.priority: 2.
- Murach, M. M., Kang, Y.-S., Goldman, S. D., Schafman, M. A., Schlecht,
494 S. H., Moorhouse, K., Bolte, J., & Agnew, A. M. (2017). Rib ge-
ometry explains variation in dynamic structural response: Potential
496 implications for frontal impact fracture risk. *Annals of biomedical
engineering*, (pp. 1–15). URL: [http://dx.doi.org/10.1007/
498 s10439-017-1850-4](http://dx.doi.org/10.1007/s10439-017-1850-4). doi:10.1007/s10439-017-1850-4. Publisher:

Springer US tex.citeulike-article-id: 14415361 tex.citeulike-linkout-0:
500 <http://dx.doi.org/10.1007/s10439-017-1850-4> tex.citeulike-linkout-1:
<http://link.springer.com/article/10.1007/s10439-017-1850-4> tex.posted-
502 at: 2017-08-17 20:48:30 tex.priority: 2.

Palanca, M., Liebsch, C., Hübner, S., Marras, D., Ruspi, M. L., Mar-
504 cono, F., Cristofolini, L., & Wilke, H.-J. (2022). Global and local
characterization explains the different mechanisms of failure of the hu-
506 man ribs. *Journal of the Mechanical Behavior of Biomedical Materials*,
125, 104931. URL: [https://linkinghub.elsevier.com/retrieve/pii/
508 S1751616121005622](https://linkinghub.elsevier.com/retrieve/pii/S1751616121005622). doi:10.1016/j.jmbbm.2021.104931.

Pignolo, R. J., Law, S. F., & Chandra, A. (2021). Bone Aging, Cellular Senes-
510 cence, and Osteoporosis. *JBMR Plus*, *5*. URL: [https://onlinelibrary.
wiley.com/doi/10.1002/jbm4.10488](https://onlinelibrary.wiley.com/doi/10.1002/jbm4.10488). doi:10.1002/jbm4.10488.

Pipkorn, B., Iraeus, J., Lindkvist, M., Puthan, P., & Bunketorp, O. (2020).
512 Occupant injuries in light passenger vehicles—A NASS study to enable
priorities for development of injury prediction capabilities of human body
514 models. *Accident Analysis & Prevention*, *138*, 105443. URL: [https://
516 linkinghub.elsevier.com/retrieve/pii/S000145751930377X](https://linkinghub.elsevier.com/retrieve/pii/S000145751930377X). doi:10.
1016/j.aap.2020.105443.

Poole, K. E. S., Treece, G. M., Mayhew, P. M., Vaculík, J., Dungal, P., Horák,
518 M., Štěpán, J. J., & Gee, A. H. (2012). Cortical Thickness Mapping to
Identify Focal Osteoporosis in Patients with Hip Fracture. *PLoS ONE*, *7*,
520 e38466. URL: <https://dx.plos.org/10.1371/journal.pone.0038466>.
doi:10.1371/journal.pone.0038466.
522

Safarini, O. A., & Bordoni, B. (2022). Anatomy, Thorax, Ribs. In *StatPearls*.
524 Treasure Island (FL): StatPearls Publishing. URL: <http://www.ncbi.nlm.nih.gov/books/NBK538328/>.

526 Schoell, S. L., Weaver, A. A., Vavalle, N. A., & Stitzel, J. D.
(2015). Age- and Sex-Specific thorax finite element model de-
528 velopment and simulation. *Traffic Injury Prevention*, *16*, S57–
S65. URL: <http://dx.doi.org/10.1080/15389588.2015.1005208>.
530 doi:10.1080/15389588.2015.1005208. Publisher: Taylor &
Francis tex.citeulike-article-id: 14232241 tex.citeulike-linkout-0:
532 <http://dx.doi.org/10.1080/15389588.2015.1005208> tex.citeulike-linkout-1:
<http://www.tandfonline.com/doi/abs/10.1080/15389588.2015.1005208>
534 tex.posted-at: 2016-12-22 23:04:48 tex.priority: 2.

Shi, X., Cao, L., Reed, M. P., Rupp, J. D., Hoff, C. N., &
536 Hu, J. (2014). A statistical human rib cage geometry model ac-
counting for variations by age, sex, stature and body mass in-
538 dex. *Journal of Biomechanics*, *47*, 2277–2285. URL: <http://dx.doi.org/10.1016/j.jbiomech.2014.04.045>. doi:10.1016/j.jbiomech.
540 [2014.04.045](http://dx.doi.org/10.1016/j.jbiomech.2014.04.045). Tex.citeulike-article-id: 13679509 tex.citeulike-linkout-0:
<http://dx.doi.org/10.1016/j.jbiomech.2014.04.045> tex.posted-at: 2015-07-
542 21 15:35:56 tex.priority: 2.

Sirmali, M., Türüt, H., Topçu, S., Gülhan, E., Yazici, U., Kaya, S., &
544 Taştepe, I. (2003). A comprehensive analysis of traumatic rib frac-
tures: morbidity, mortality and management. *European journal of cardio-*
546 *thoracic surgery*, *24*, 133–138. URL: <http://view.ncbi.nlm.nih.gov/>

pubmed/12853057. Tex.citeulike-article-id: 14358150 tex.citeulike-linkout-
548 0: <http://view.ncbi.nlm.nih.gov/pubmed/12853057> tex.citeulike-linkout-
1: <http://www.hubmed.org/display.cgi?uids=12853057> tex.posted-at:
550 2017-05-16 20:38:13 tex.priority: 2.

Sozen, T., Ozisik, L., & Calik Basaran, N. (2017). An
552 overview and management of osteoporosis. *European Journal
of Rheumatology*, 4, 46–56. URL: [https://eurjrheumatol.org/
554 /en/an-overview-and-management-of-osteoporosis-132921](https://eurjrheumatol.org/en/an-overview-and-management-of-osteoporosis-132921).
doi:10.5152/eurjrheum.2016.048.

556 Stawicki, S. P., Grossman, M. D., Hoey, B. A., Miller, D. L., & Reed, J. F.
(2004). Rib fractures in the elderly: A marker of injury severity. *Journal
558 of the American Geriatrics Society*, 52, 805–808. URL: [http://dx.doi.
org/10.1111/j.1532-5415.2004.52223.x](http://dx.doi.org/10.1111/j.1532-5415.2004.52223.x) doi:10.1111/j.1532-5415.
560 2004.52223.x. Tex.citeulike-article-id: 14649061 tex.citeulike-linkout-0:
<http://dx.doi.org/10.1111/j.1532-5415.2004.52223.x> tex.posted-at: 2018-
562 10-29 01:08:30 tex.priority: 2.

Talbot, B. S., Gange, C. P., Chaturvedi, A., Klionsky, N., Hobbs, S. K.,
564 & Chaturvedi, A. (2017). Traumatic Rib Injury: Patterns, Imaging Pit-
falls, Complications, and Treatment. *RadioGraphics*, 37, 628–651. URL:
566 <http://pubs.rsna.org/doi/10.1148/rg.2017160100>. doi:10.1148/rg.
2017160100.

568 Telfer, S., Brunnquell, C. L., Allen, J. D., Linnau, K. F., Zamora, D., &
Kleweno, C. P. (2021). The effect of age and sex on pelvic bone density
570 measured opportunistically in clinical CT scans. *Journal of Orthopaedic*

572 *Research*, 39, 485–492. URL: <https://onlinelibrary.wiley.com/doi/10.1002/jor.24792>. doi:10.1002/jor.24792.

574 Treece, G. M., & Gee, A. H. (2015). Independent measurement of femoral cortical thickness and cortical bone density using clinical CT. *Medical Image Analysis*, 20, 249–264. URL: <http://dx.doi.org/10.1016/j.media.2014.11.012>. doi:10.1016/j.media.2014.11.012. Tex.citeulike-article-id: 14346480 tex.citeulike-linkout-0: <http://dx.doi.org/10.1016/j.media.2014.11.012> tex.posted-at: 2017-04-28 19:31:52 tex.priority: 2.

580 Vavalle, N. A., Schoell, S. L., Weaver, A. A., Stitzel, J. D., & Gayzik, F. S. (2014). Application of Radial Basis Function Methods in the Development of a 95th Percentile Male Seated FEA Model. *Stapp Car Crash Journal*, 58, 361–384.

584 Witt, C. E., & Bulger, E. M. (2017). Comprehensive approach to the management of the patient with multiple rib fractures: a review and introduction of a bundled rib fracture management protocol. *Trauma Surgery & Acute Care Open*, 2, e000064. URL: <https://tsaco.bmj.com/lookup/doi/10.1136/tsaco-2016-000064>. doi:10.1136/tsaco-2016-000064.

590 Worsley, K., Taylor, J., Carbonell, F., Chung, M., Duerden, E., Bernhardt, B., Lyttelton, O., Boucher, M., & Evans, A. (2009). SurfStat: A Matlab toolbox for the statistical analysis of univariate and multivariate surface and volumetric data using linear mixed effects models and random field theory. *NeuroImage*, 47, S102. URL: <https://>

594 linkinghub.elsevier.com/retrieve/pii/S1053811909708821. doi:10.1016/S1053-8119(09)70882-1.

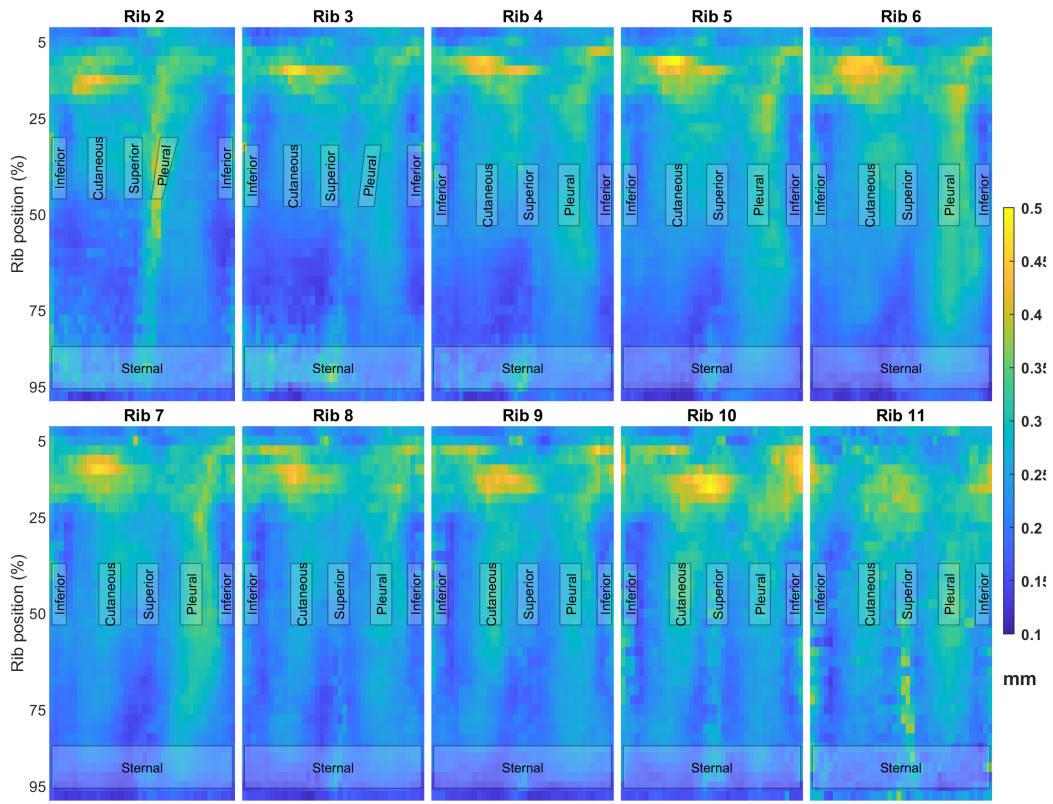
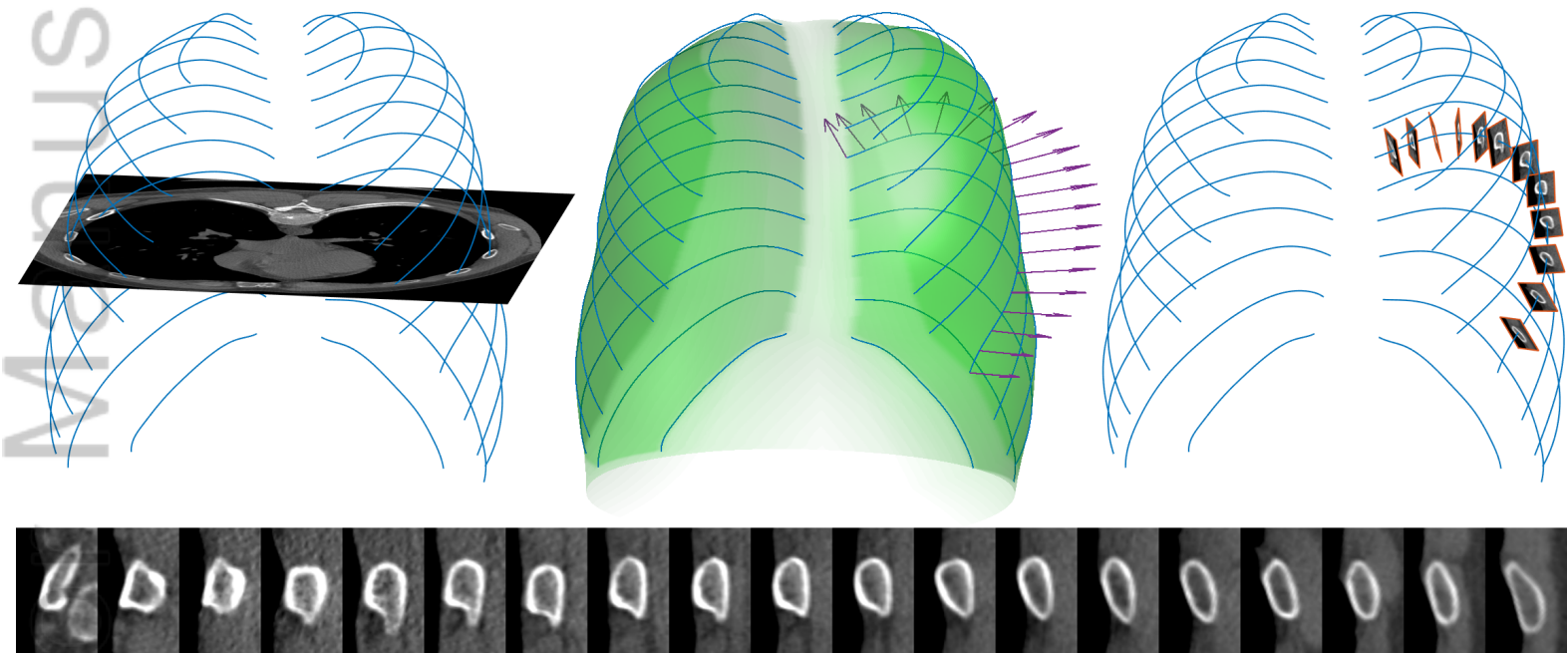
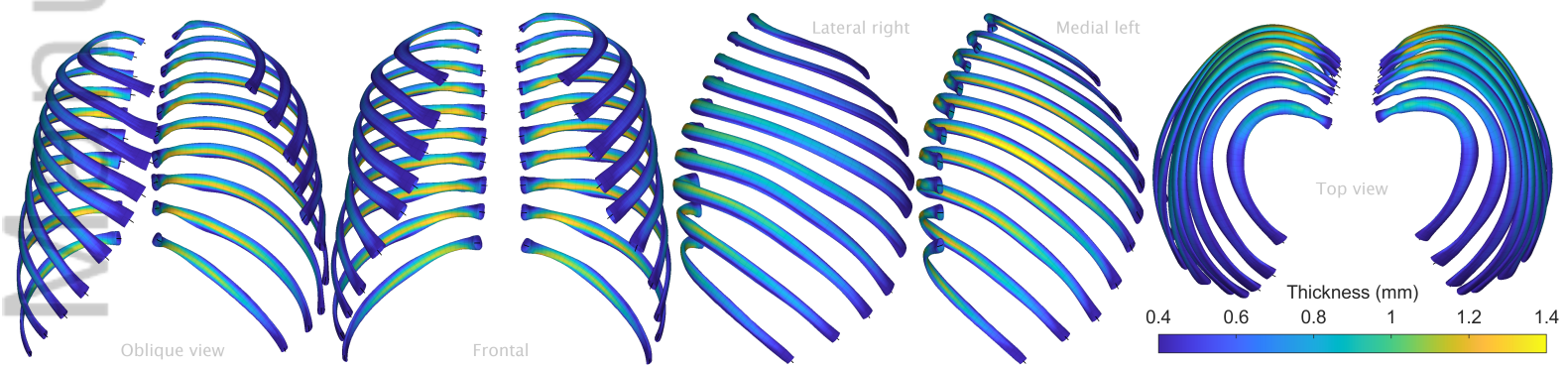


Figure A.1: Cortical thickness standard deviation maps for ribs 2-11.

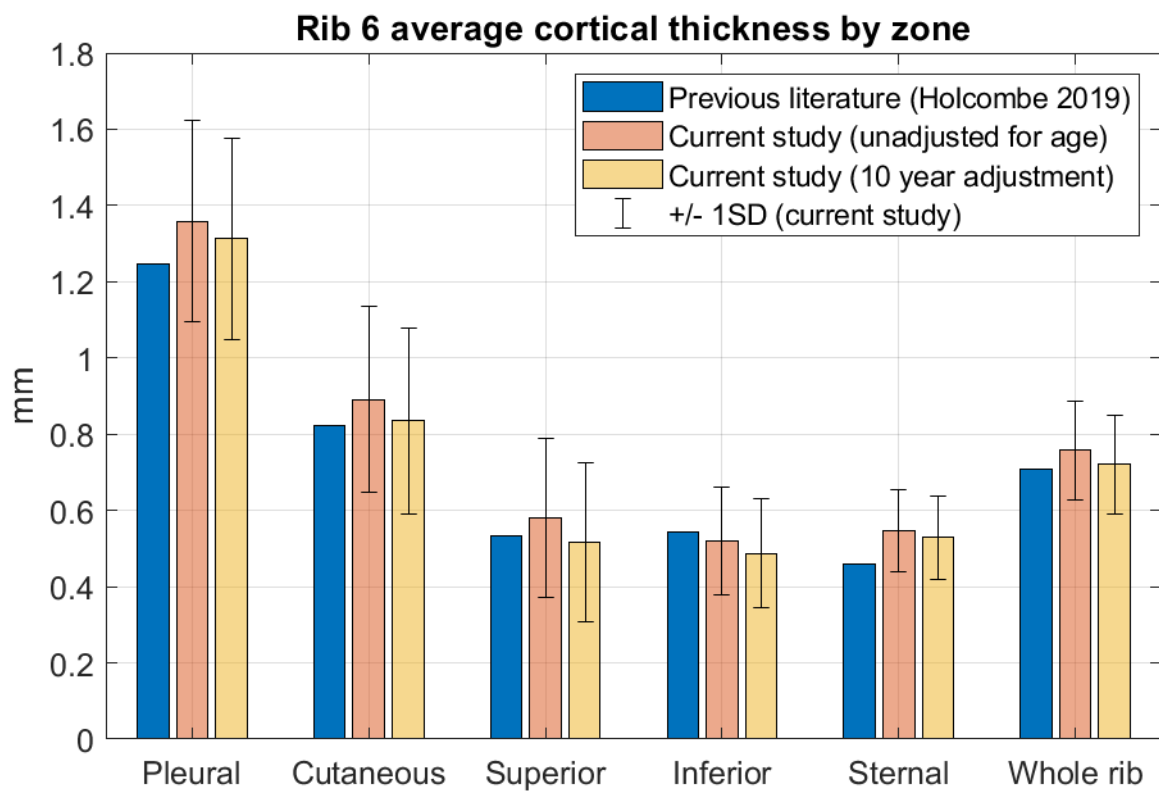
596 Appendix



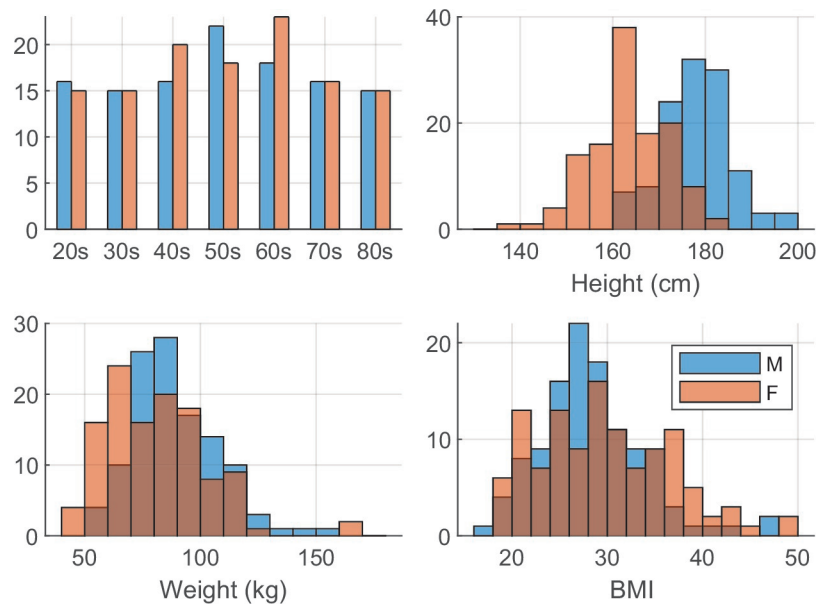
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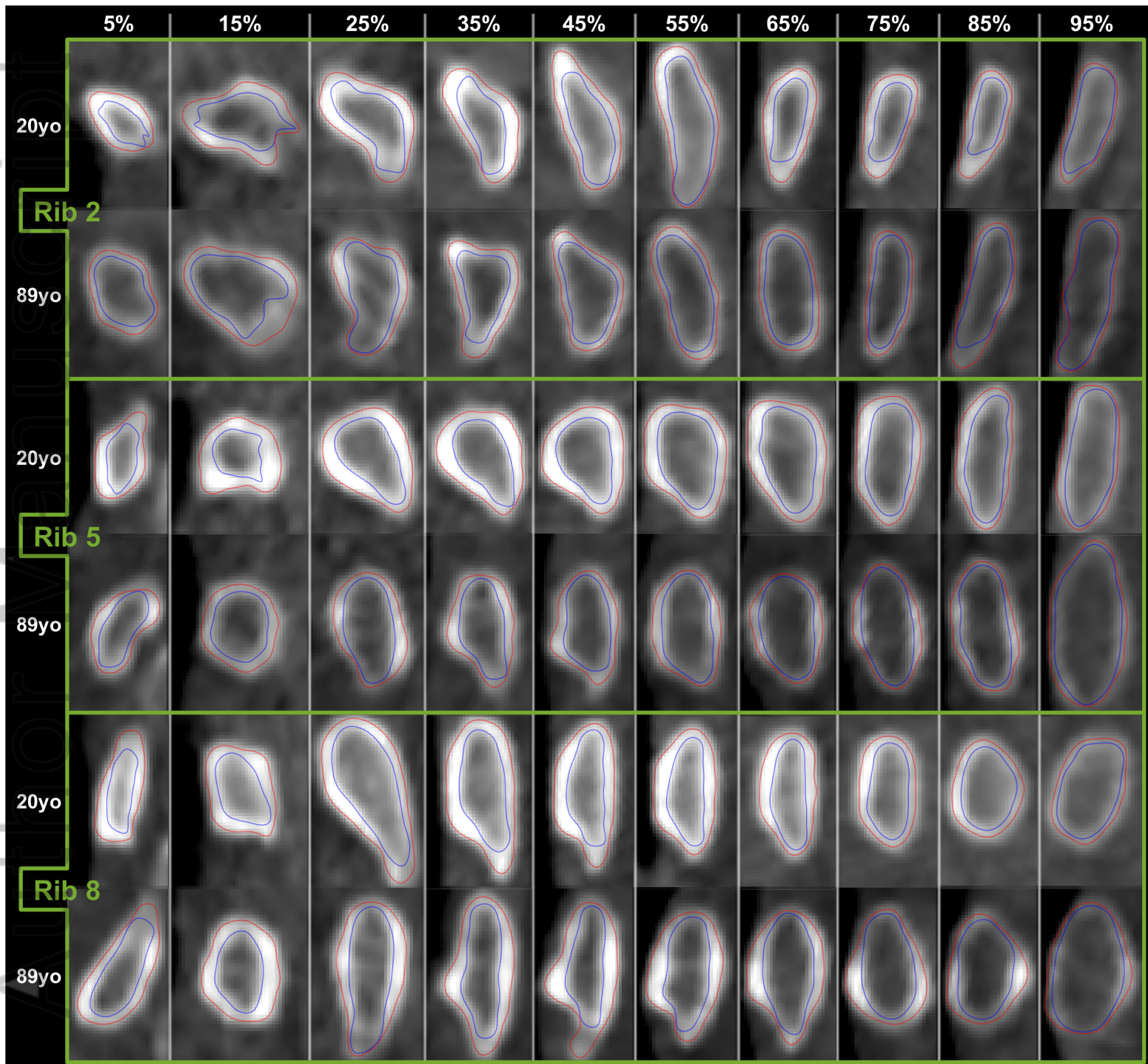
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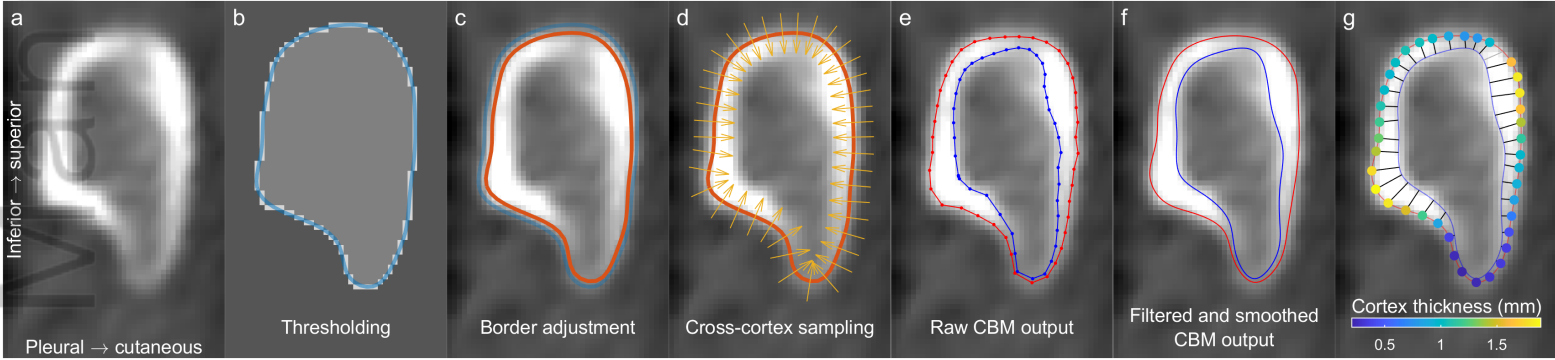
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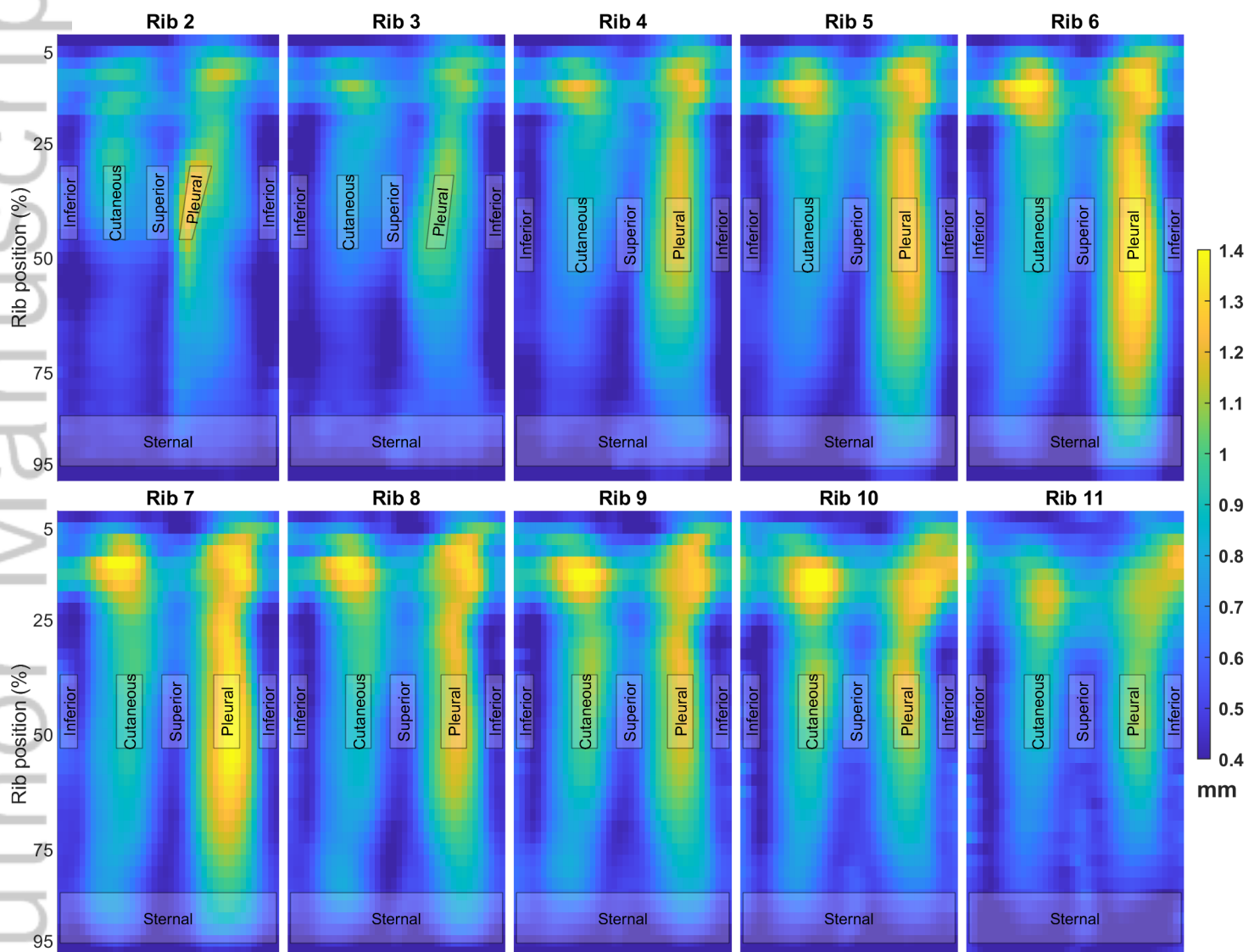
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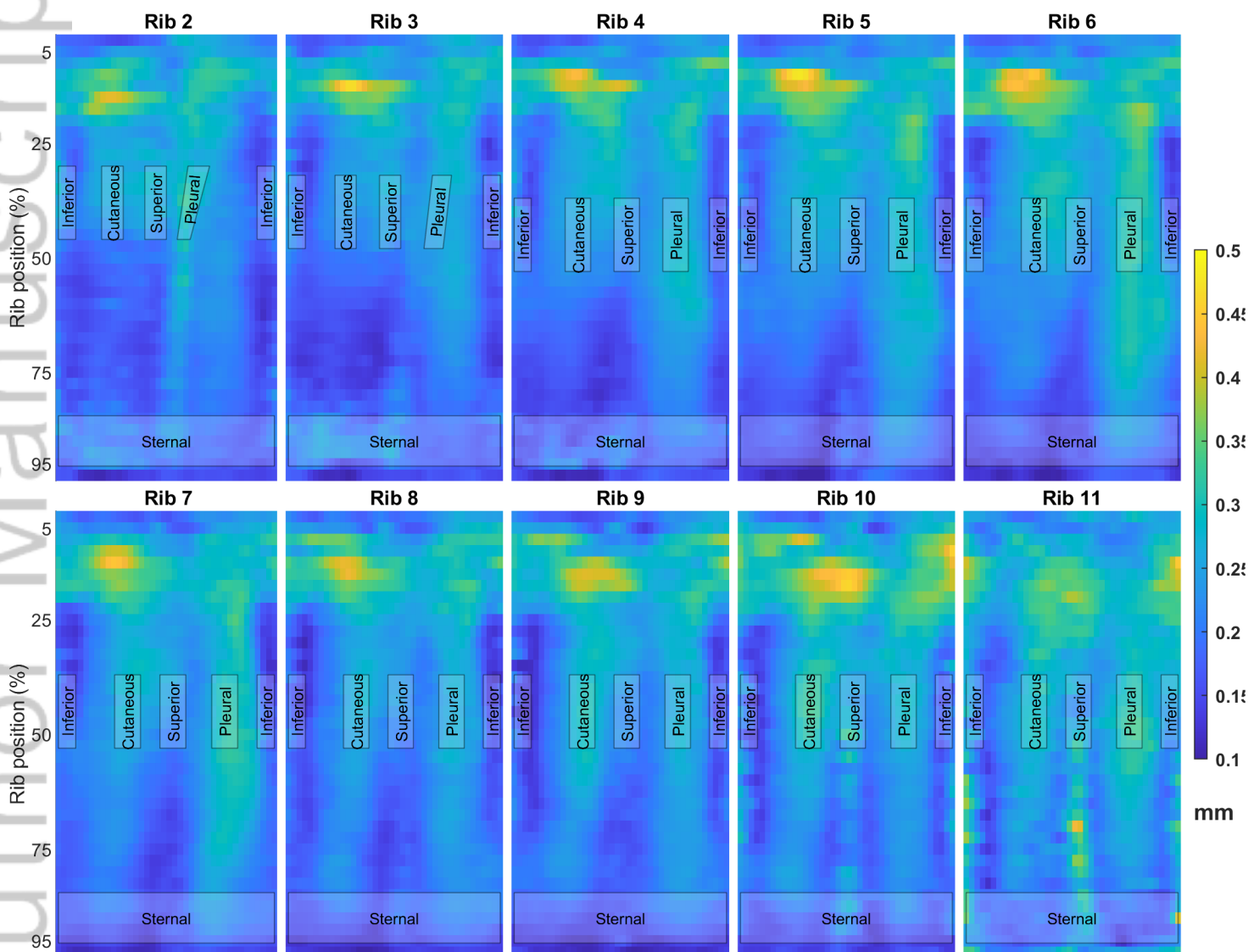
JOA_13751_FIG_imProcSteps.tif



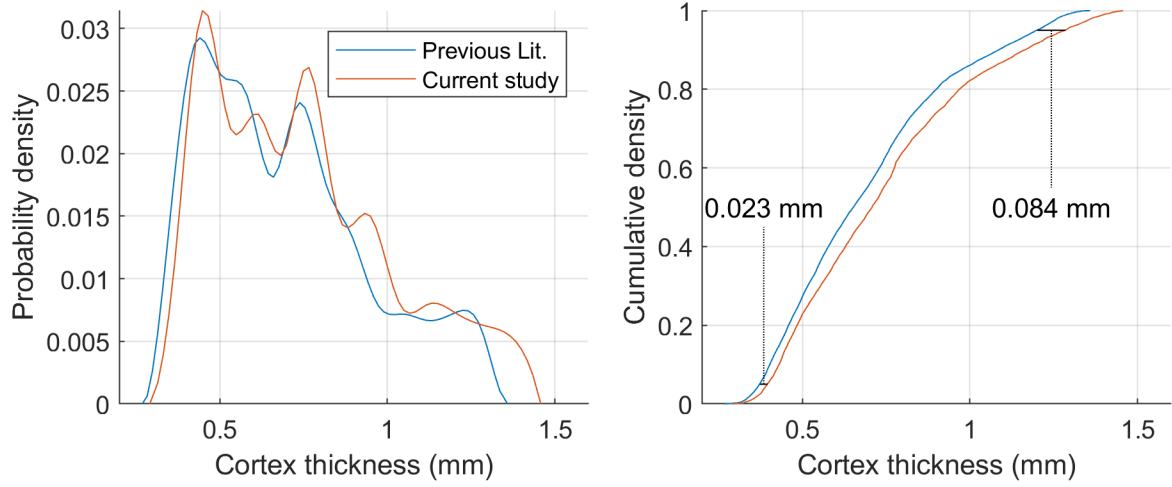
joa_13751_fig_regressionsbyzonetoage.eps



JOA_13751_FIG_ribZonesExplanation_mean.tif

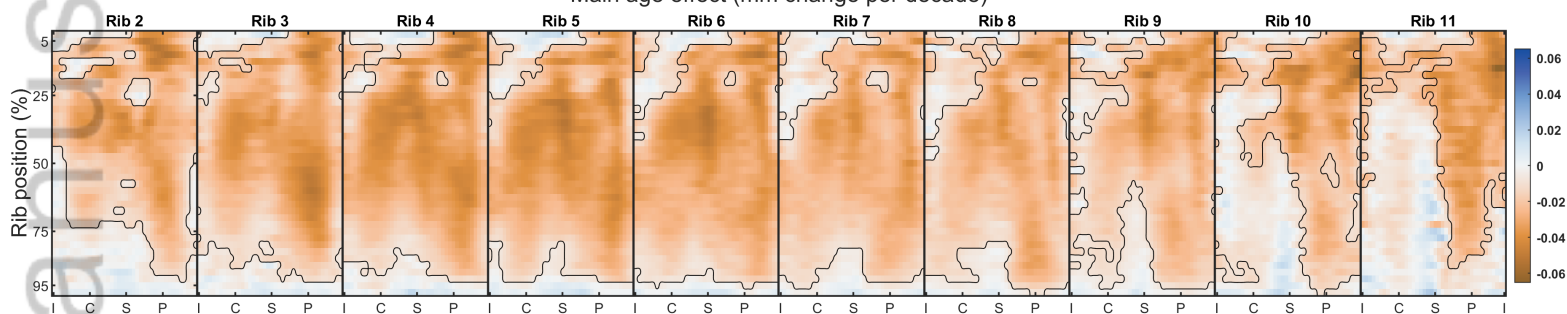


JOA_13751_FIG_ribZonesExplanation_std.tif

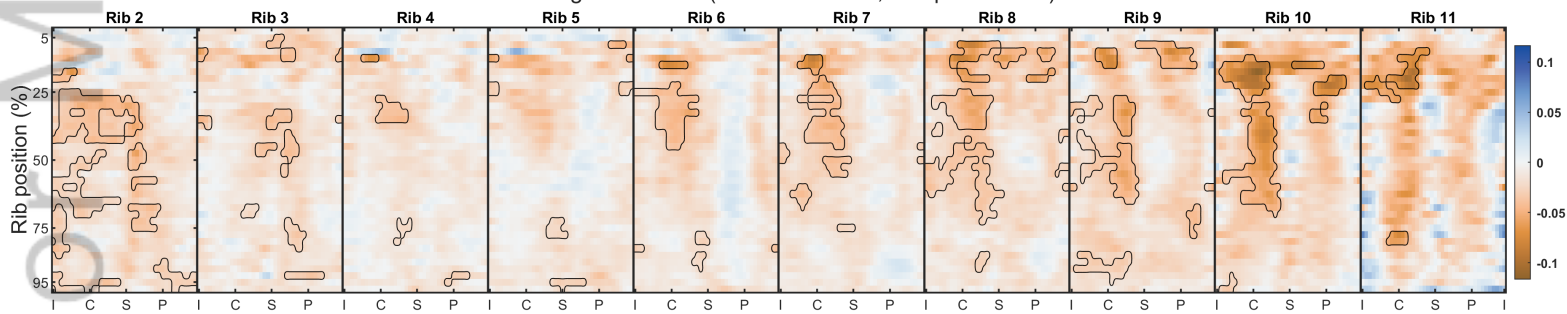


JOA_13751_FIG_spectralLitComparison.tif

Main age effect (mm change per decade)



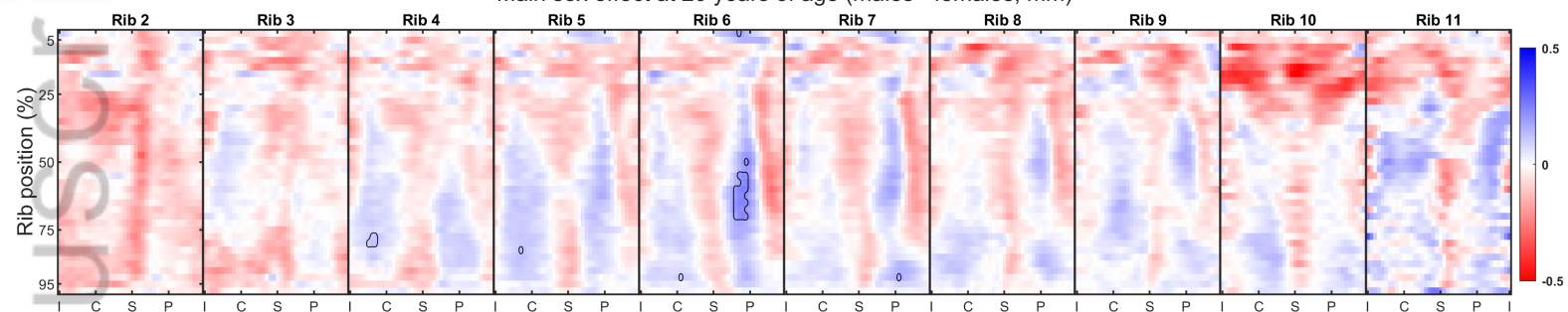
Main age*sex effect (males - females, mm per decade)



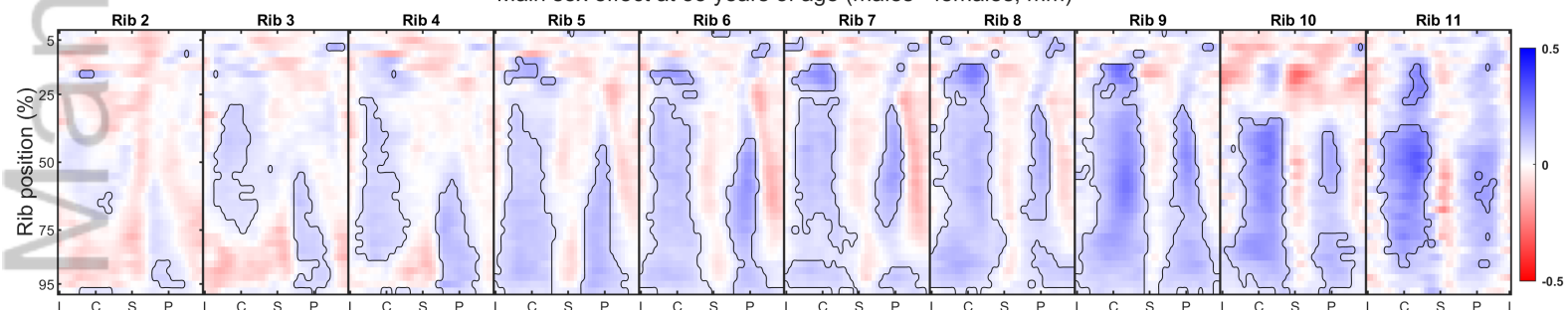
JOA_13751_FIG_surfStatEffect_FIN_age.tif

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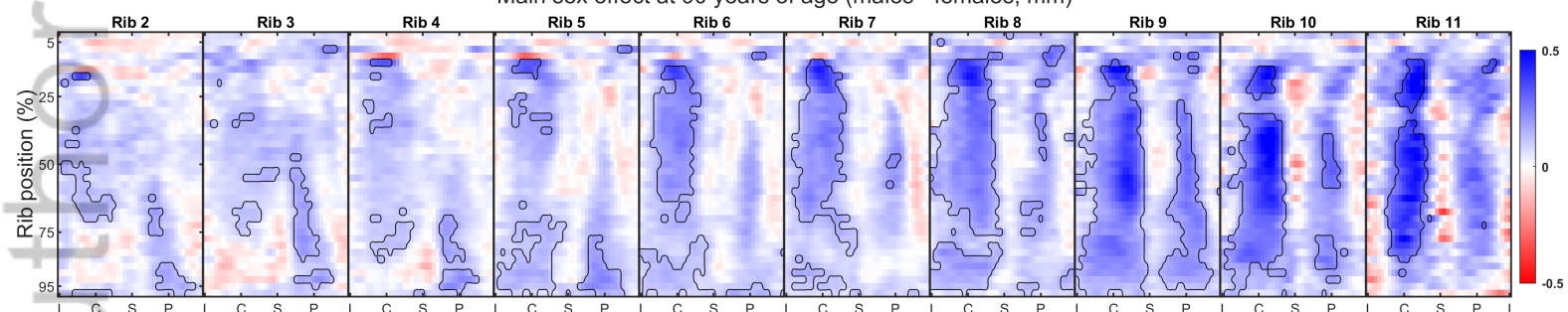
Main sex effect at 20 years of age (males - females, mm)



Main sex effect at 55 years of age (males - females, mm)



Main sex effect at 90 years of age (males - females, mm)



JOA_13751_FIG_surfStatEffect_FIN_sex.tif