

Motivation

- Prosthesis currently on the market and described in literature have struggled to match human muscle performance. This is due to a variety of factors including torque density, weight, and speed capabilities [1].
- Electroadhesive devices provide a light weight, low power, modulated actuation solution for a variety of applications to improve the performance of prostheses.
- Due to their configurability in size and shape, electroadhesives can be readily implemented in many different prosthesis architectures.

State of the Art

- Electroadhesives are currently used in a variety of applications, including haptics, tactile displays, and grippers.
- The best performing electroadhesive in terms of force density [3]:
 - Shear force density: 210kPa
 - Operating voltage: 300V
 - Parallel plate configuration.
- Another notable configuration is the interdigitated electrode geometry [4]:
 - Shear force density: 33kPa
 - Operating voltage: 1kV

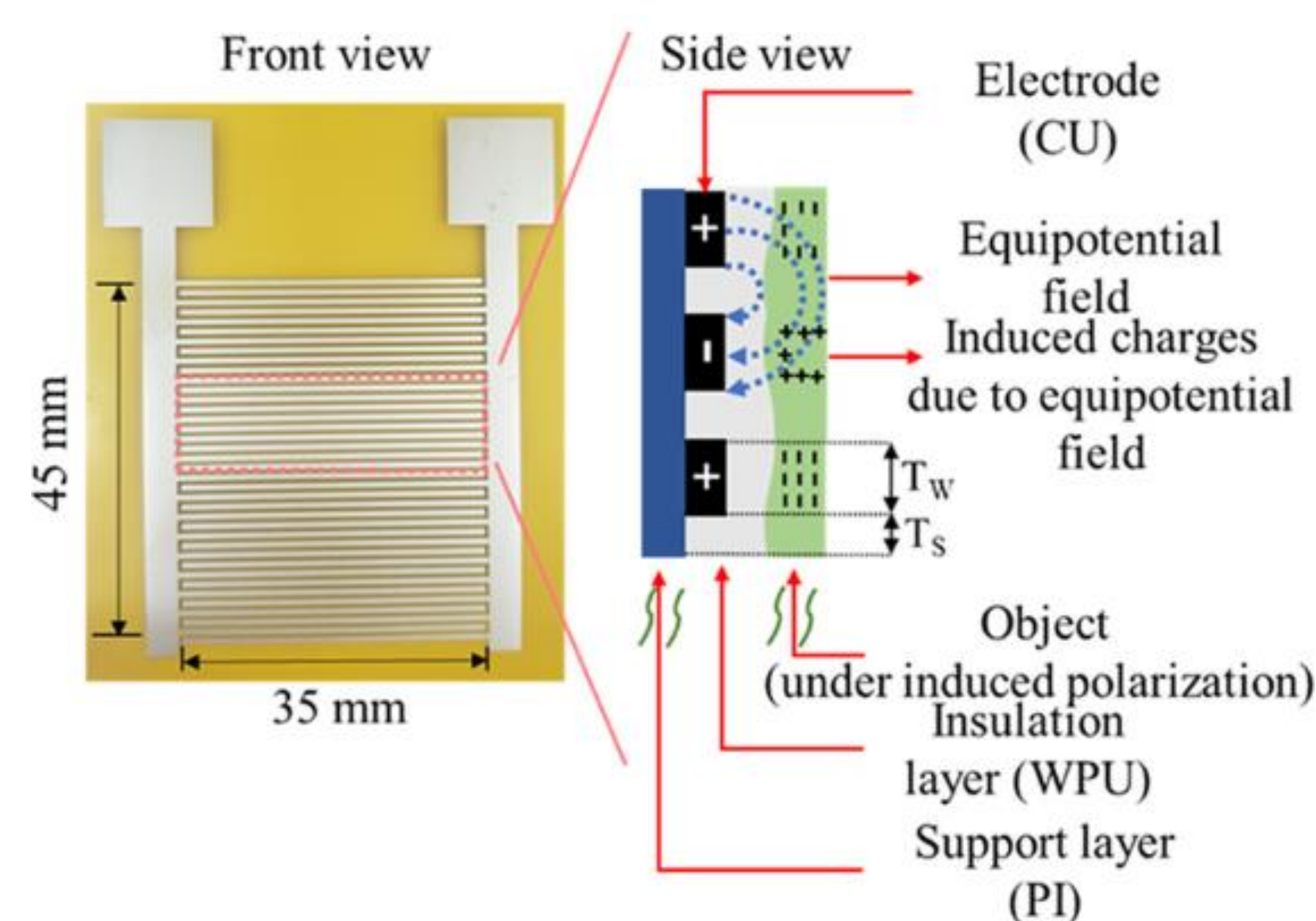


Figure 1: Top performing interdigitated electroadhesive[4].

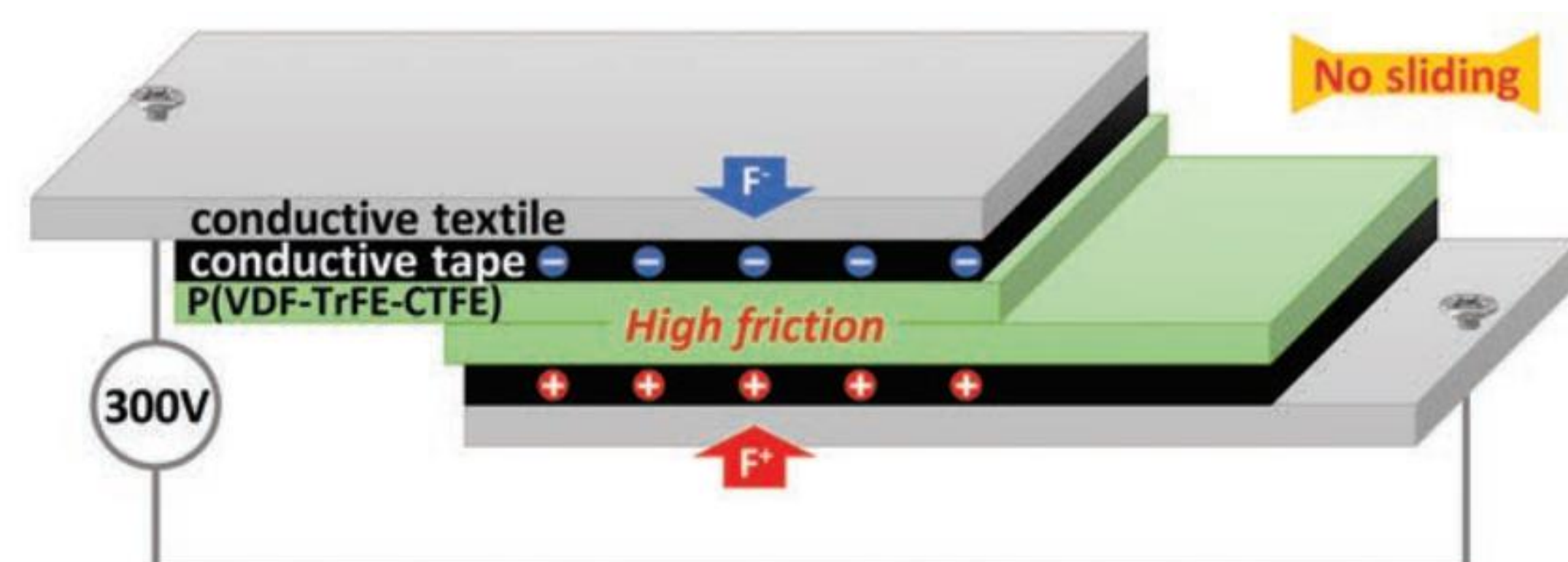


Figure 2: Top performing parallel plate electroadhesive[3].

Objective

- Certain disadvantages of electroadhesives make implementation difficult in prostheses.
 - Parallel electrode geometry requires grounding of one side.
 - Most interdigitated electrode designs are too weak for many applications in prostheses.
- Leverage characteristics of state of the art electroadhesive designs to accommodate prosthesis applications, i.e. high force density, small profile, and flexibility.

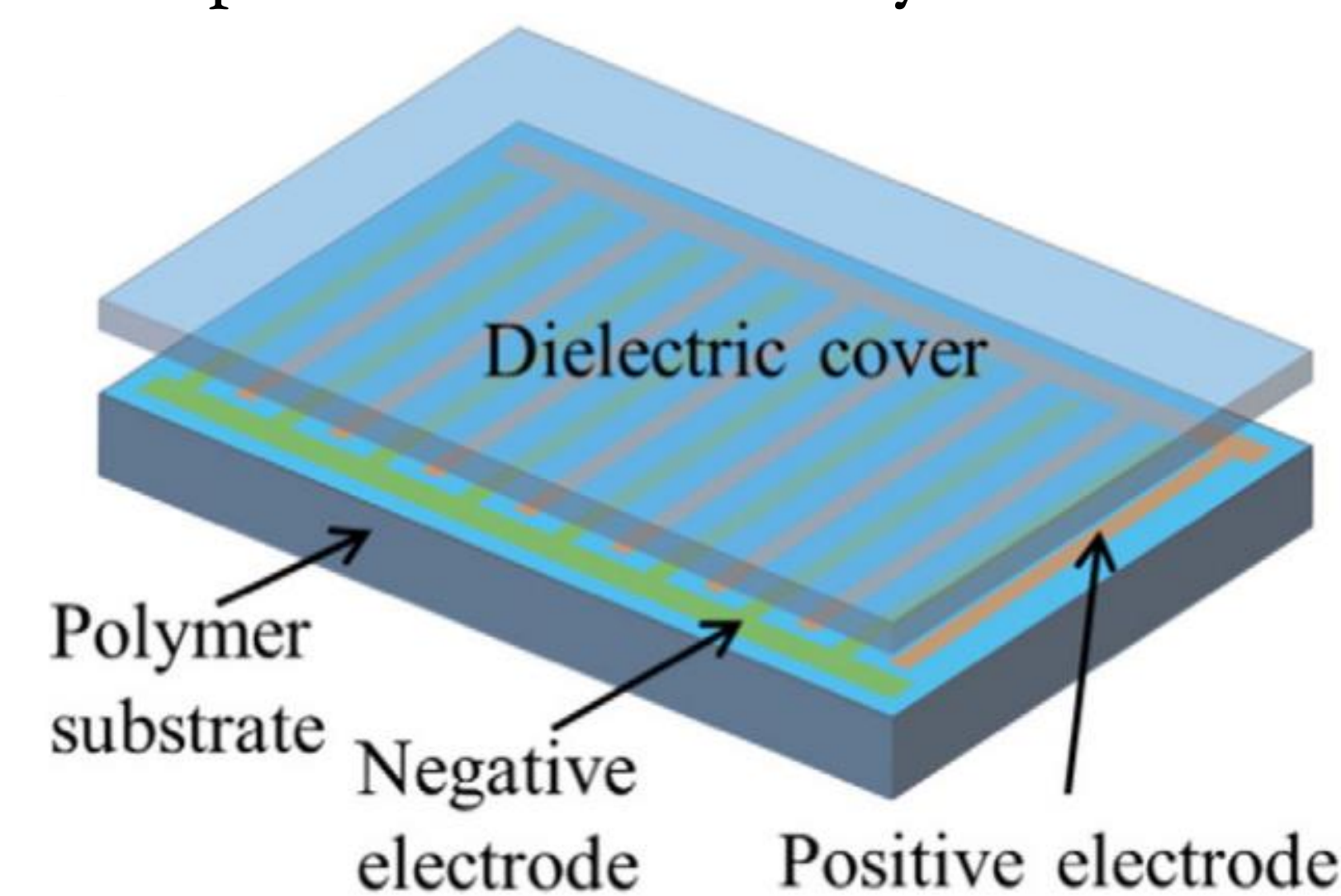


Figure 3: Electroadhesive architecture representative of the concept proposed for this work[2].

Approach

Materials Research

- Force density is dependent on electrical properties of the dielectric.
 - Ability to withstand high operating voltages (breakdown voltage).
 - Ability to permit electric field (electrical permittivity).
- Varying fabrication methods with dielectrics affect design feasibility.

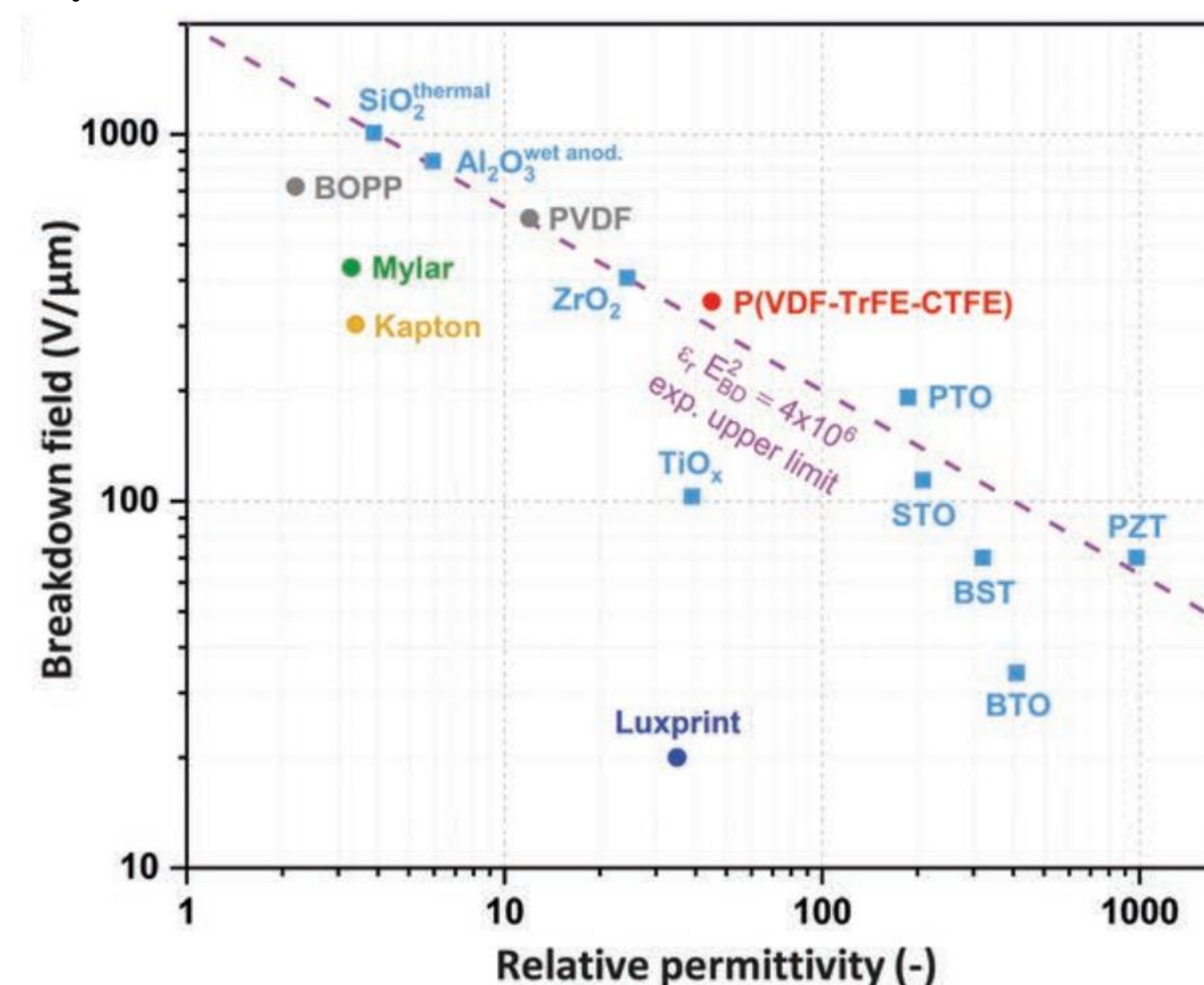


Figure 4: Dielectric performance of materials used in prior art[4].

Electrode Geometry

- Interdigitated electrode geometry provides easiest implementation for different applications.
- Force density directly related to electrode's width, spacing, and dielectric thickness[2].

Initial Design Concept

Materials Selection

- 0.002" copper foil electrodes
- PiezoTech® P(VDF-TrFE-CTFE) RT-TS dielectric ($\kappa = 40$)
- 1/8" Fabric-Reinforced High-Temperature Silicone Rubber Base
- DEVMO 8-32V to 45-390V DC-DC High Voltage Boost Converter
- LM317 voltage regulator

Design Parameters

- Supply voltage: 350V DC
- Electrode dimensions (width, spacing): 2mm, 0.5mm
- Dielectric thickness: 25 μ m
- Device profile (length, width): 3cm, 1.5cm
- Predicted Force Density: >25kPa

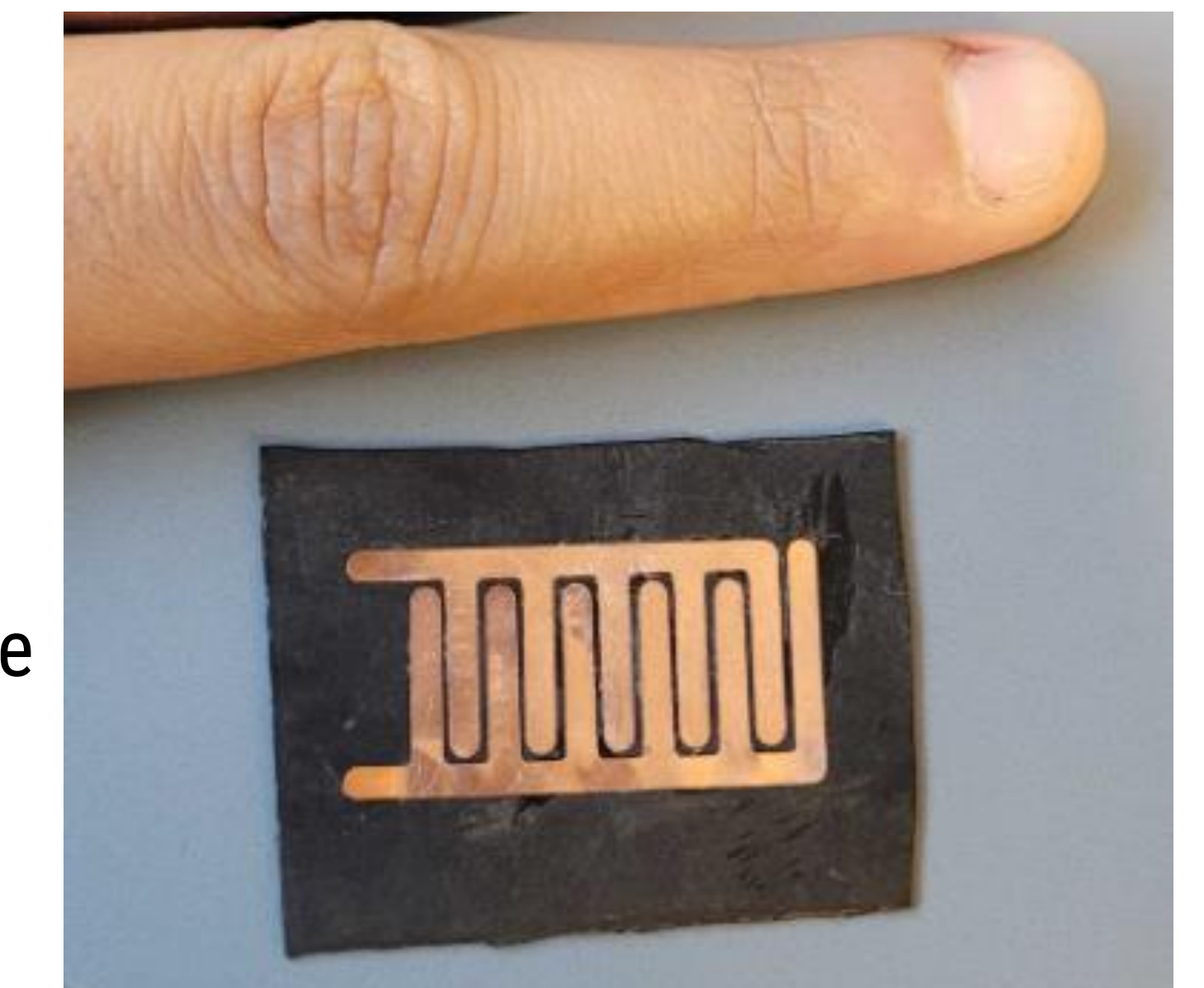


Figure 5: Fabrication test of electrodes on rubber substrate. Electrode width and spacing will be reduced to find the limitations of the current fabrication method.

Future Work

- Determine electrode dimension limit of fabrication method
- Complete fabrication of functioning prototype
- Verification and characterization testing of prototype
- Implement H-bridge to actuate with AC
- Prosthesis implementation

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References

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